

Intra-fractional motion management

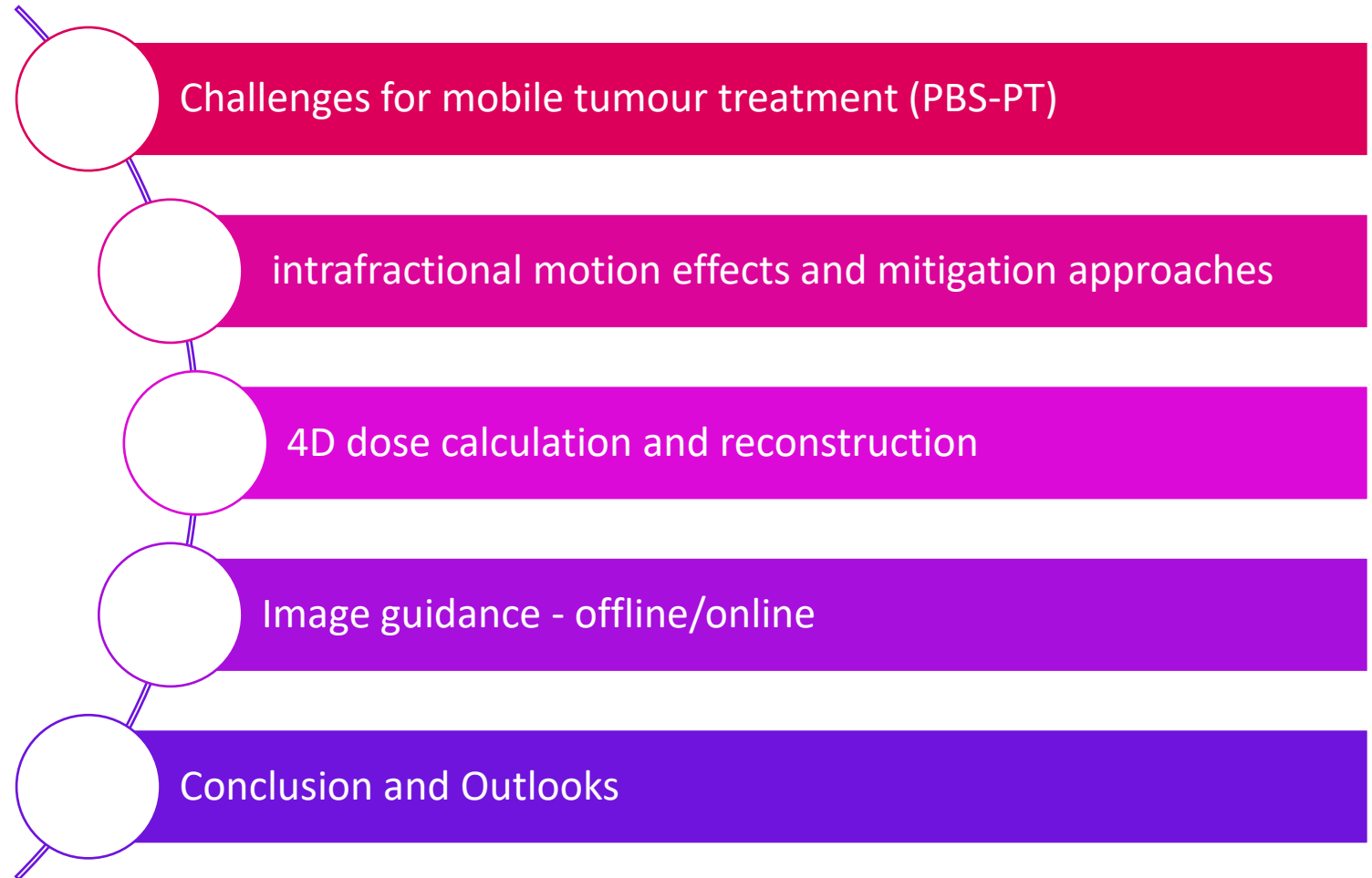
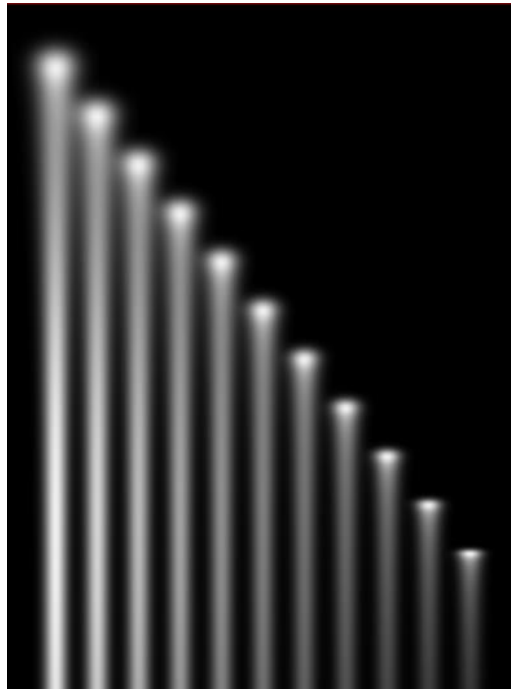
The 1st UPLIFT school on “Advanced Radiotherapy”

Ye Zhang, PhD

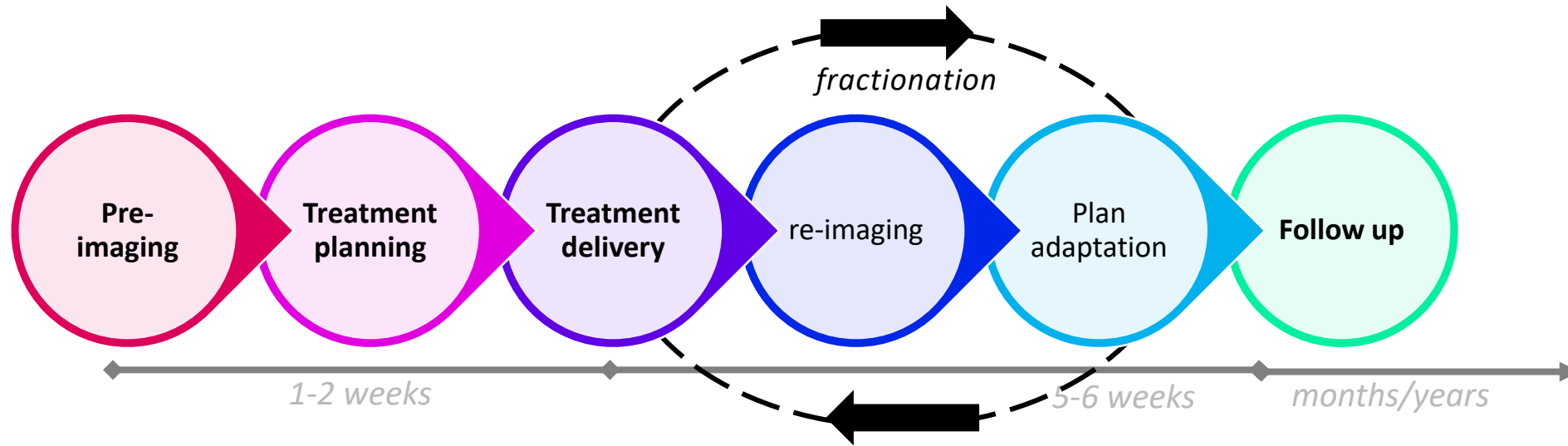
Centre for Proton Therapy,
Paul Scherrer Institute, Switzerland

Lyon, France, 2025/11/21

Contents of this presentation



What is 4D treatment? and why?

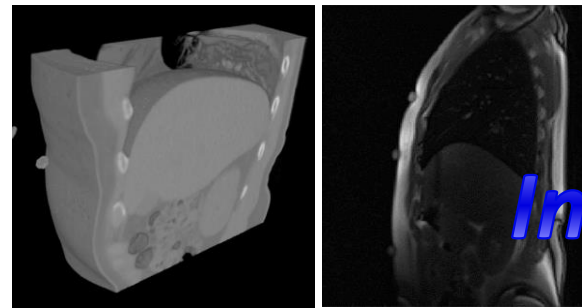


Intra-fractional: respiration, heart beating
(deformable movement)



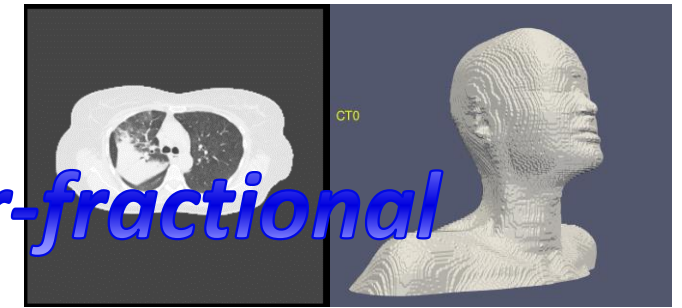
seconds

+ digesting movement, muscle
relaxation (deformation, drift)



minutes

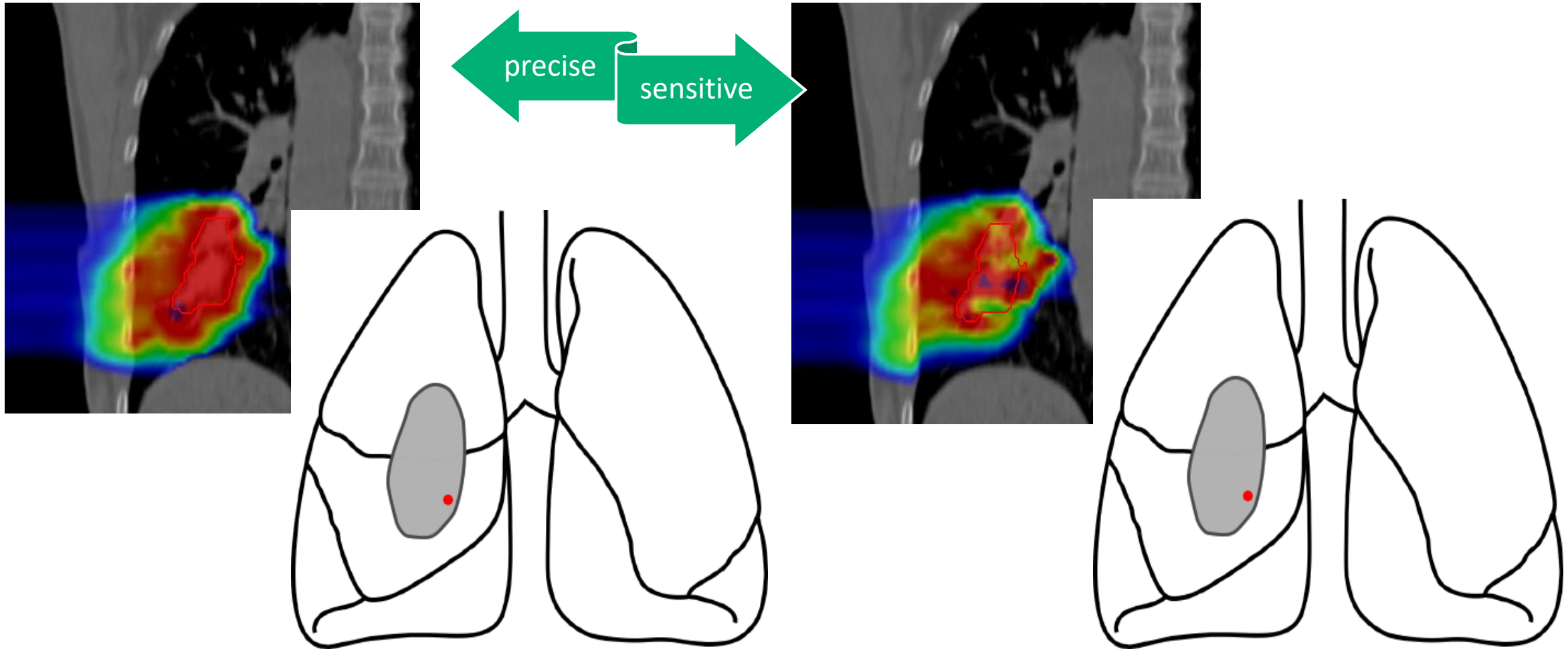
Inter-fractional: anatomy variation
(deformable grows, shrinks, shift)



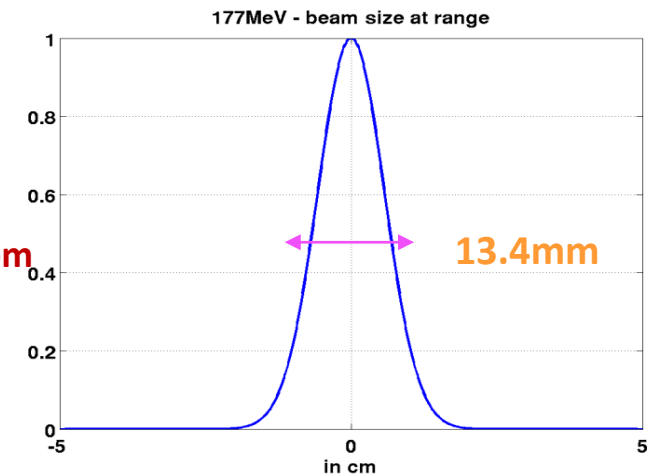
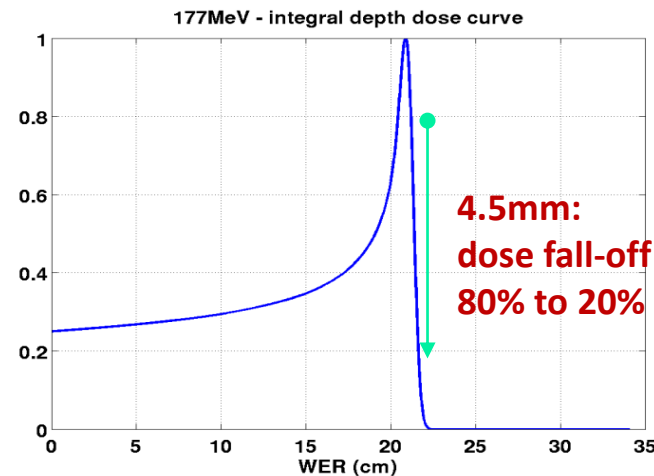
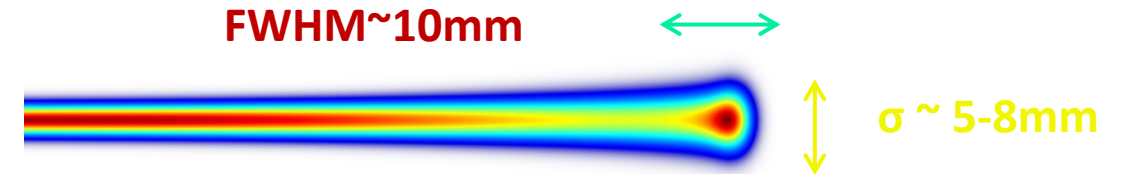
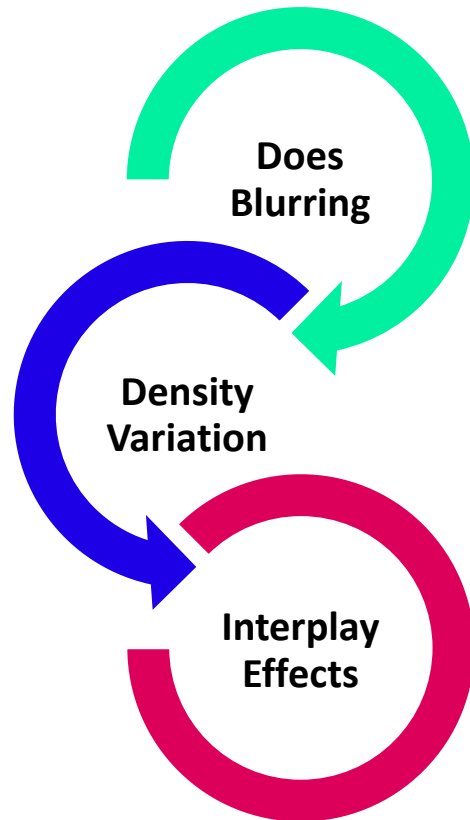
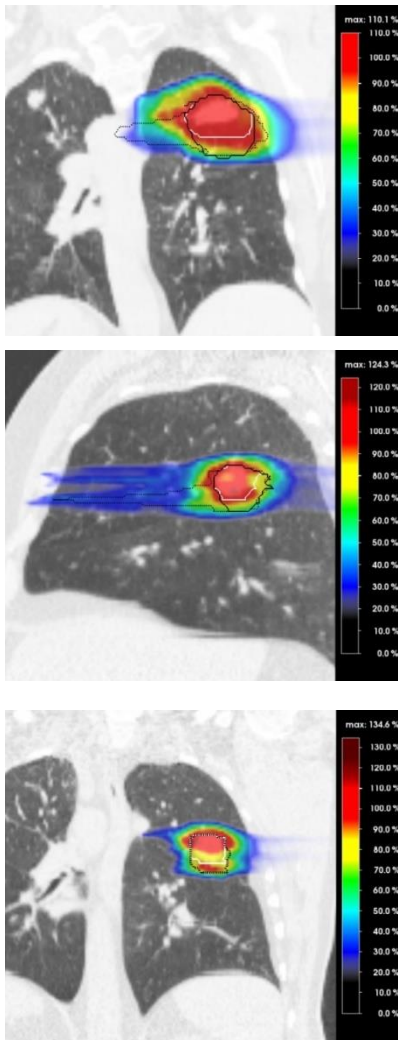
days

4D -> any geometric difference between the phase of planning and the phase of dose delivery

Pencil beam scanned proton is a double-edged sword



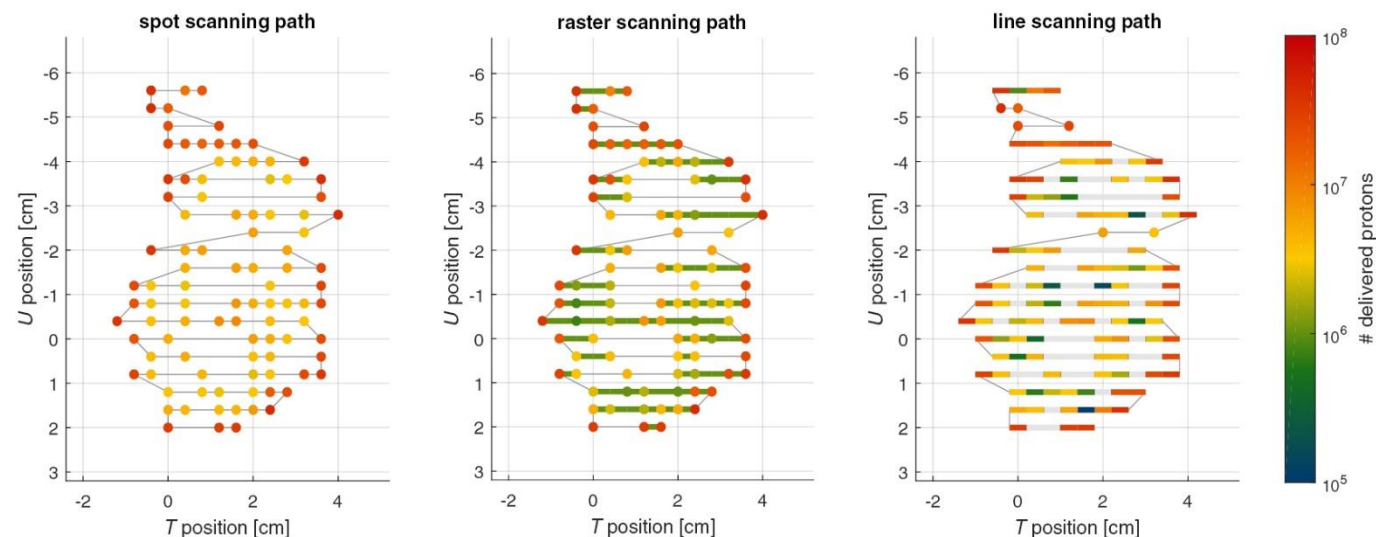
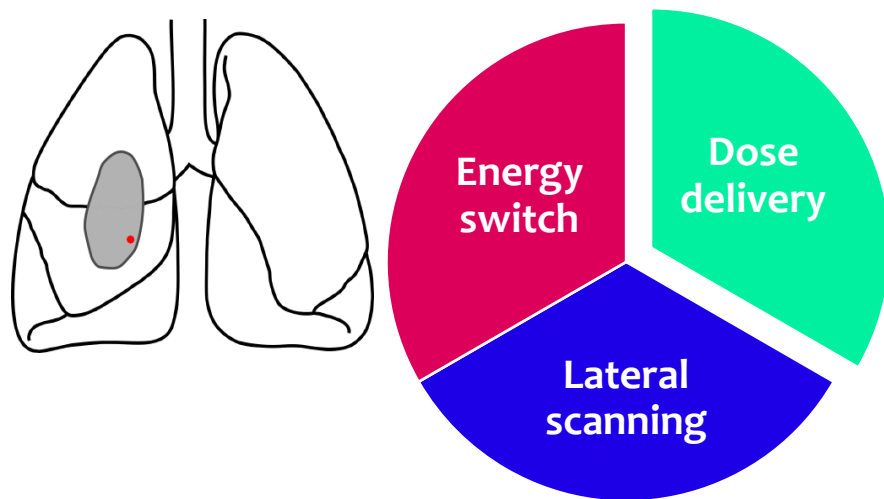
Intra-fractional motion effects



- **lateral dose conformity:** Universal for any external RT target out of planned dose delivery field
- **distal dose conformity:** for particle therapy density variations in the beam path
- **dose homogeneity:** only for scanning delivery Interference target motion and timing of active scanning

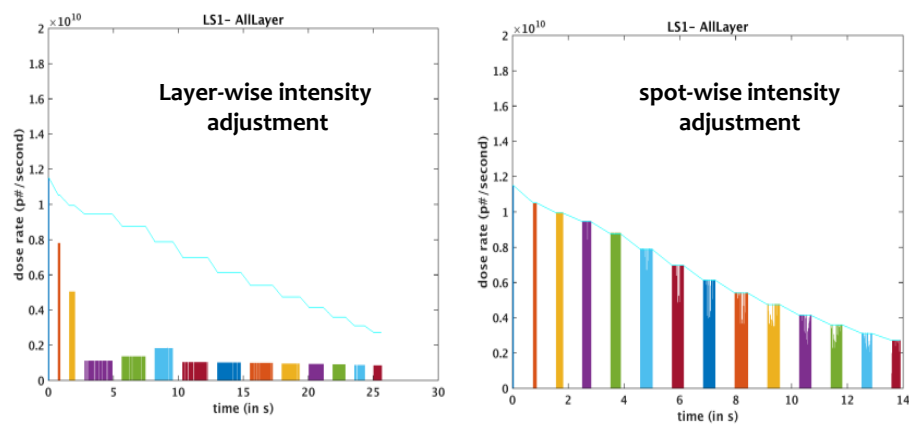
Intra-fractional motion effects are significant, requiring individual assessment and combined mitigation strategy

Dynamic beam delivery

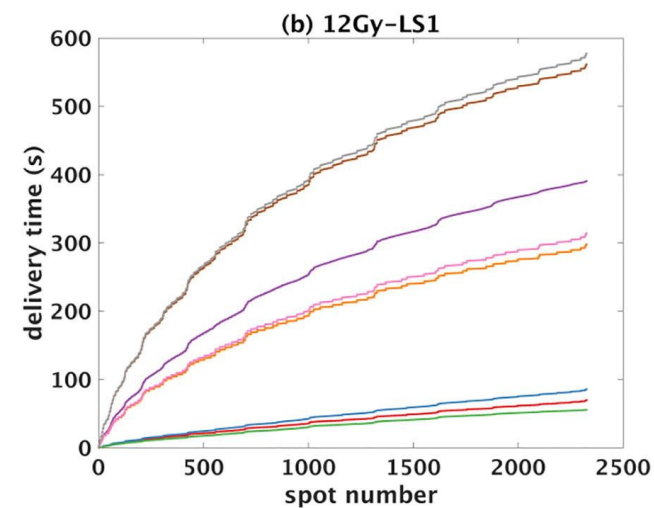
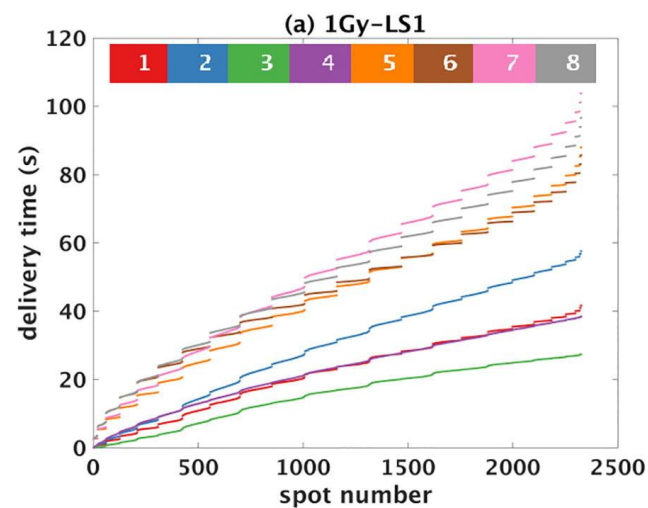


Lateral scanning mode

G Klimpki et al 2018 PMB

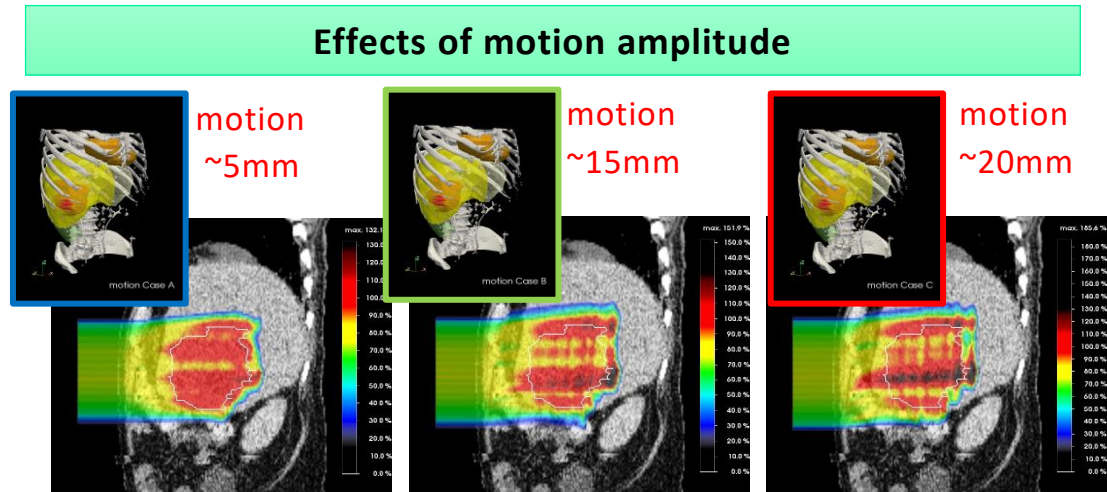
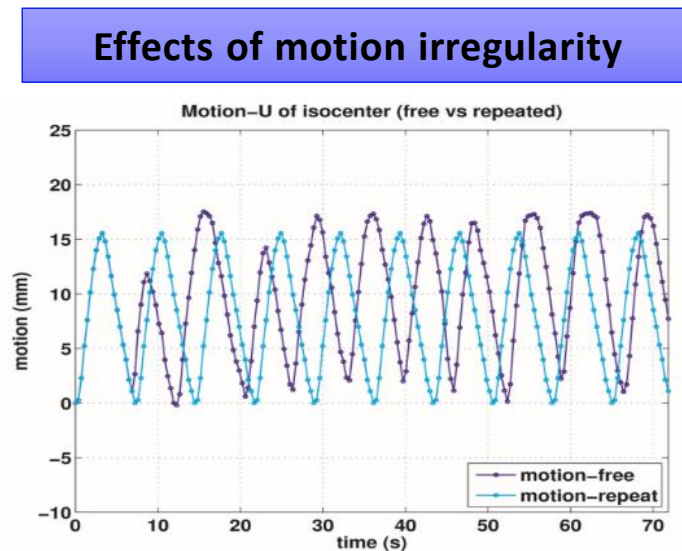
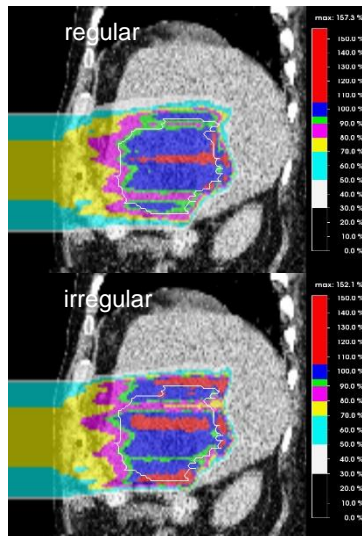


beam current

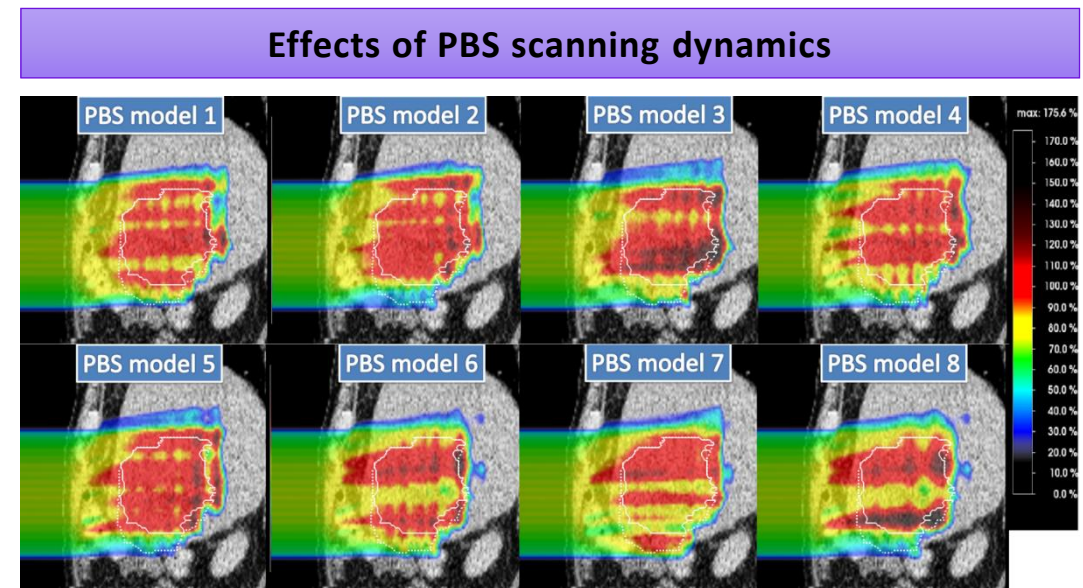


Interplay effects for dynamic dose delivery

- The **interplay effect** are significant, individualized and can be influenced by many 4D parameters
- 4D dose distribution** patterns is very difficult to predict without appropriately modelling the dynamics from both *moving organ* and *PBS-based dose delivery*

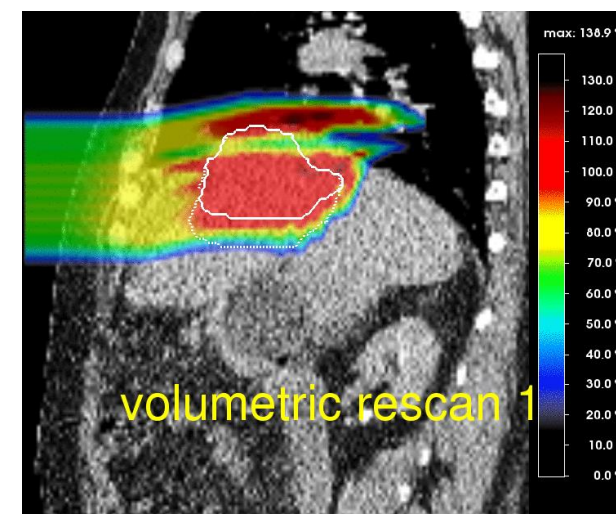
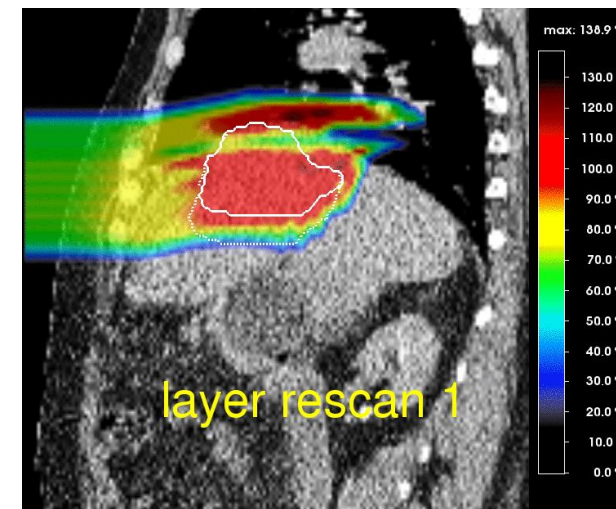
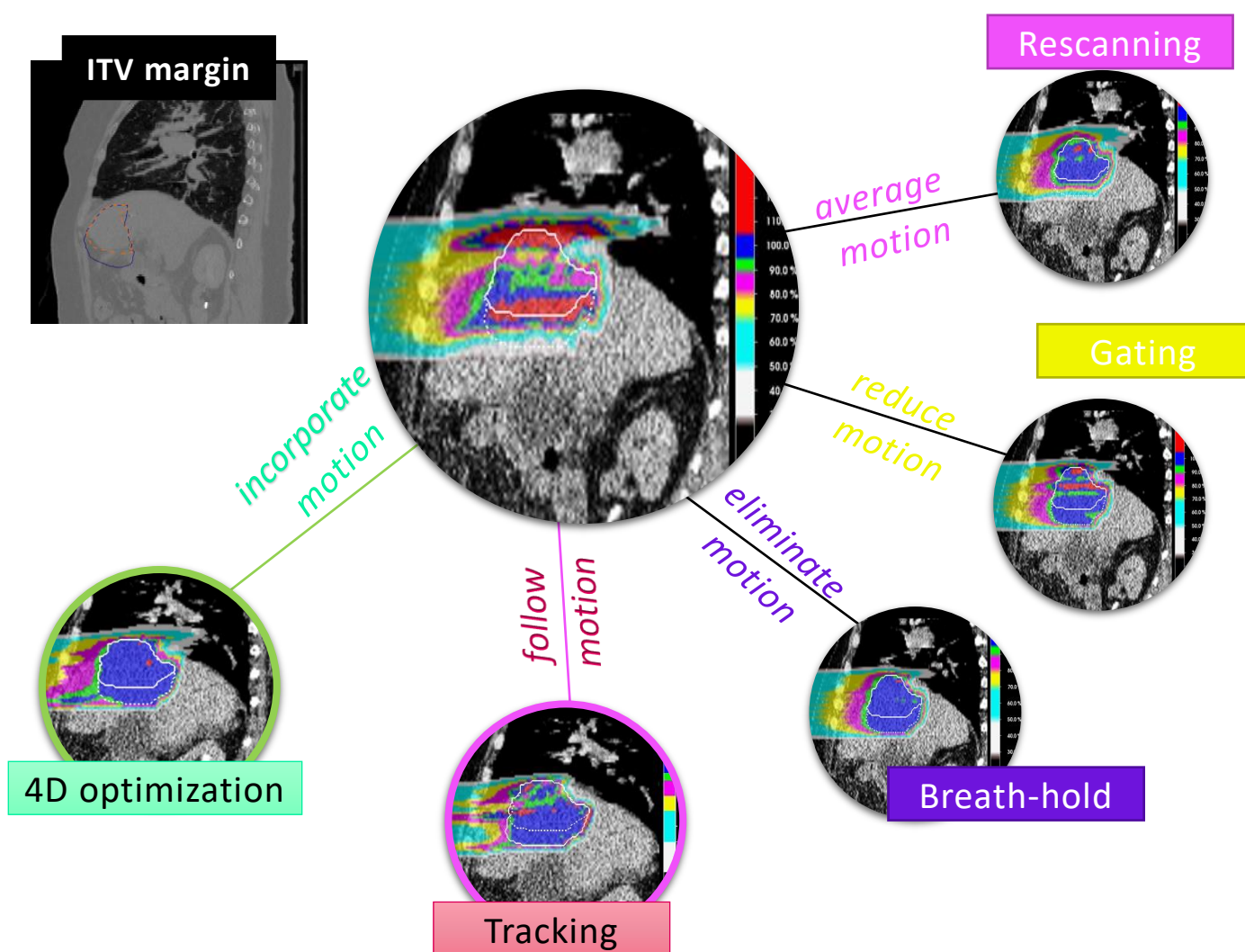


Zhang et al PMB 2017



Zhang et al Radiotherapy and Oncology 2016

Intra-fractional motion mitigation



Breath-hold: fast delivery and patient cooperation



Technical challenges

Max. beam current for Cyclotron

Energy dependent beamline transmission

Max. acceptable beam current for beam diagnostic

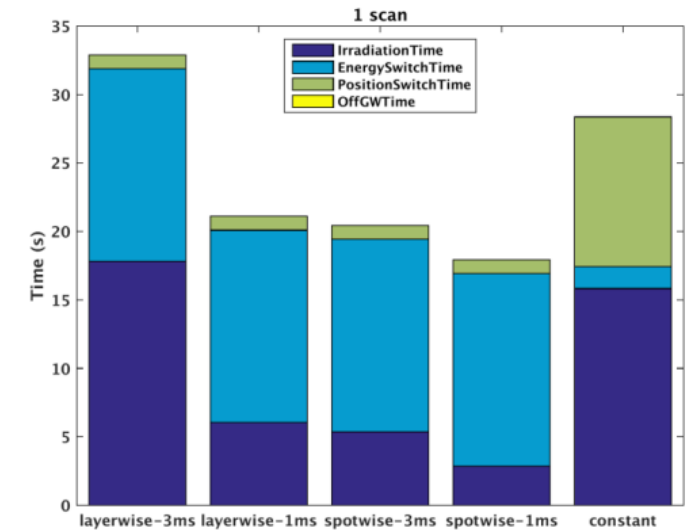
Achieve the minimal spot duration

Plan requirements

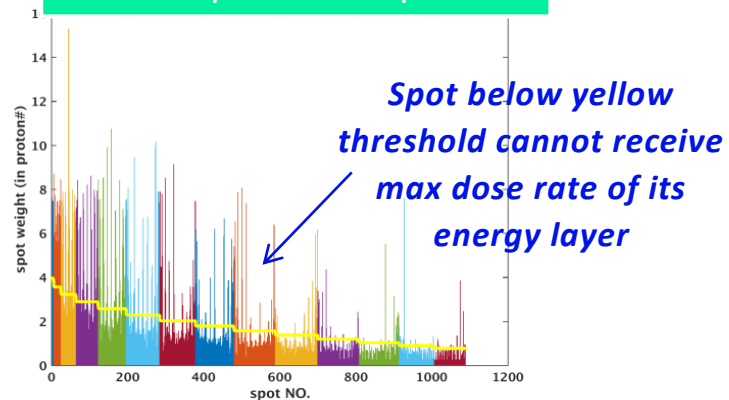
high spot weight dynamics with each energy layer varies up to 10 times

More low weight spots due to rescanning

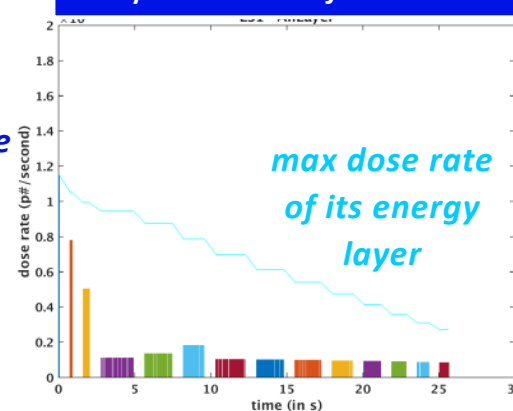
Capability to irradiate small weight spot



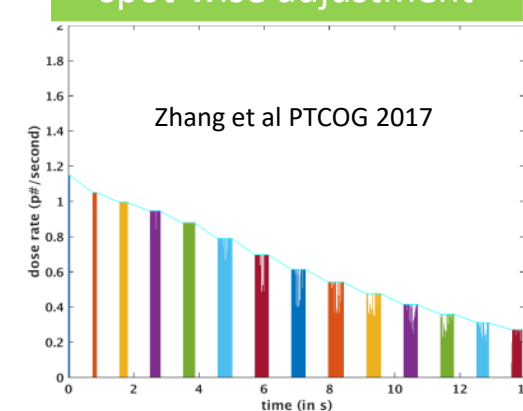
Example clinical plan



layer-wise adjustment



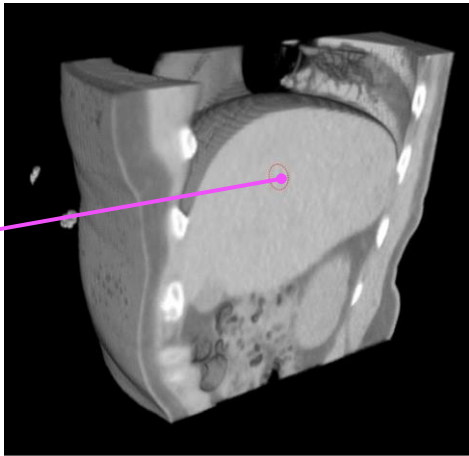
spot-wise adjustment



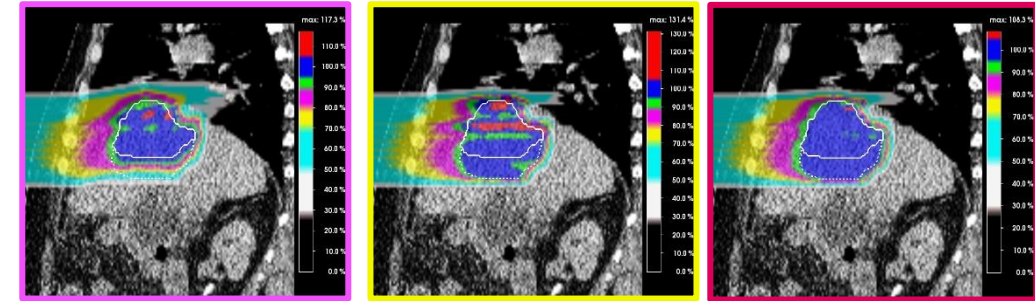
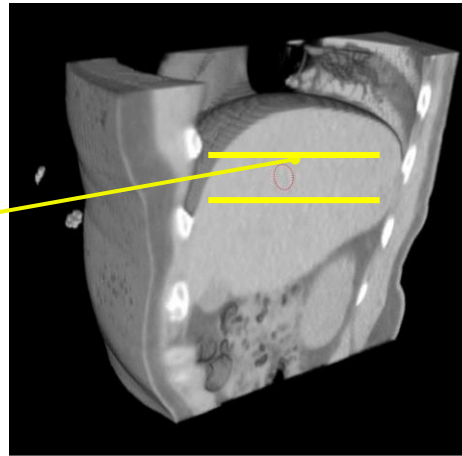
Rescanning-gating: a clinical practical approach



rescanning

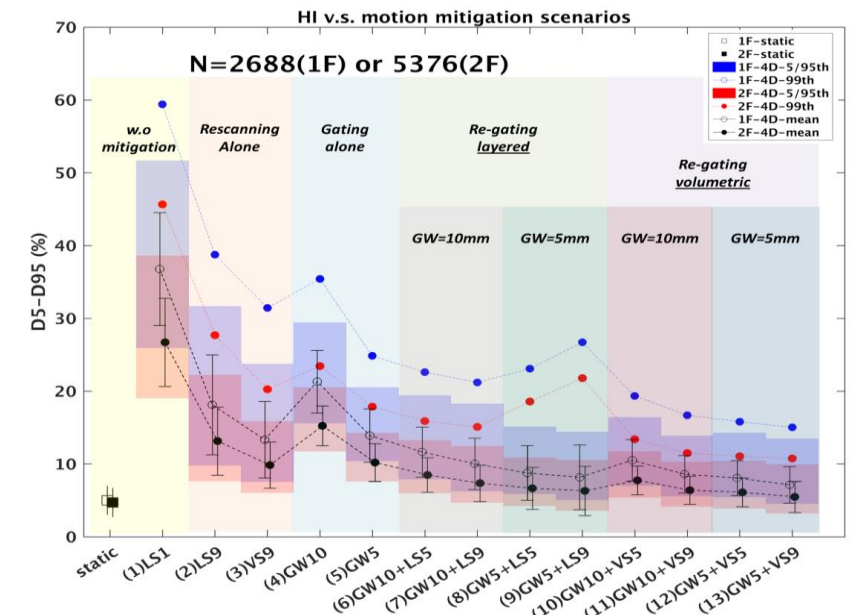


gating



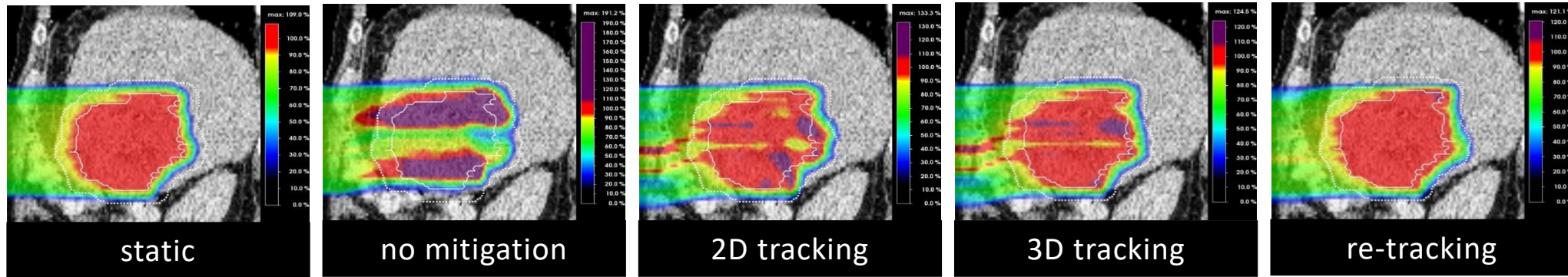
- easy to implement
- prolonged treatment duration
- extended irradiation volume
- appropriate ITV predefined
- scanning dynamic dependent
- need sufficient rescan number
- Statistical averaging is insufficient for large motion

- not difficult to implement
- prolonged treatment duration
- Restricted target volume expansion
- need to tackle the residual motion (wi rescanning)
- need online motion monitoring and correlation
- need to update gating window (baseli shift)



Zhang et al Radiotherapy and Oncology 2018

Beam tracking: towards real-time plan adaptation



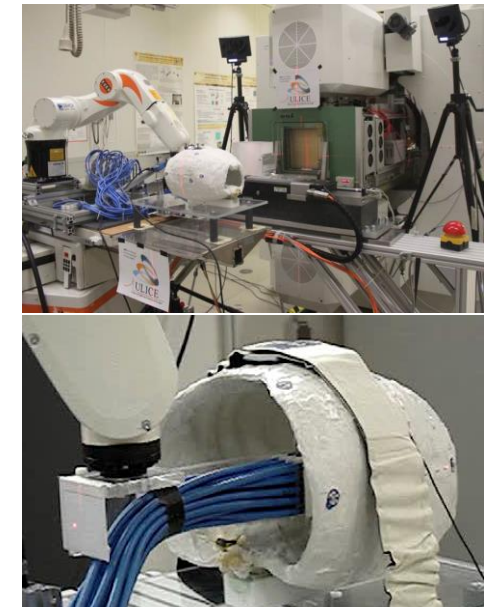
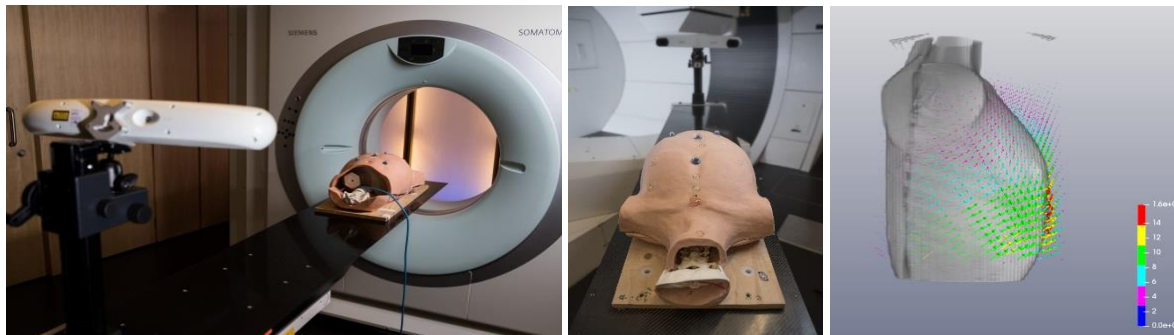
Zhang et al 2014 PMB

clinical beneficial

technical feasible

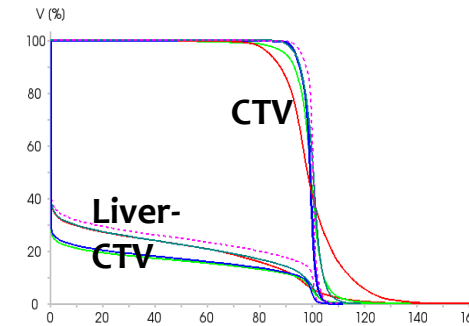
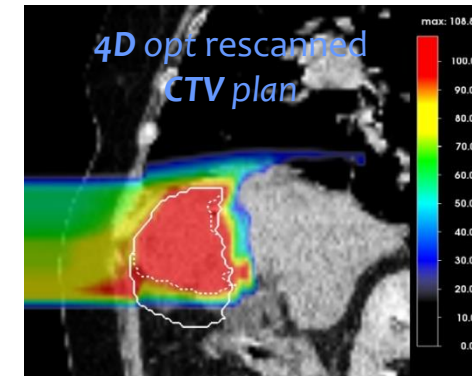
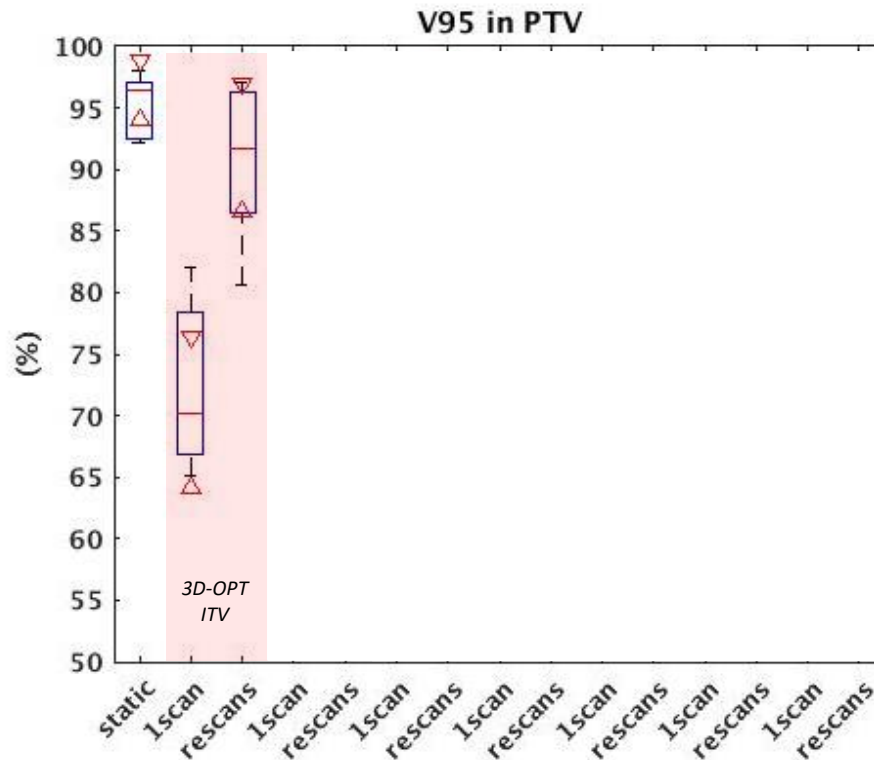
clinical applicable?

- Real-time motion monitoring without “too much additional” imaging dose
- Low latency (~50ms) measurements with high accuracy (<1mm)
- Fast energy adaptation with good beam quality
- Capable of adapting treatment field according to real-time updates



Steidl et al 2012 PMB (project from GSI)

4D optimization: making plan robust by itself



Advantage

No prolonged delivery time
No extended ITV margin

Disadvantage

Sensitive to difference in motion for optimization and for delivery
(if motion used by 4D optimization was not reproducible for validation, optimized dose homogeneity would collapse)

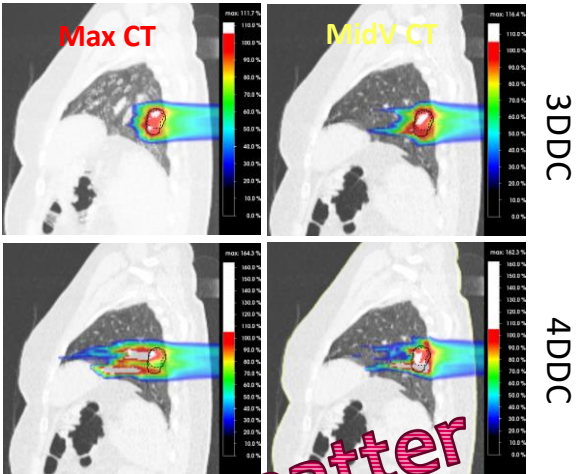
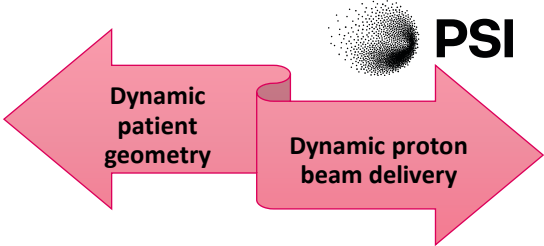
clinical beneficial

technical feasible?

clinical applicable?

How to calculate 4D dose perspective ?

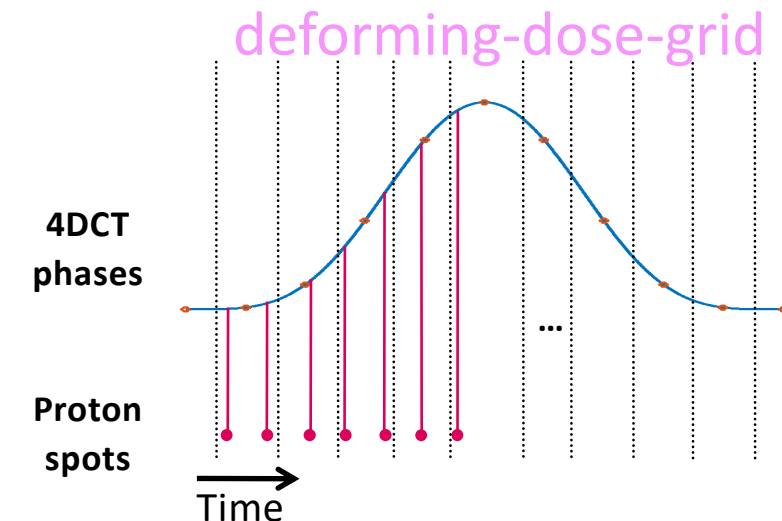
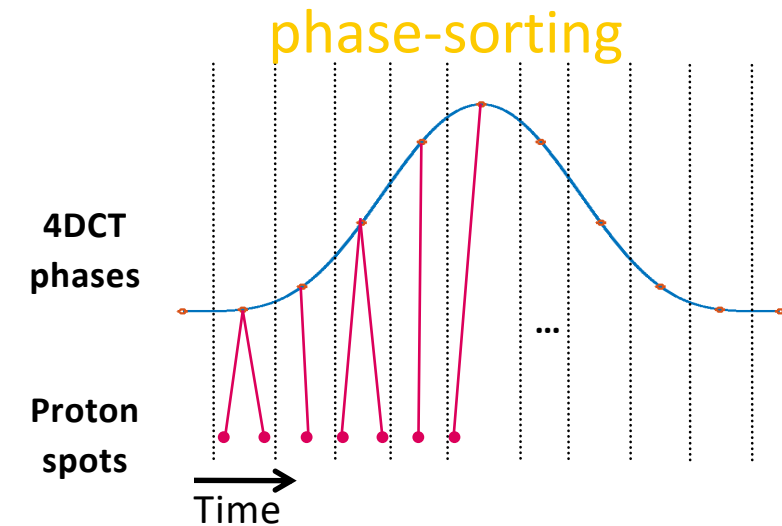
- The interplay effects are significant, individualized and can be influenced by many 4D parameters
- 4D dose is sensitive to all input factors from either machine side or patient side.
- 4D dose distribution is very difficult to predict without appropriately modelling the dynamics from both sides (moving organ and PBS-based dose delivery)
- It can be risky to make any conclusion or decision when only partial parameters are considered



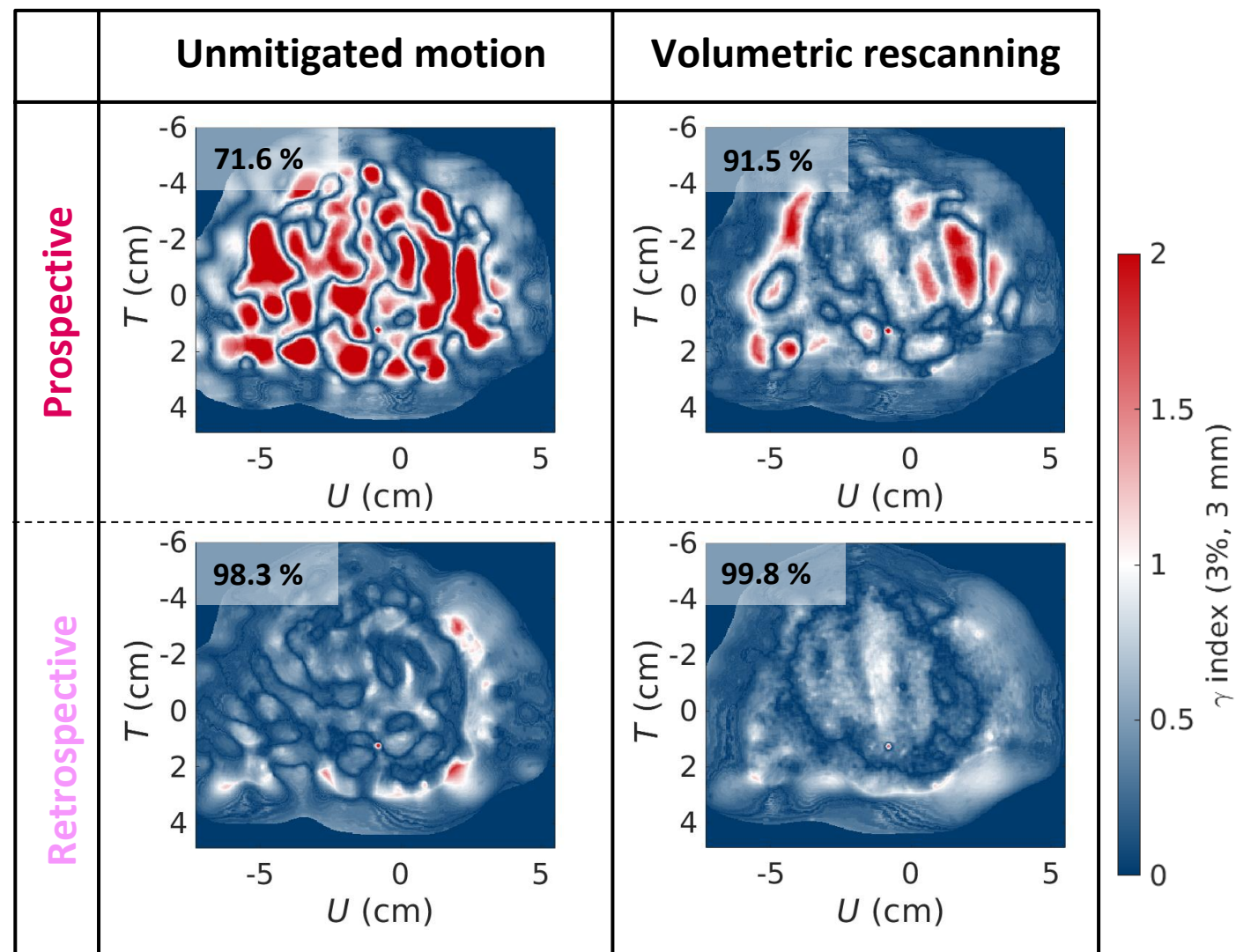
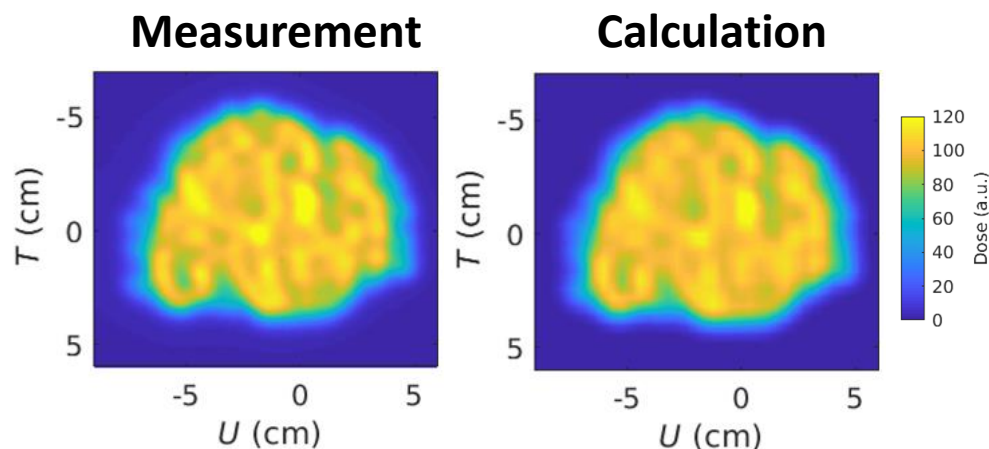
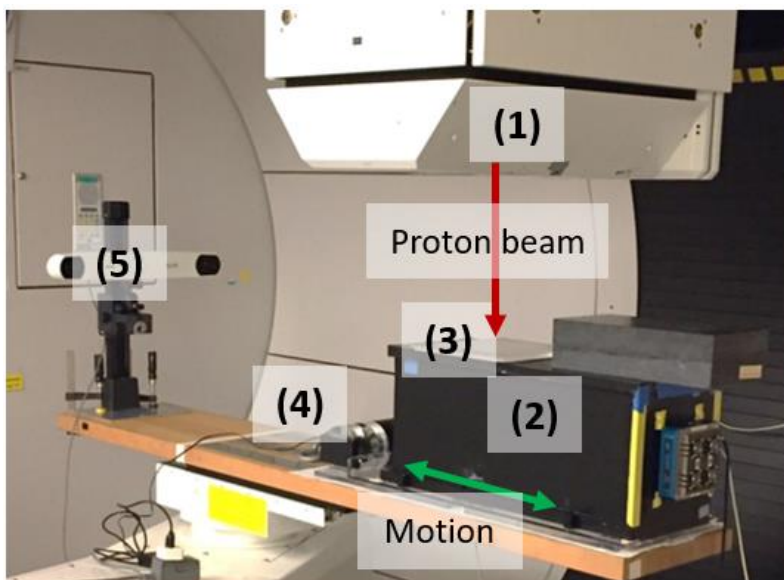
Motion mitigation		Motion	delivery dynamics	Interactions	Initial 3D plan	
rescanning	Type/path Number min-MU	amplitude	Lateral scanning mode: <ul style="list-style-type: none">• raster or spot beam	Starting phase for beam delivery	Patient geometry	PBS beam data
gating	Gating window Surrogate type Phase or amplitude	period direction	lateral scanning speed	Starting phase for multi-field combination	Field direction	Field arrangement
Breath hold	Amplitude Reproducibility	deformation	Energy switching time Dose rate		Spot distance	Energy layer distance
tracking	2D/3D w/wo weight optimization	Irregularity in period or amplitude	Dose deposition mode: <ul style="list-style-type: none">• constant• varied layer-wise• varied spot-wise	Number of field Number of fractionation	Scanning path	Scanning direction
4D optimization	scenarios				Prescribed dose	Fractionation scheme
					3D plan density: Max/mean/midV CT	3D plan geometry: CTV/gITV/rITV

4DDC approach and implementation

- Always remember 4DDC is based on 3DDC
 - analytical, pencil beam, MC ...
- 4DDC is calculating sub-groups of proton beams to their corresponding patient model of the beam delivery time, then summing them up to one defined geometry
 - Density model: CT (CT-like image)
 - Motion model: 4D images + deformable registration
 - Induced density variation model: 4DCT or warped 4DCT
- Calculation/prediction for the dose delivery timeline is essential
- Beam to motion assignment



Experimental validation of the 4DDC algorithm



How to use *perspective* 4DDC in clinics?

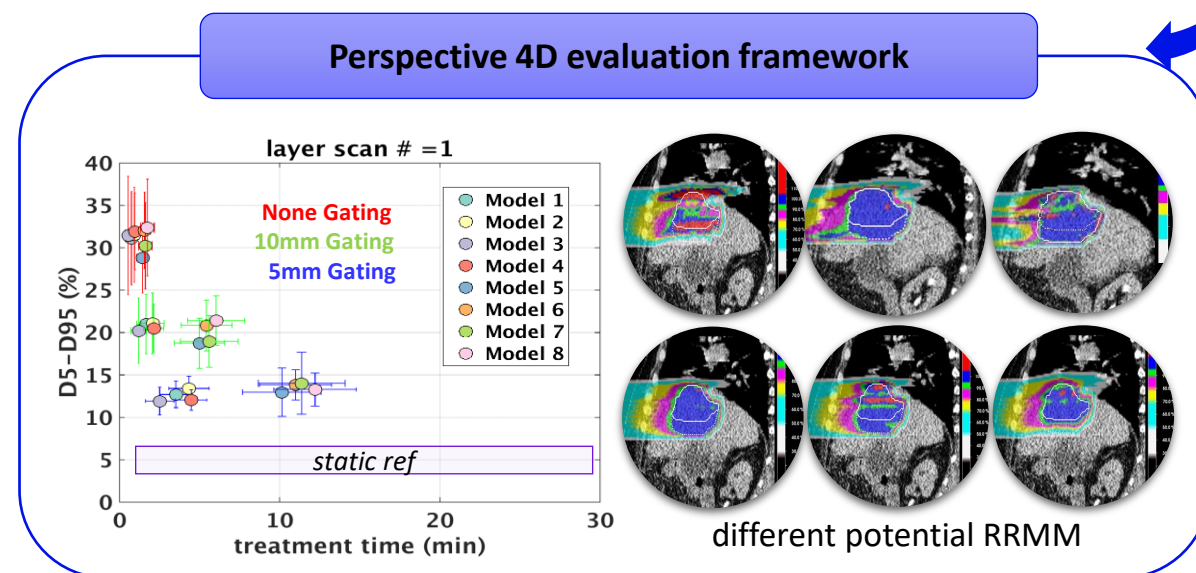
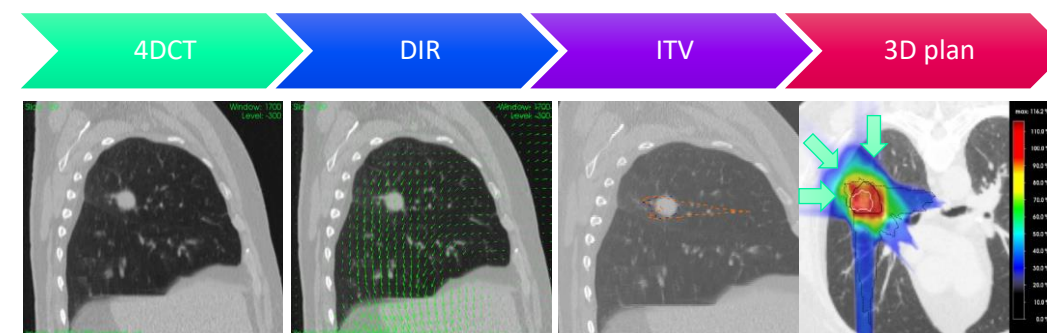


Patient specific 4D treatment evaluation

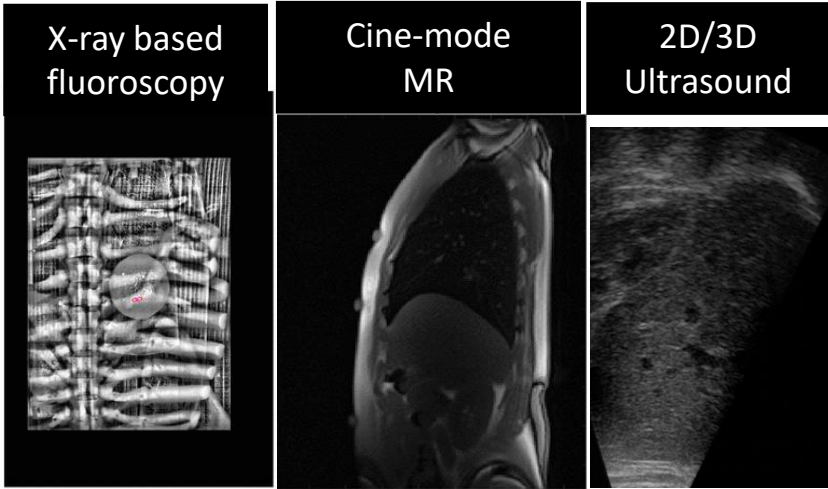
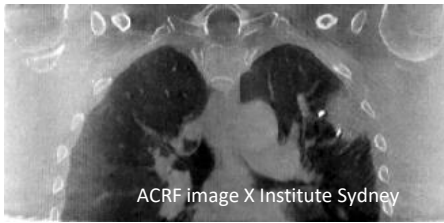
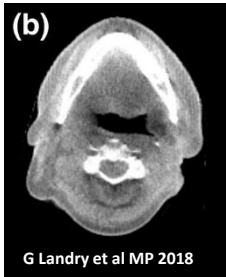
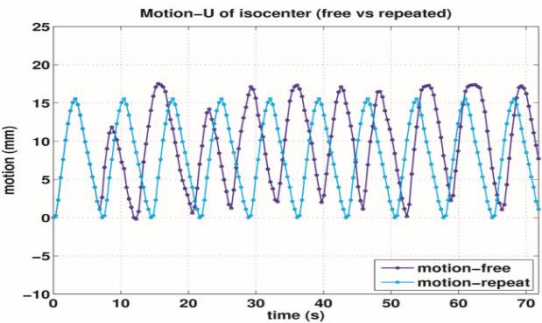
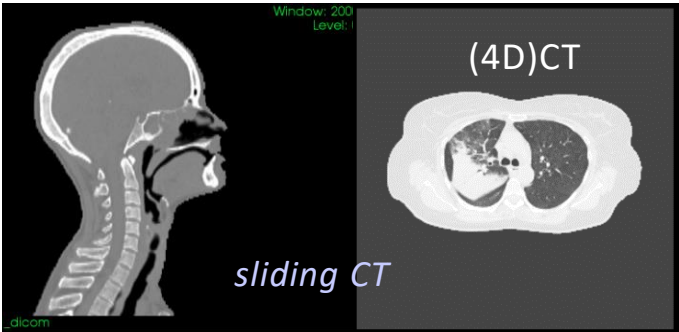
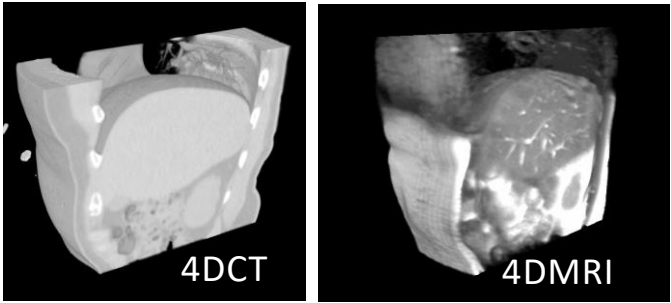
- to quantify interplay effect
- to determine effective motion management strategy
- to estimate potential uncertainty of fractional dose delivery

However, it is difficult to achieve due to the high dimension 4D parameters

Calculation load will increase exponentially The uncertainty from both machine delivery and patient motion during the dose delivery



4D image guidance: *offline*, *online* and *real time*



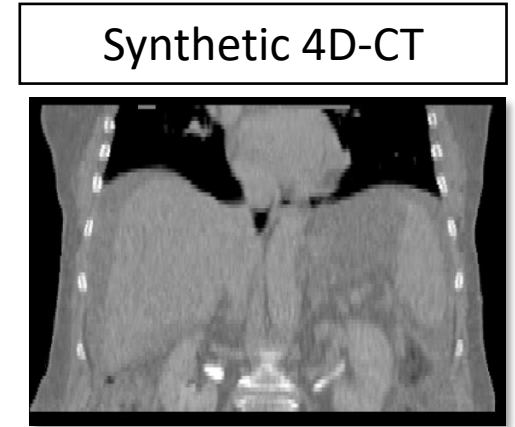
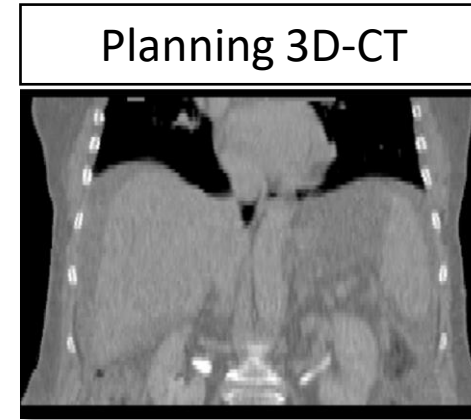
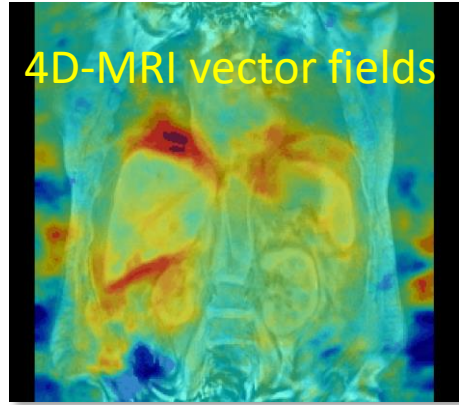
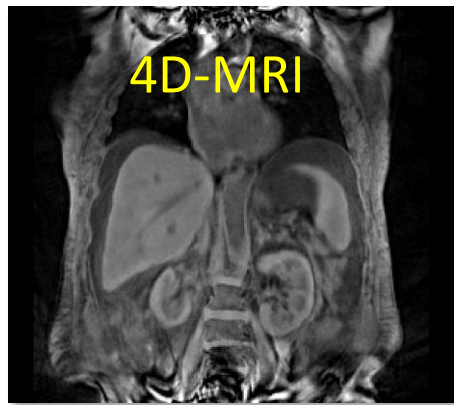
Volumetric	+++	++	-
Precise density	+++	+/-	-
Time resolved	++/+++	++	+++
Real time	-	+	+++
Sufficient VOI	+++	++	+
At treatment position	-	++	+++

Pre-treatment

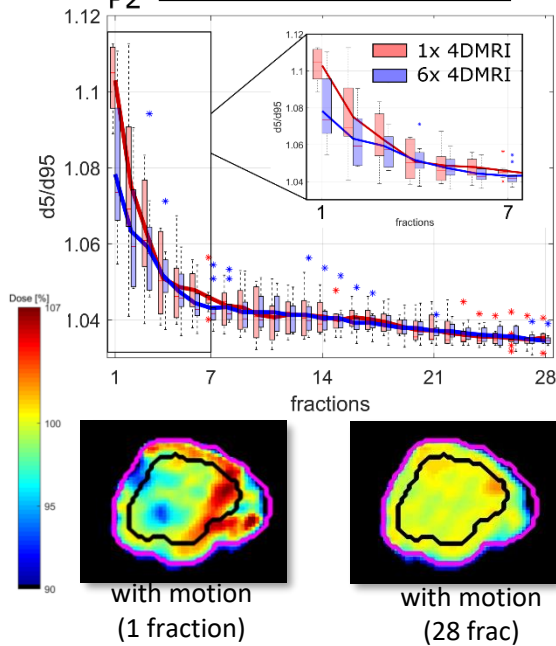
Before Fx treatment

During treatment

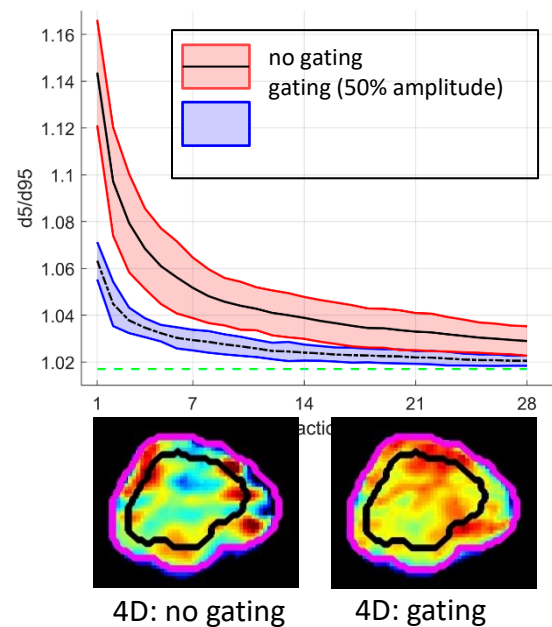
4DMR for 4D planning and evaluation



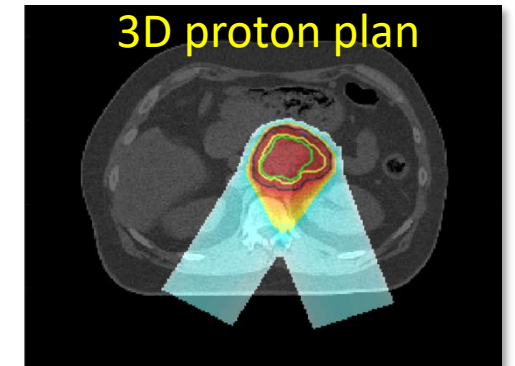
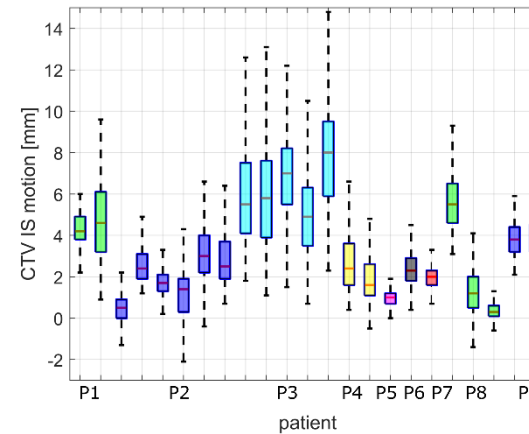
Effects of fractionation



Effective of gating

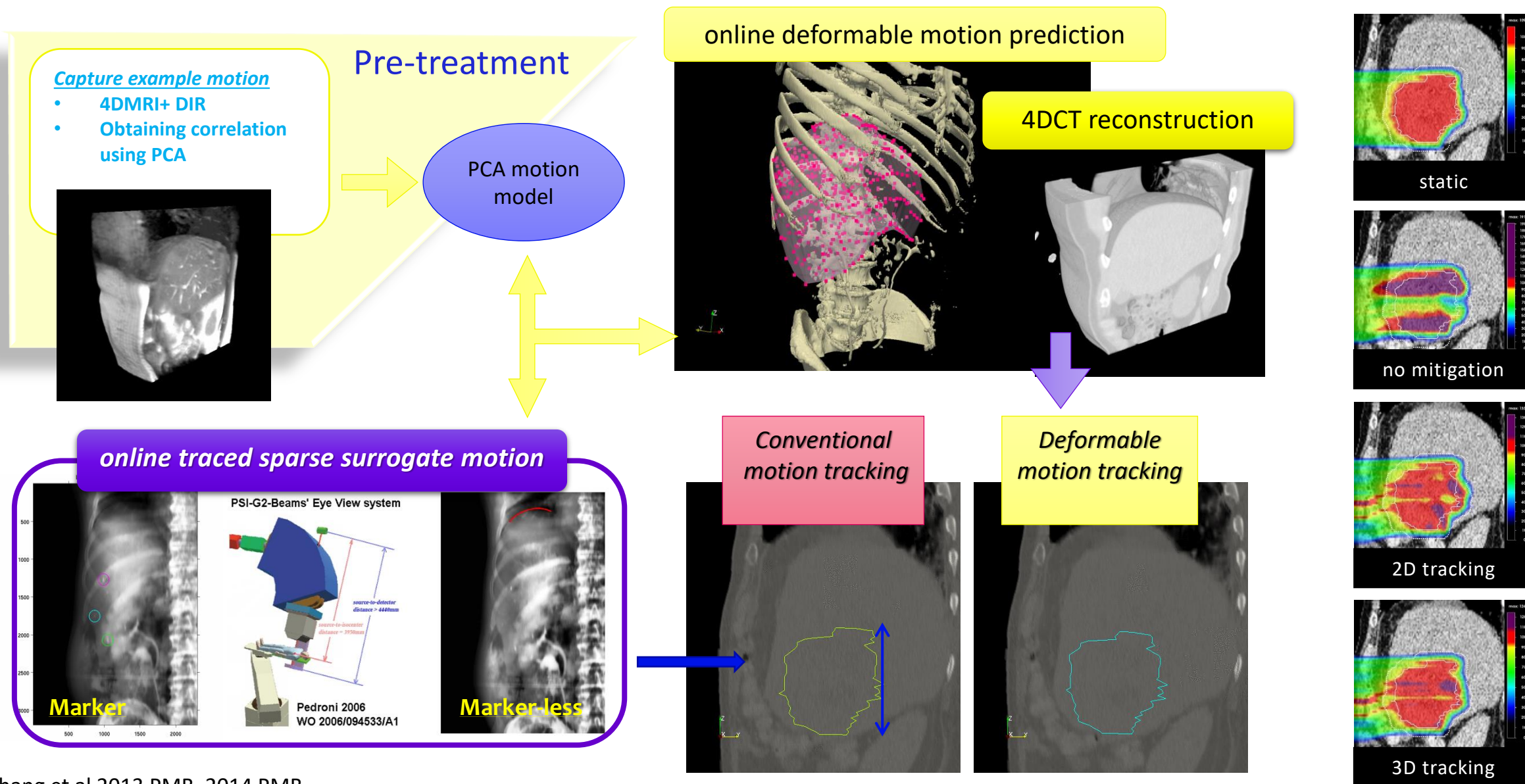


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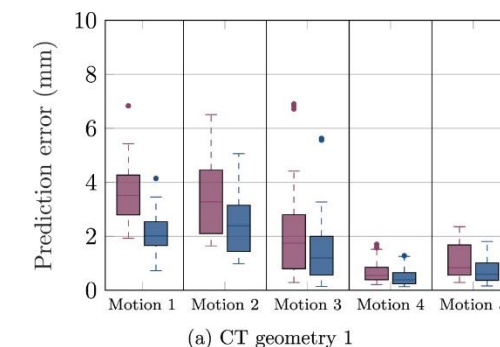
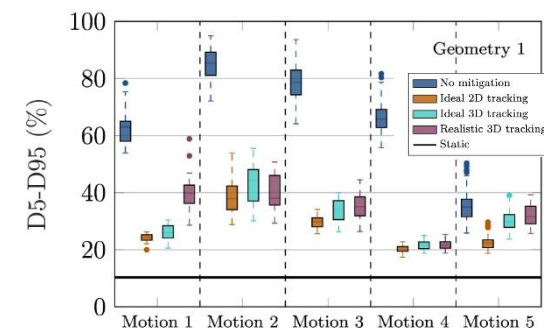
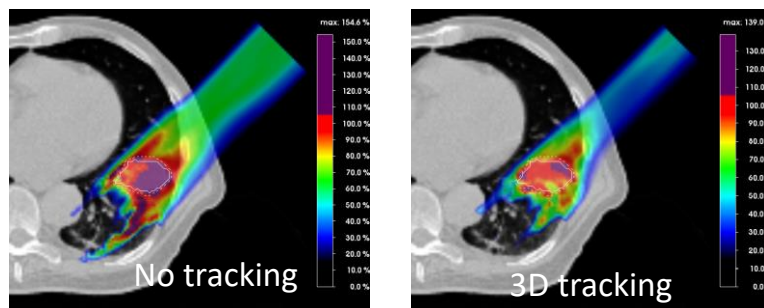
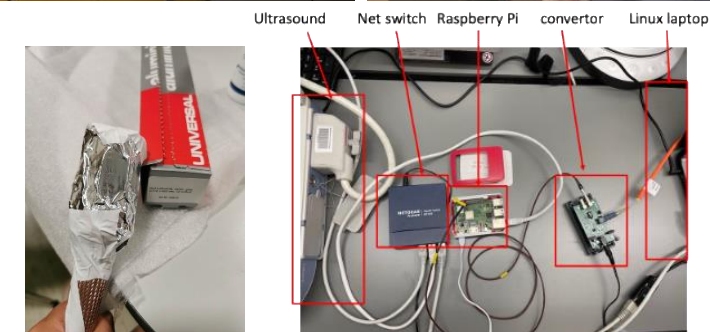
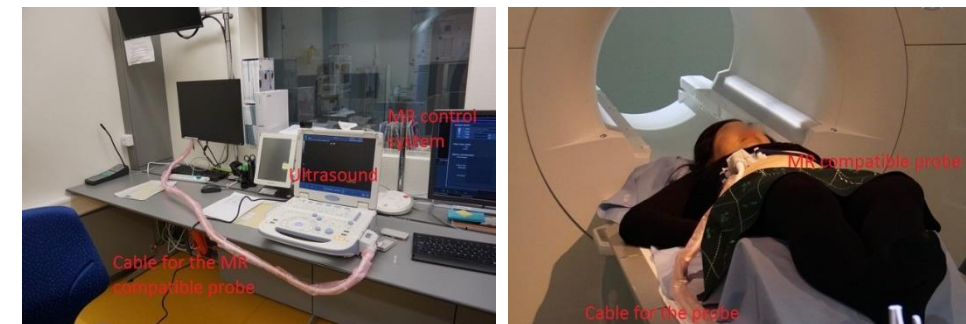
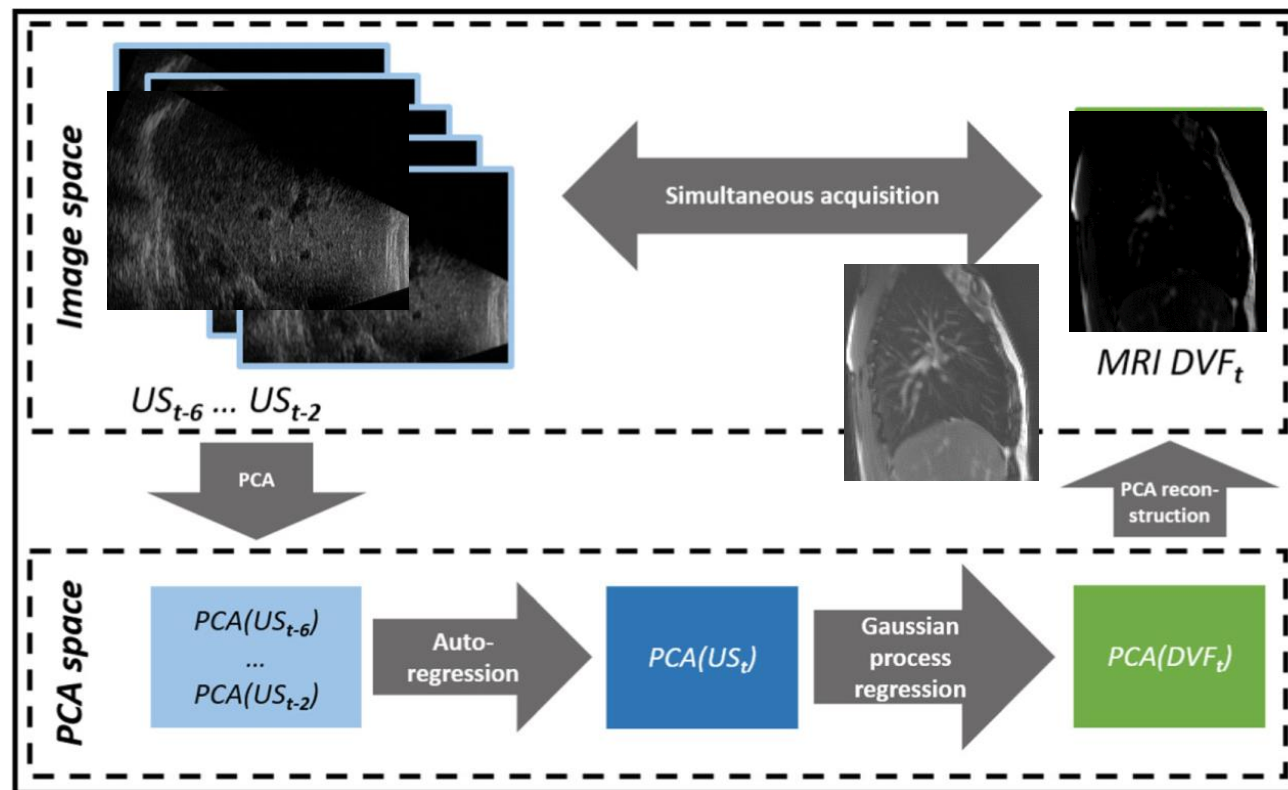


- K. Dolde, P. Naumann, C. David, R. Gnirs, M. Kachelriess, A.J. Lomax, N. Saito, D.C. Weber, A. Pfaffenberger, **Ye Zhang**. 4D dose calculation for PBS proton therapy of pancreatic cancer using repeated 4DMRI dataset. *Physics in Medicine and Biology*, 63(16) (2018) 165005 (**PMB 2018 Highlights collection**)
- K. Dolde, **Ye Zhang**, N. Chaudhri, C. David, M. Kachelriess, A.J. Lomax, P. Naumann, N. Saito, D.C. Weber, A. Pfaffenberger. 4DMRI-based investigation on the interplay effect for pencil beam scanning proton therapy of pancreatic cancer patients. *Radiation Oncology* (2019) vol: 14 (1) pp: 30 (shared first authorship)
- K. Dolde, P. Naumann, A.J. Lomax, N. Saito, D.C. Weber, A. Pfaffenberger, **Ye Zhang**. Comparison the effectiveness and efficiency of various gating approaches for PBS proton therapy of pancreatic cancer using 4DMRI datasets. *Physics in Medicine and Biology* (2019), 64 085011

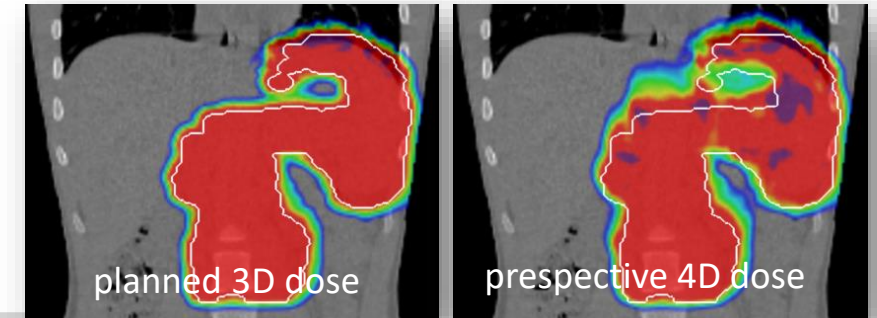
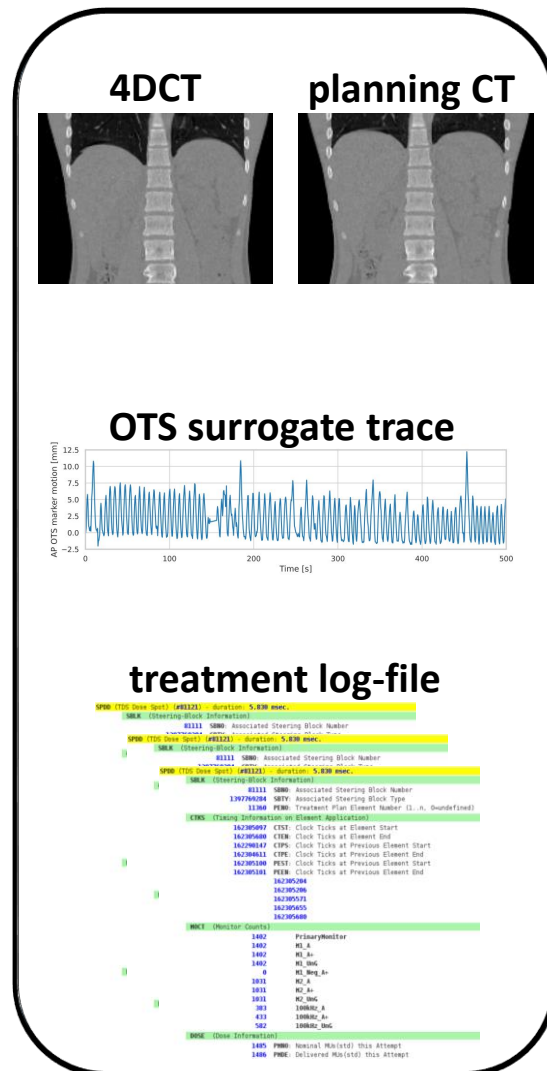
Motion model: bridging offline and online info



Liver-Ultrasound-guided lung tumour tracking



Motion model-guided Log file based 4D dose recon: method

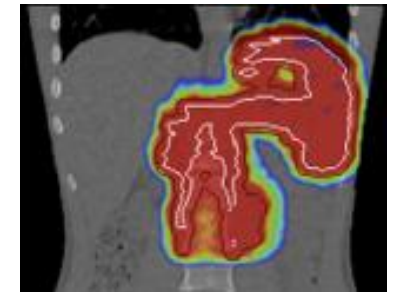


PCA motion-model

- patient-specific based on 4DCT
- reconstruction from OTS traces

4D dose reconstruction

- based on treatment log-files

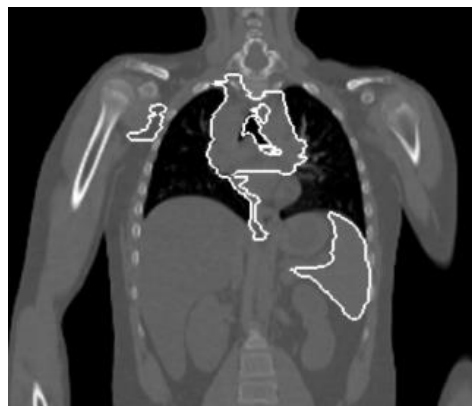


- Alisha Duetschler, Lili Huang, Giovanni Fattori, Gabriel Meier, Sairos Safai, Damien C. Weber, Antony J. Lomax, Ye Zhang. A motion model-guided 4D dose reconstruction for pencil beam scanned proton therapy. Physics in Medicine and Biology, 68 (2023) 115013

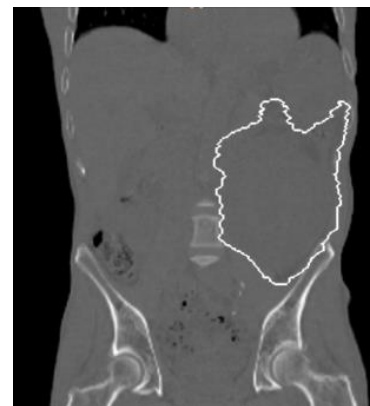
Motion model-guided Log file based 4DDR: clinic case



Case A
(Hodgkin's)

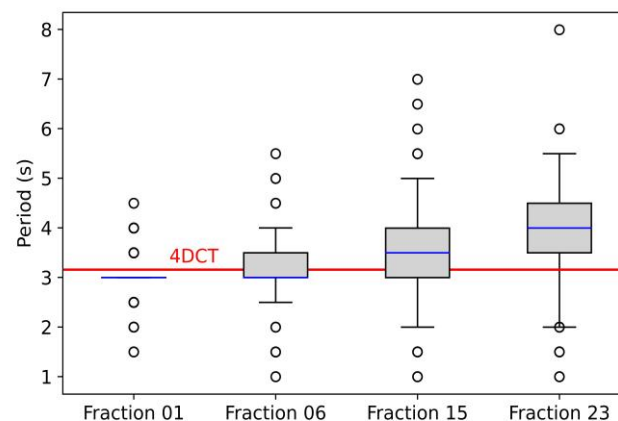
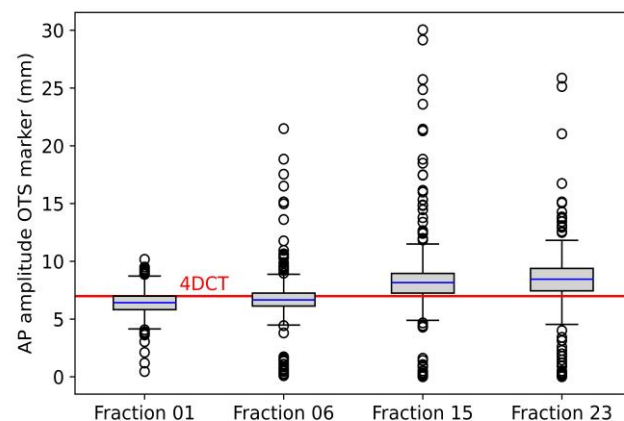


Case B
(Hodgkin's)



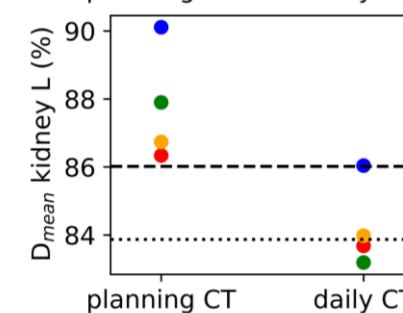
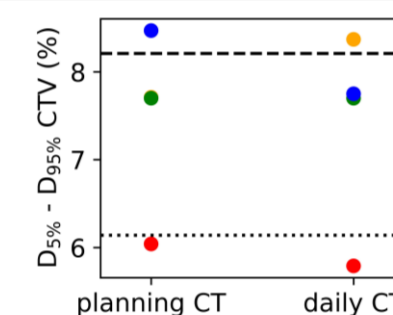
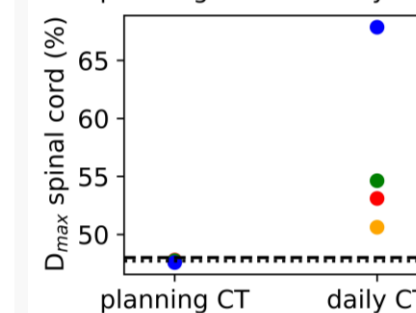
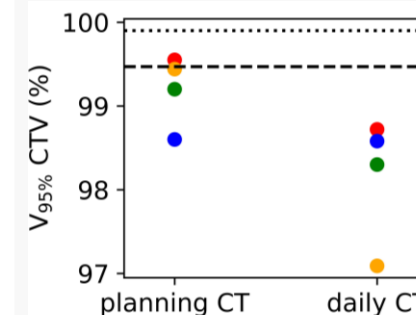
Case C
(malignant neoplasm)

Intra- and inter-fractional motion variability



Inter-fractional differences

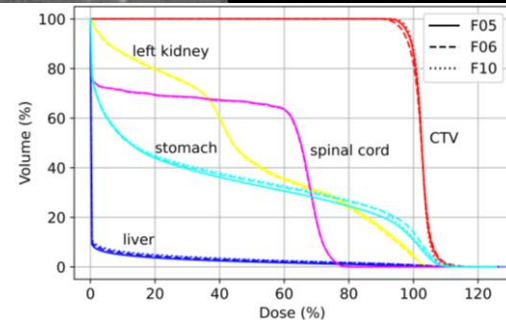
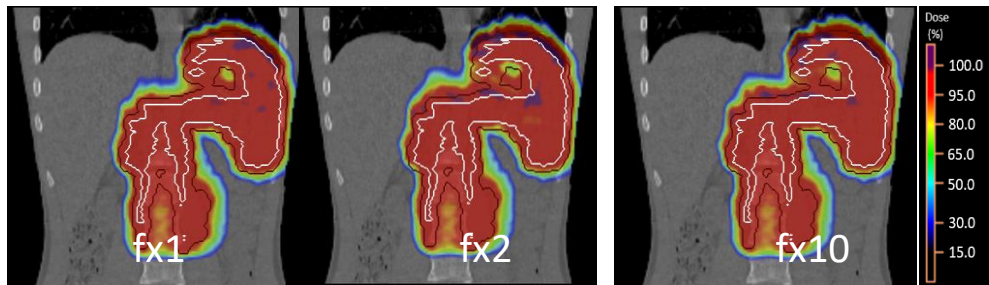
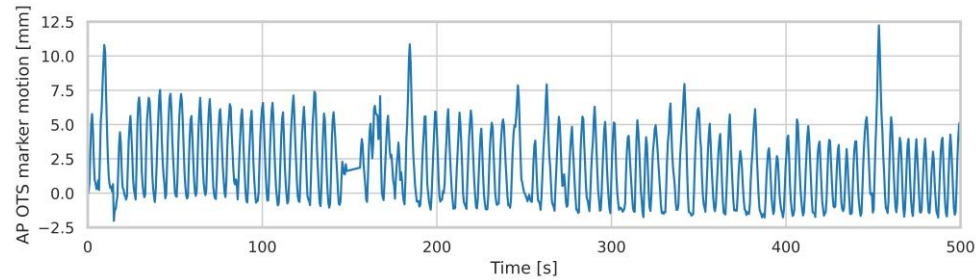
- up to 2.0% in CTV $V_{95\%}$
- up to 2.9% in $D_{5\%}-D_{95\%}$



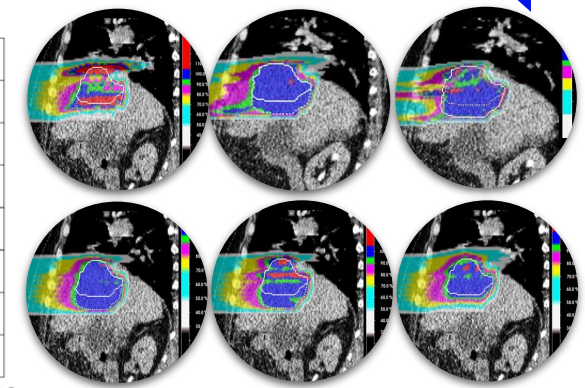
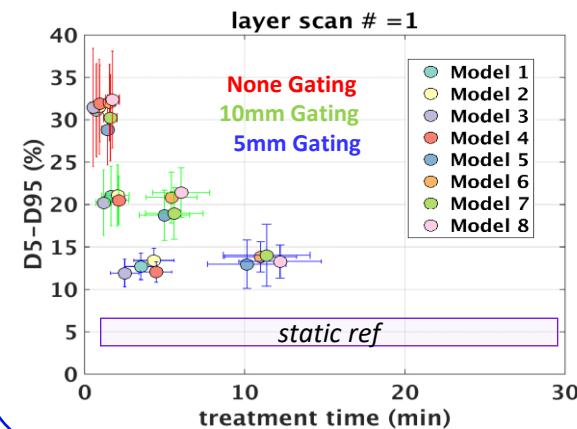
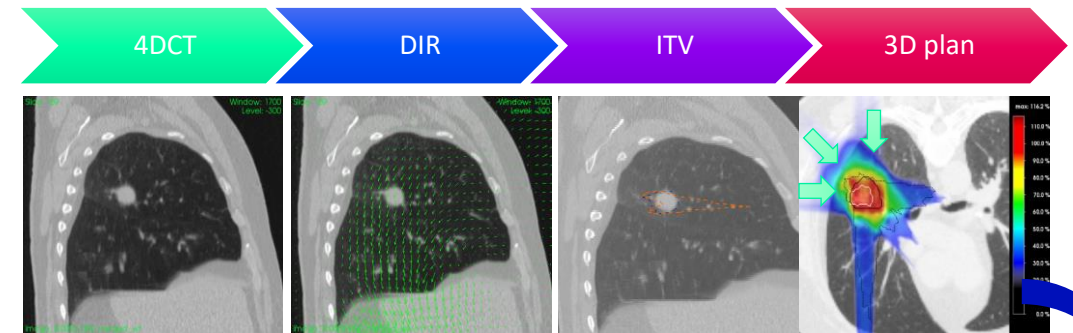
..... planning CT (static) Fraction 01 Fraction 15
 --- 4DCT (no gating) Fraction 06 Fraction 23

Joint efforts of perspective 4DDC and retrospective 4DDR

Retrospective fx 4D dose verification



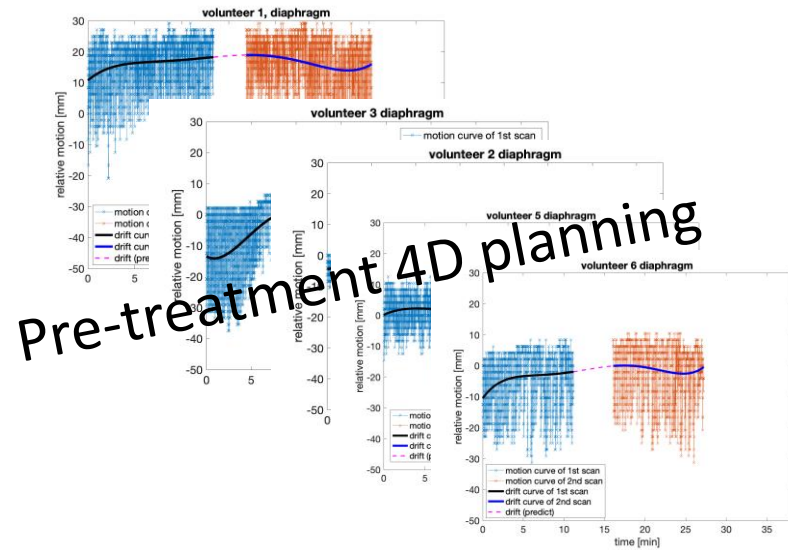
Perspective 4D evaluation framework



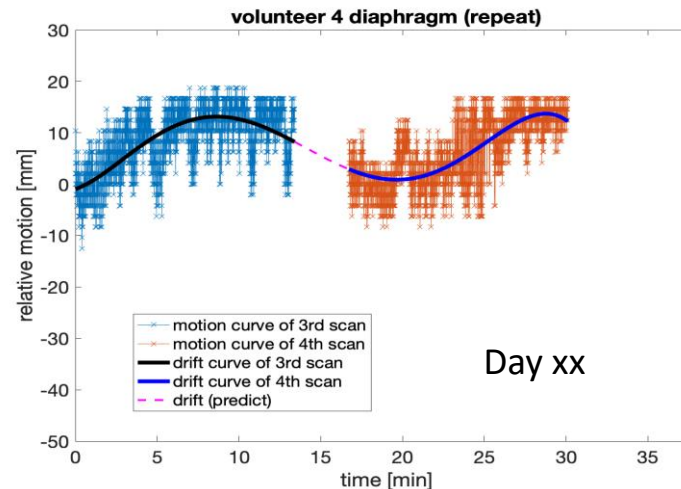
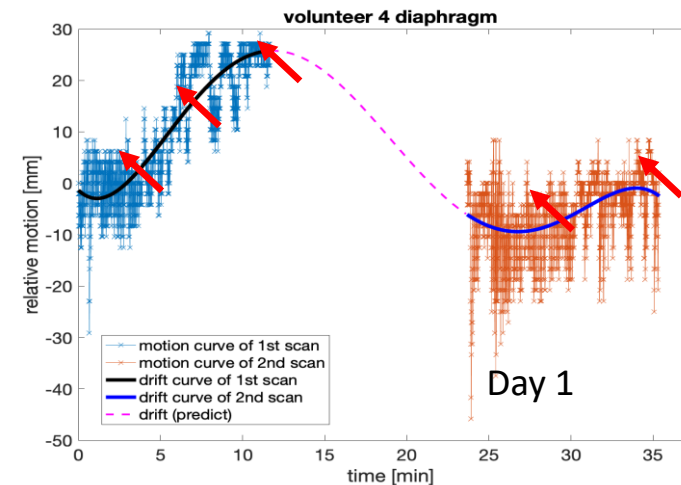
different potential RRMM

DAPT for 4D treatment – motion variability

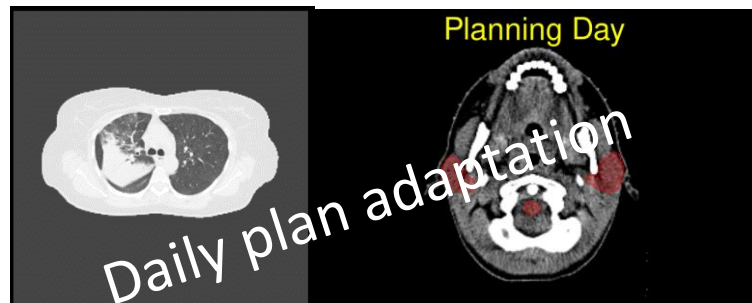
Patient specific motion characteristics



“variations” of the motion irregularity *inter-fractionally*



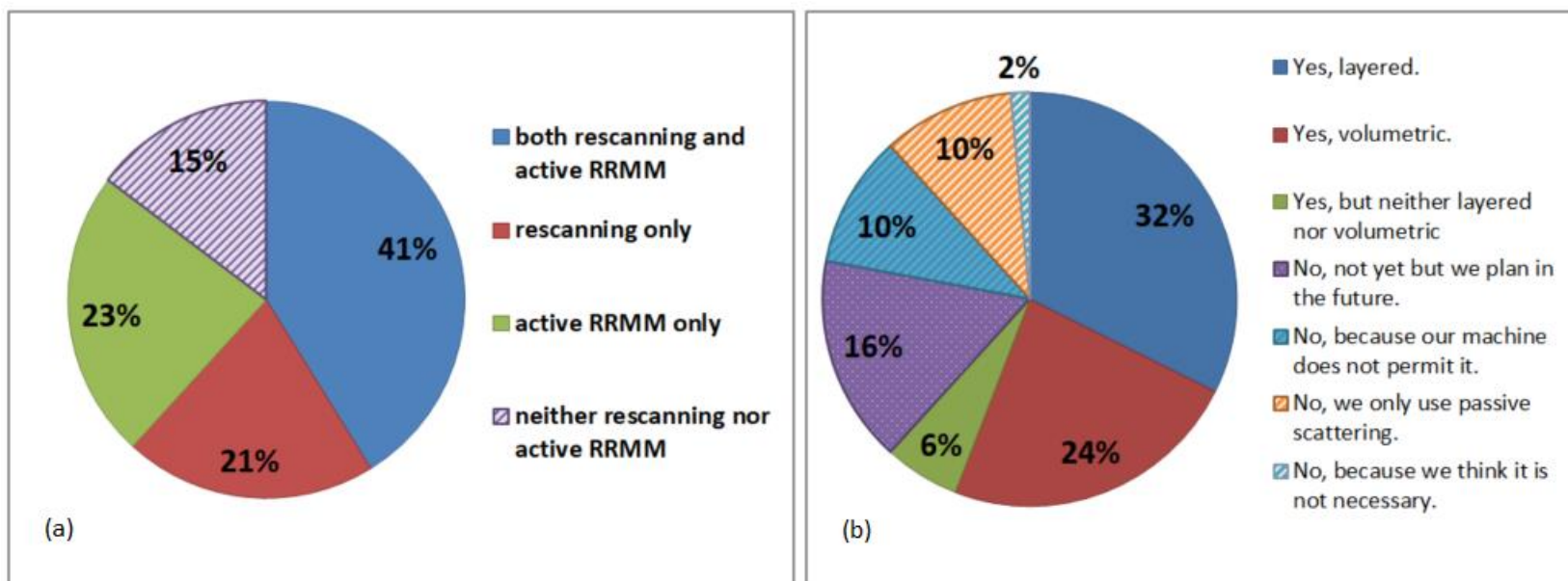
Anatomic variations during full treatment



Baseline can drift intra-fractional, which is not reproducible inter-fractionally

Current status of motion mitigation

RRMM implementation globally (N=68)



Status of rescanning application in clinics

Zhang Y, Trnkova P, Toshito T, Heijmen B, Richter C, Aznar M, Albertini F, Bolsi A, Daartz J, Bertholet J, Knopf A. A survey of practice patterns for real-time intrafractional motion management in particle therapy. Physics and Imaging in Radiation Oncology 2023 Apr 11;26:100439

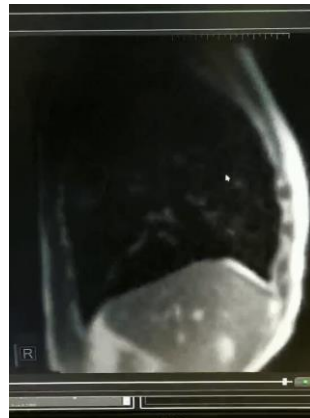
Summary of the most important conclusions from 3 round DELHI consensus analysis

VISION AND RECOMMENDATIONS

- Real-time motion management is needed for adaptive treatment of moving targets
 - Future real-time motion management should combine strategies according to the individual patient selection criteria
- Dosimetric deteriorations for both target and OARs are considered equally important
 - The rescanning parameters should be evaluated and optimized for an individual patient
 - The selection criteria of active RRMM should be based on pre-treatment motion characteristics
 - The uncertainty of the motion model should be considered in the 4D evaluation
 - The pre-treatment 4D plan evaluation should be recorded for multi-centre clinical trial
- 4D dose calculation including uncertainty evaluation, is the top required feature on clinical software in the next 2 years

Zhang Y, Trnkova P, Toshito T, Heijmen B, Richter C, Aznar M, Albertini F, Bolsi A, Daartz J, Bertholet J, Knopf A. A survey of practice patterns for real-time intrafractional motion management in particle therapy. *Physics and Imaging in Radiation Oncology* 2023 Apr 11;26:100439

Go beyond/exceed MR guided photon therapy



Current mature solution for
MR linear accelerator



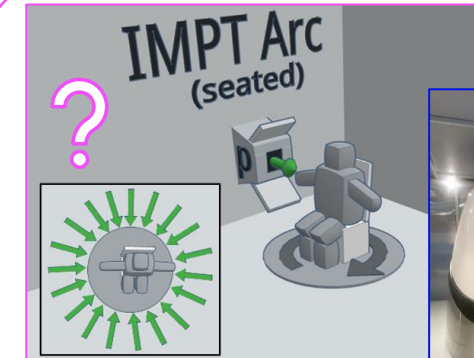
cost²



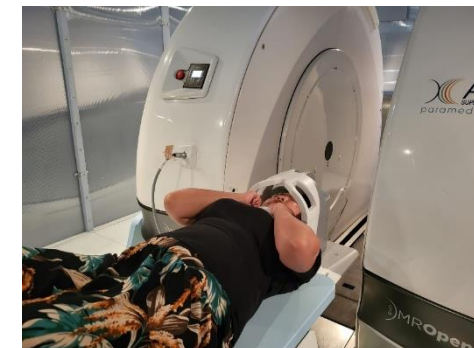
complex²



Potential conceptual designs for
MR-guided proton machine

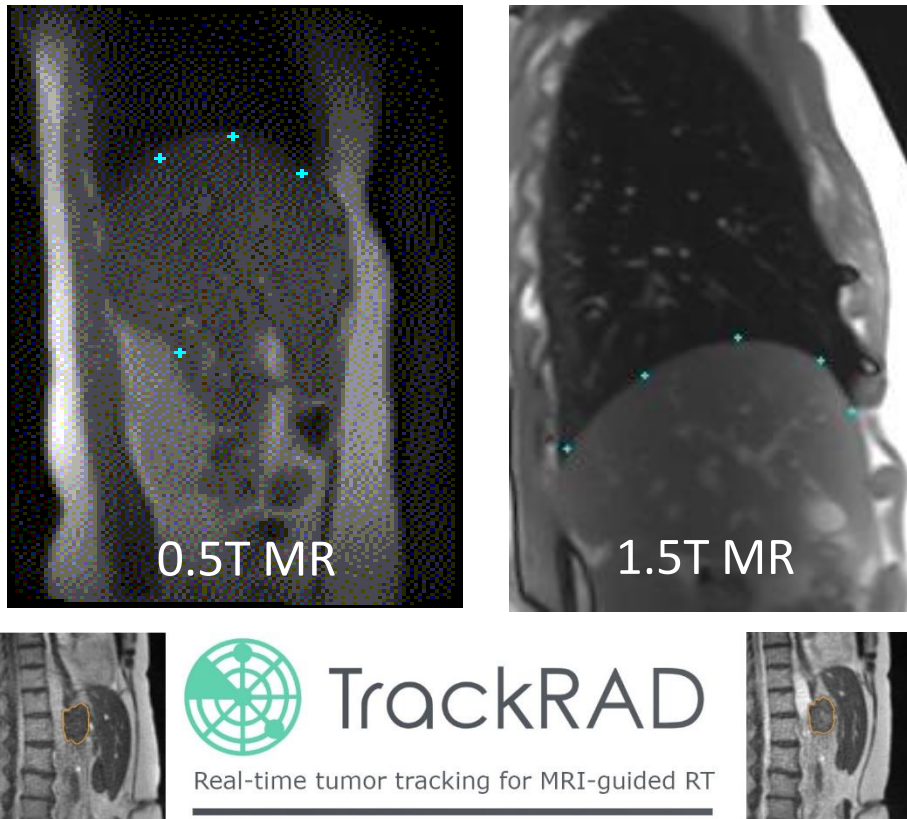


Enable online MR for proton
without anti-democratization

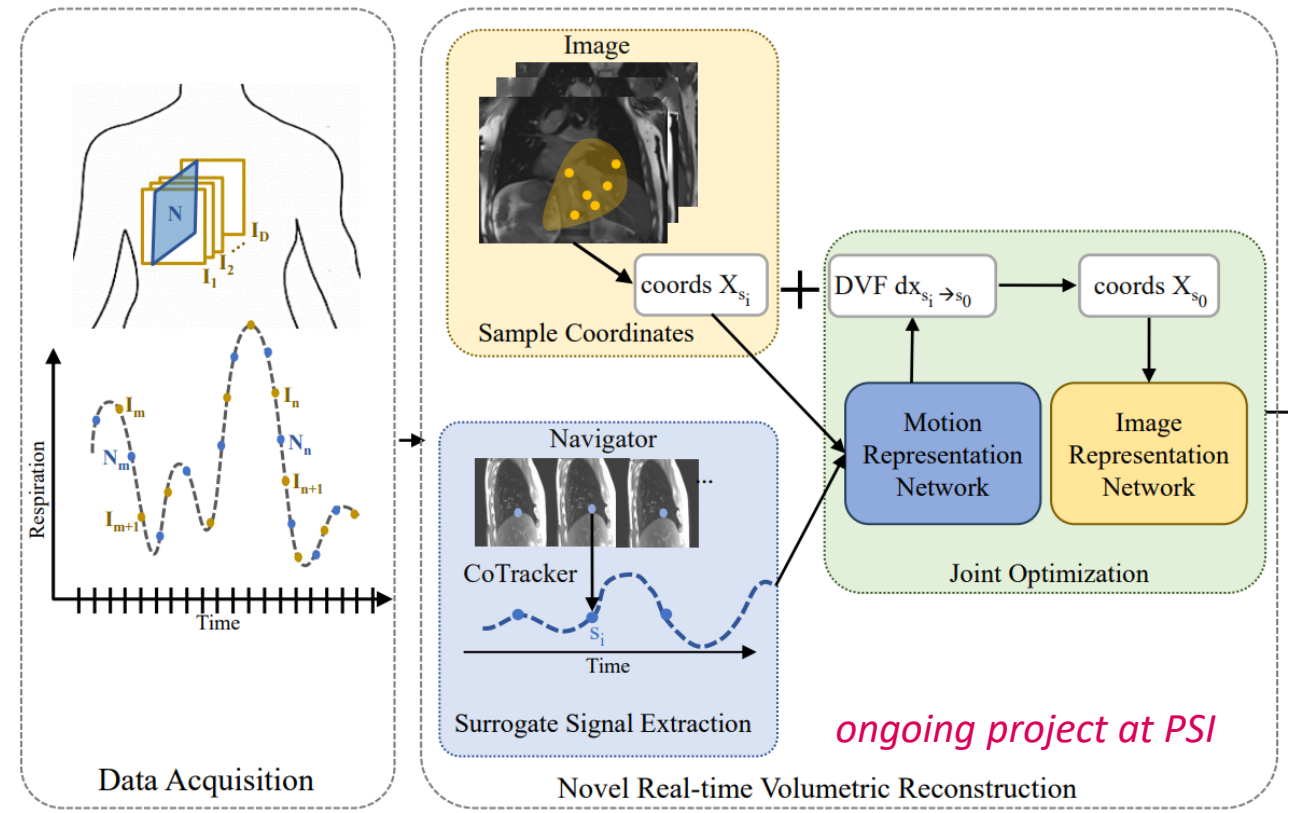


Real-time 4DMRI based online motion tracking

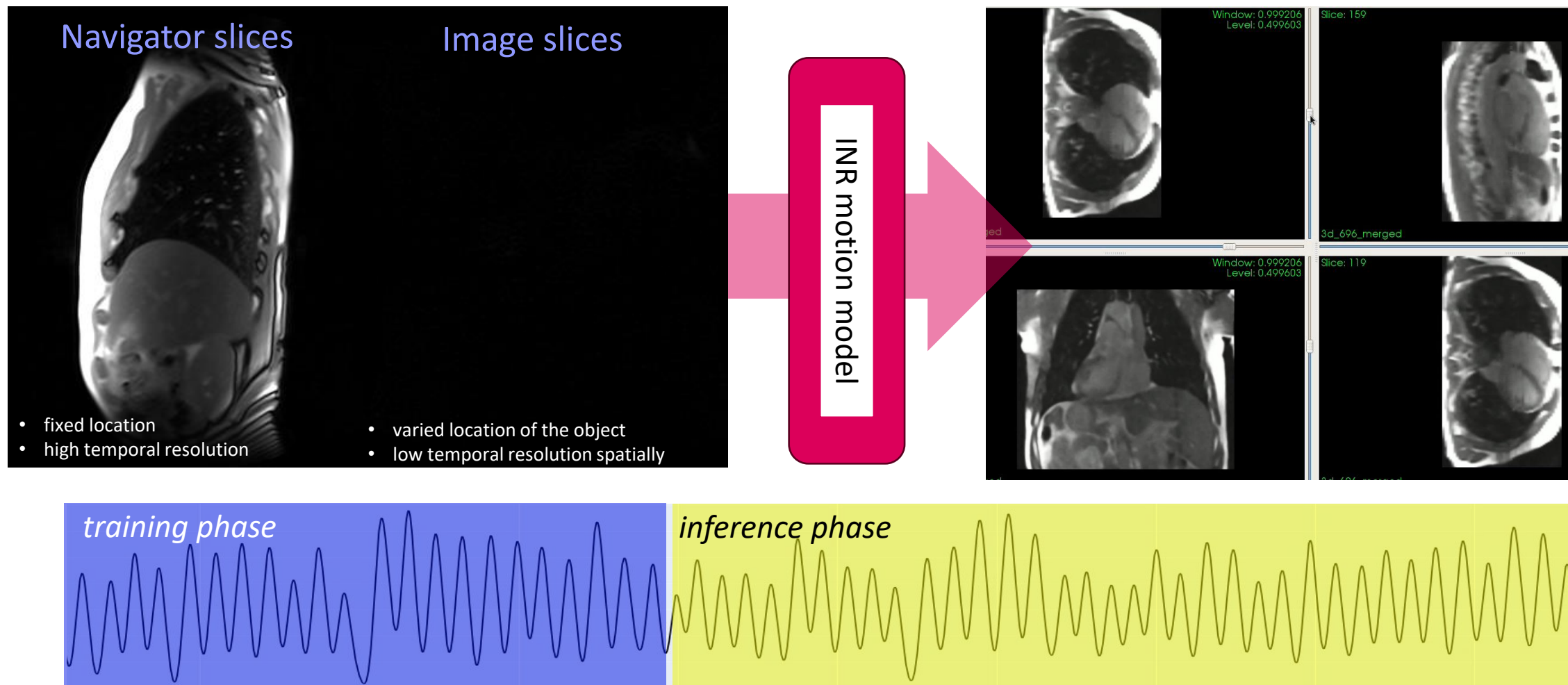
Real-time 2D motion tracking using transformer-based foundation model



4DMRI reconstruction and concurrent motion tracking using *Implicit Neural Representation*



Real-time 4DMRI for online motion tracking



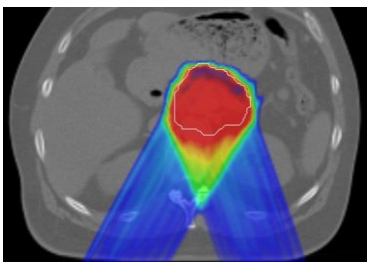
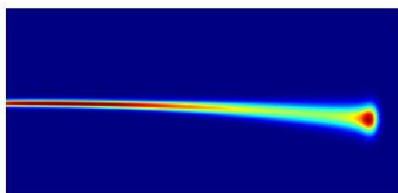
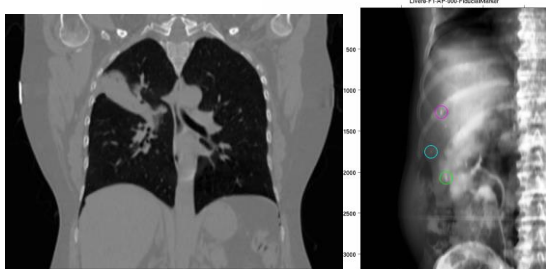
MRgPT: Next-generation 4D treatment and image guidance



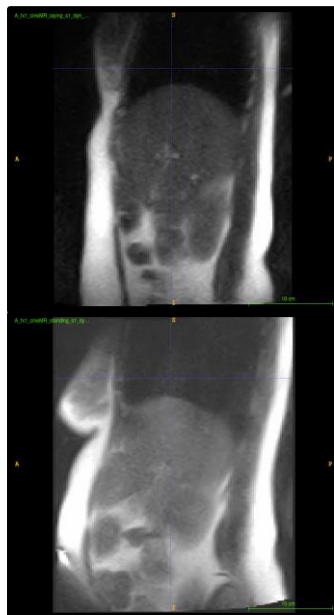
High soft-tissue contrast
No radiation image dose
Real-time imaging

Onboard MR-guided proton therapy Upright treatment

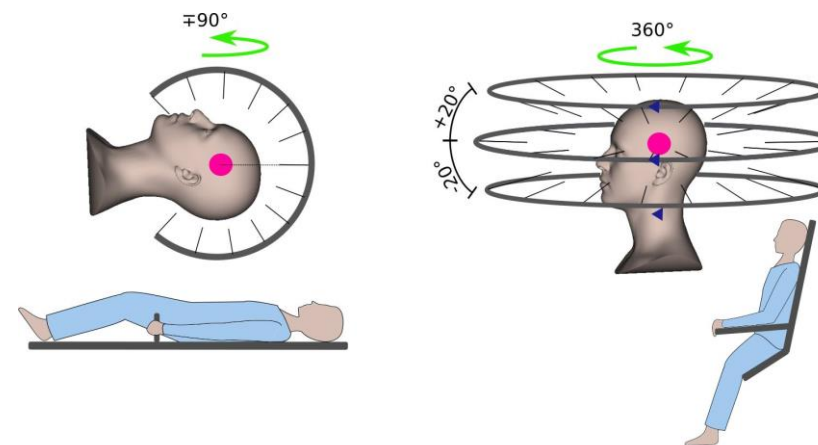
Reduced facility cost
Increase clinical advantage
Possibility for advanced IGRT



proton dose calculation under magnetic field

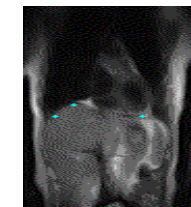
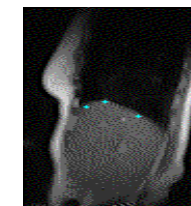
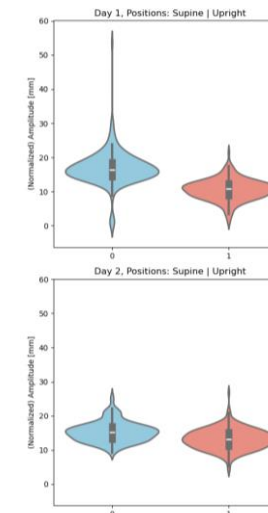
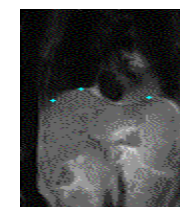
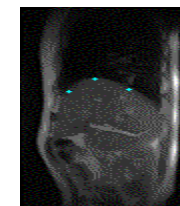


MR-guided upright proton therapy



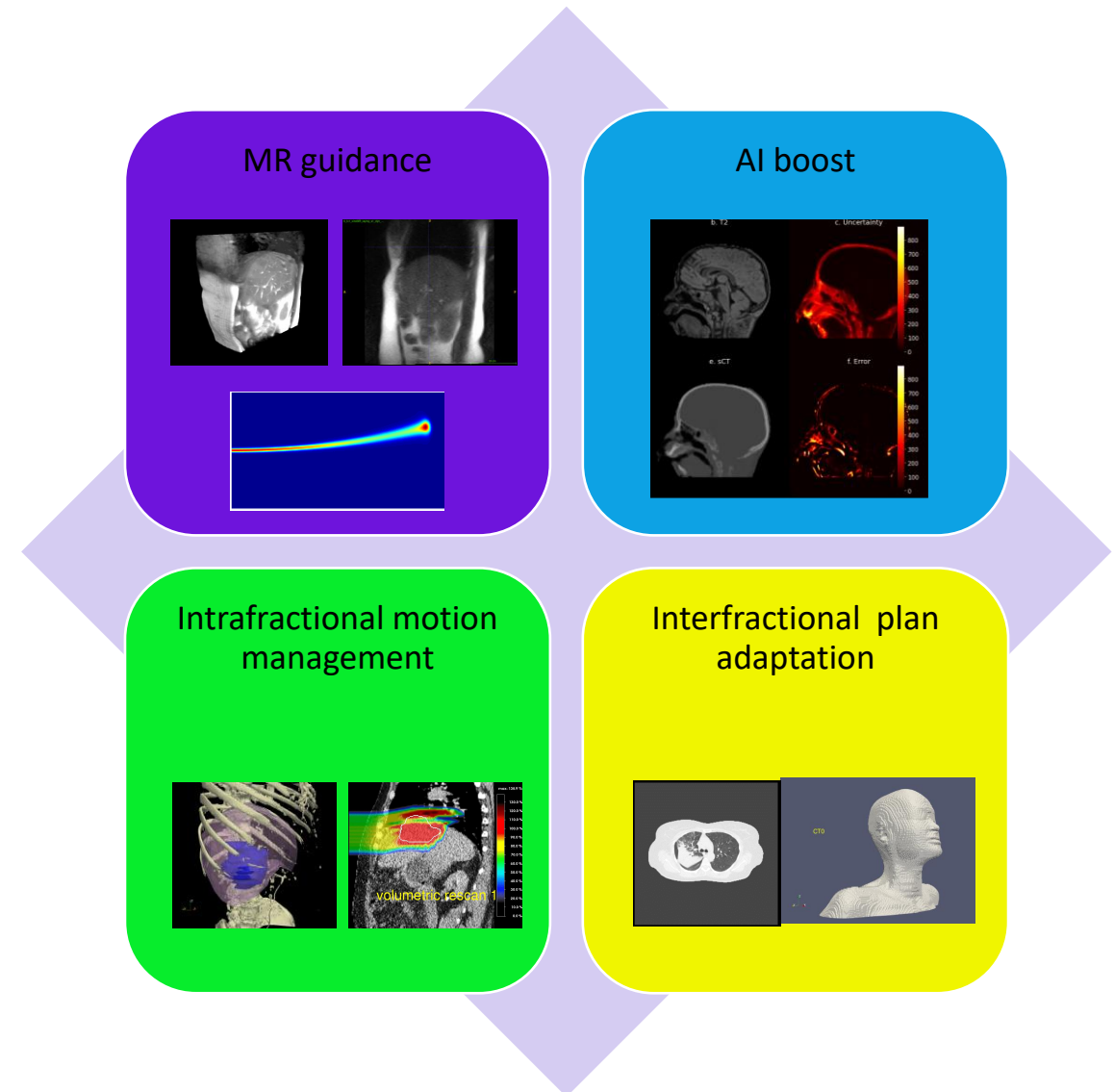
Recumbent

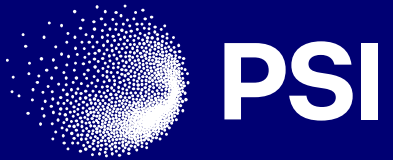
Upright



Conclusion and outlooks

- Intra- and inter-fraction motions for PBS proton are significant but can be evaluated prospectively or retrospectively using 4D dose calculation, image guidance, motion model, daily plan adaptation
- Joint impact of intra- and inter-fraction motion effects must be emphasized and mitigated in the next five years
- MR should play a more critical role in further proton therapy, offline, online or in real-time.
- Combining upright treatment with open MR would be a feasible solution for onboard MRgPT
- Advanced image processing techniques based on AI will significantly improve the efficiency of proton therapy workflow for the ultimate goal towards true real-time adaption





Thank you!

