



# New applications of positron-emitting nuclei in medical imaging and treatment at GSI

**Sivaji Purushothaman**

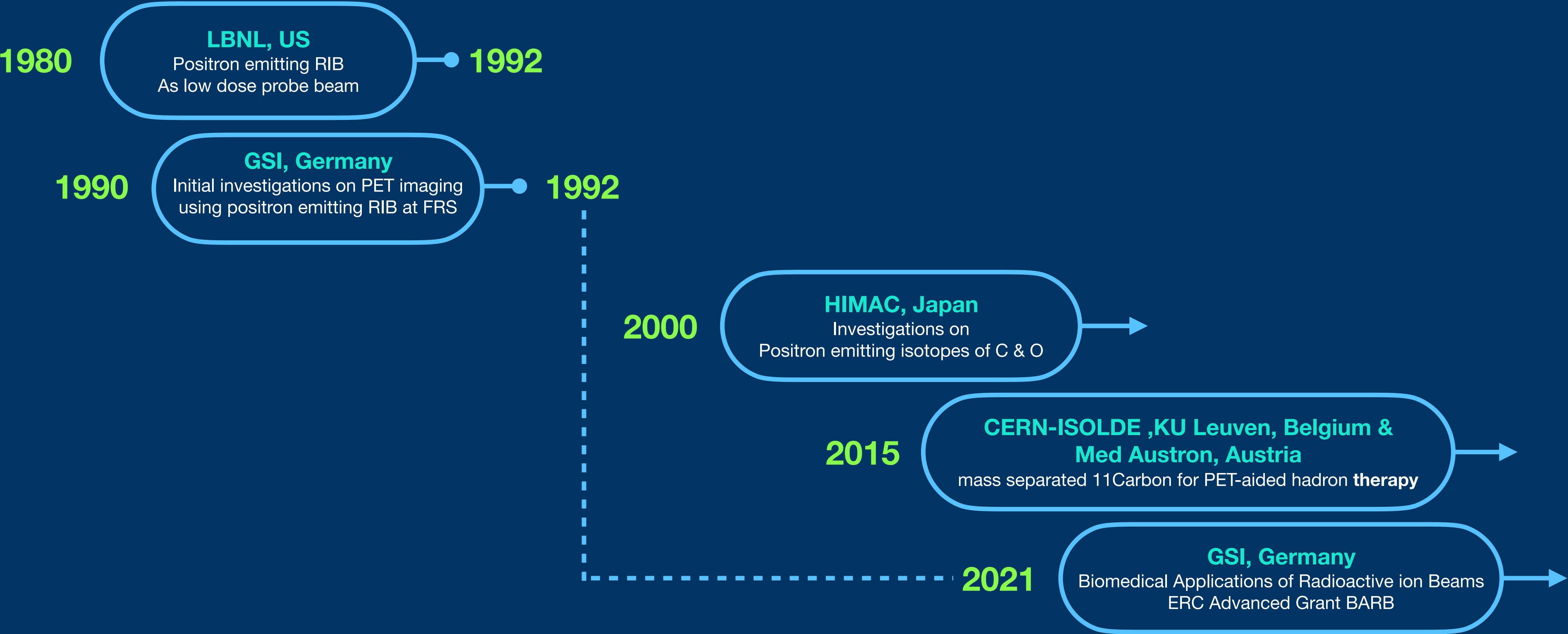
for Super-FRS Experiment Collaboration and BARB collaboration

NUSTAR Annual Meeting 2024



# RIB for hadron therapy

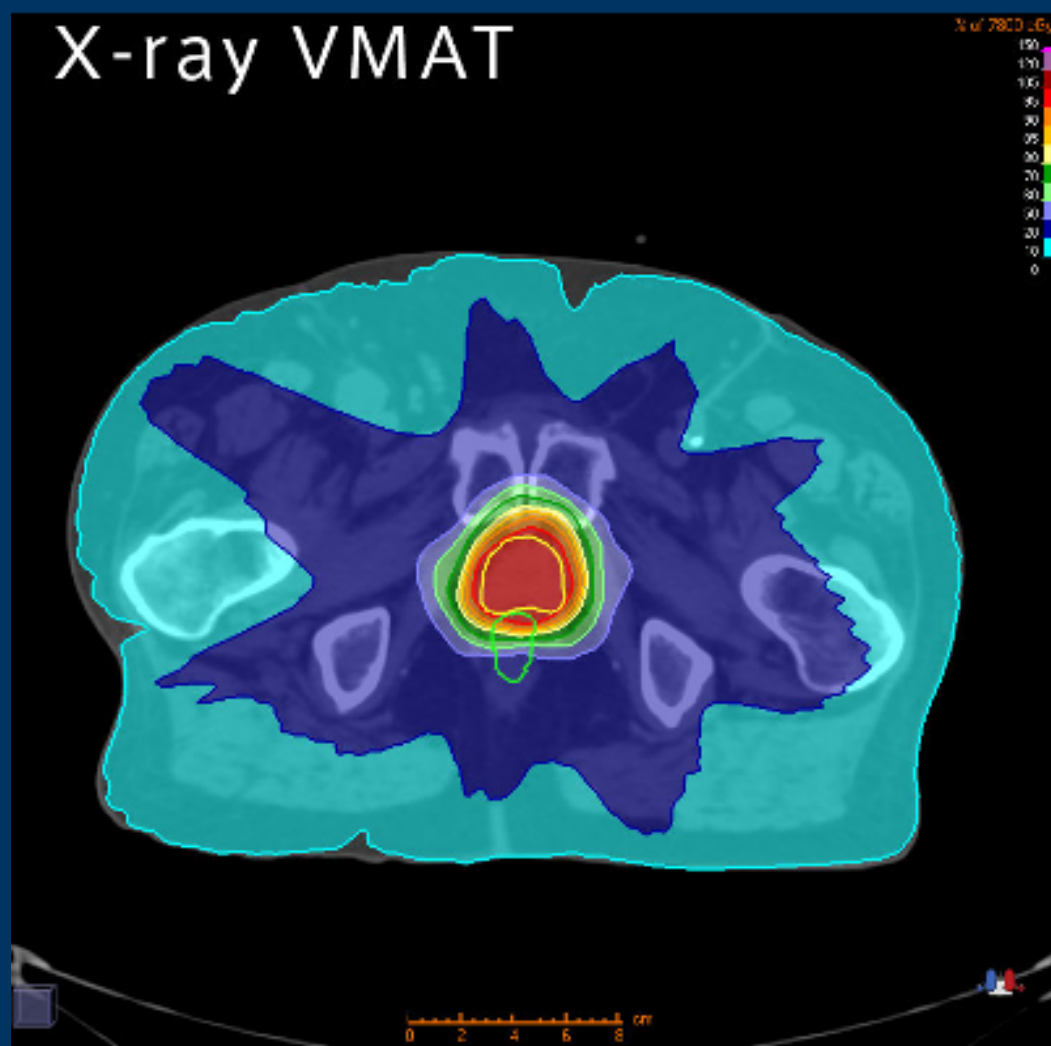
## Range verification with RIB of positron emitters and PET



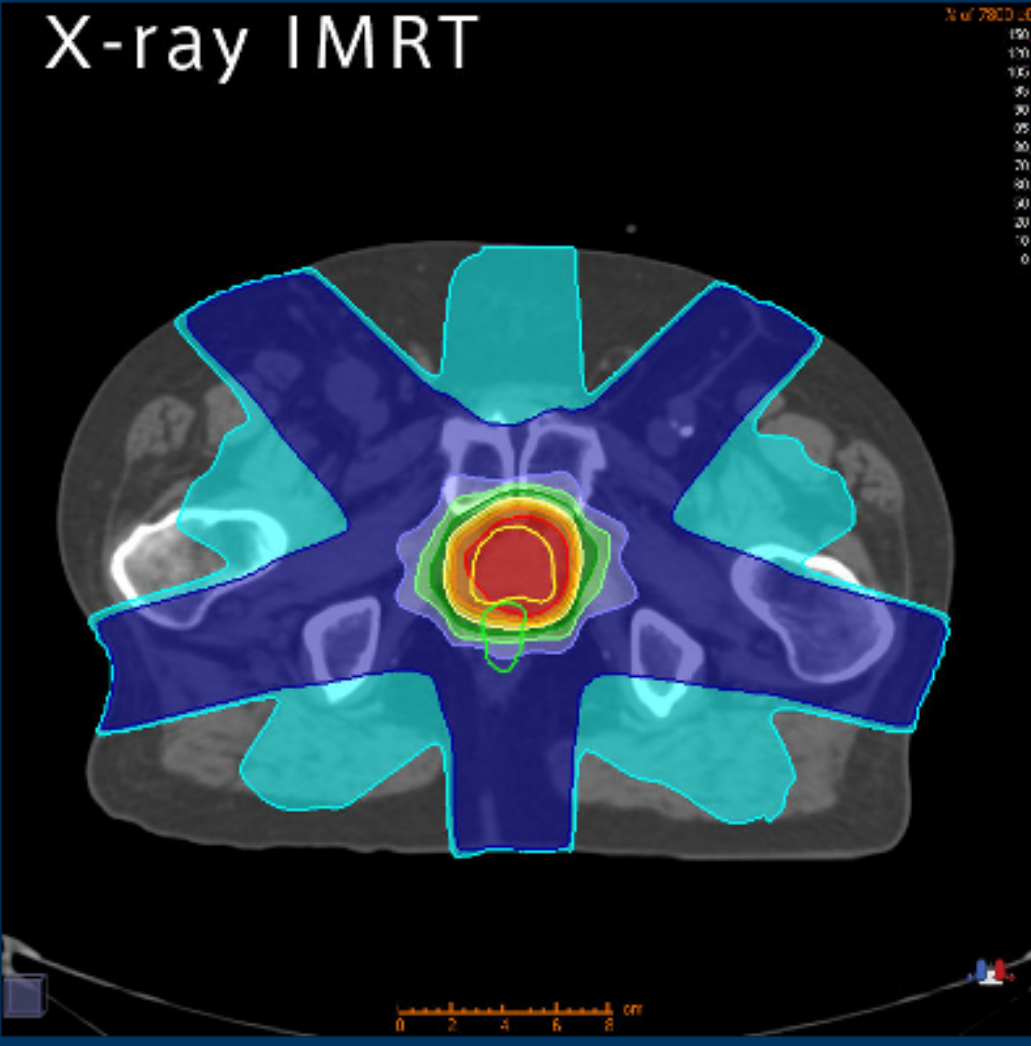
# Ion beam therapy : Benefits

## Photon Therapy

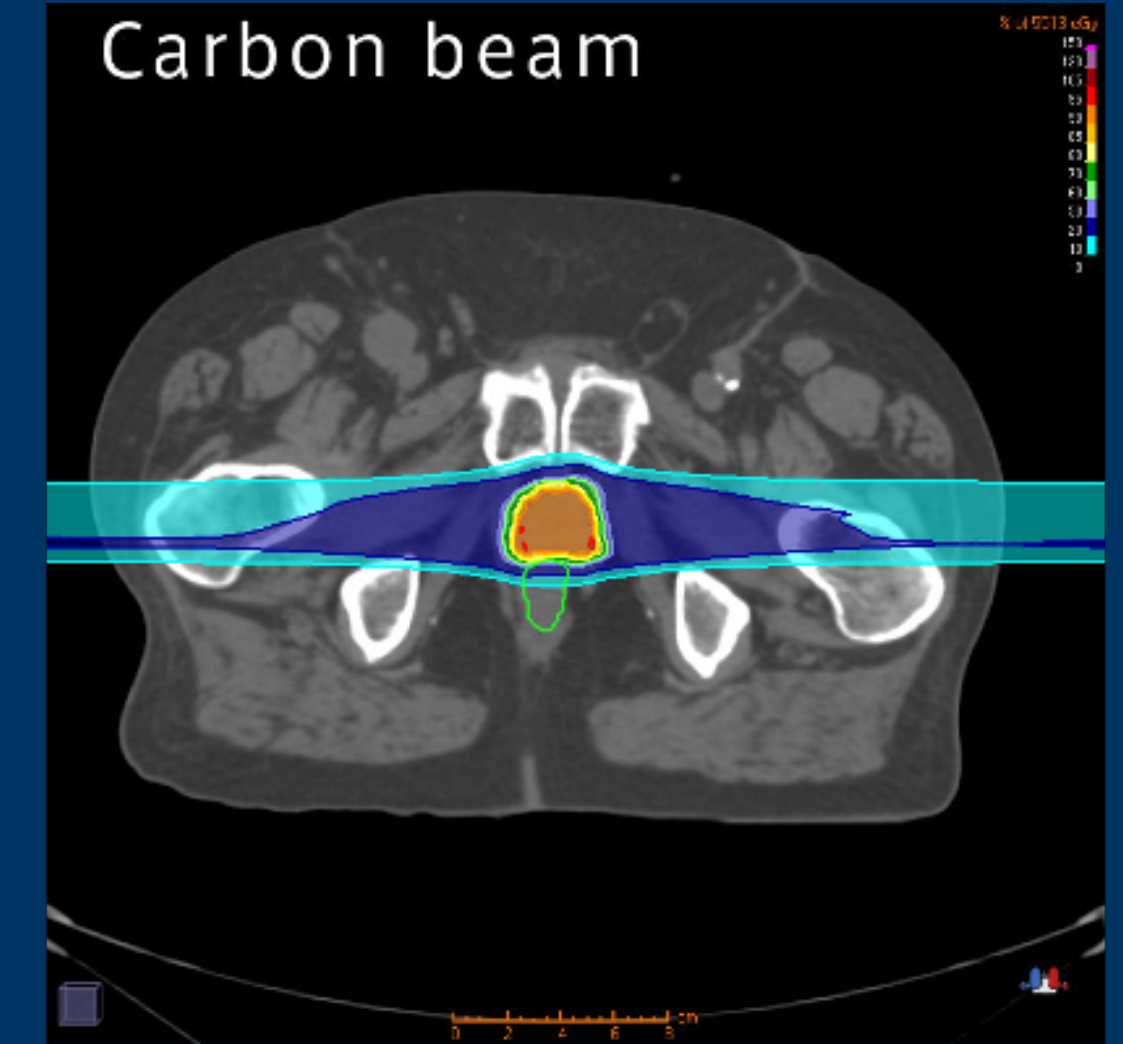
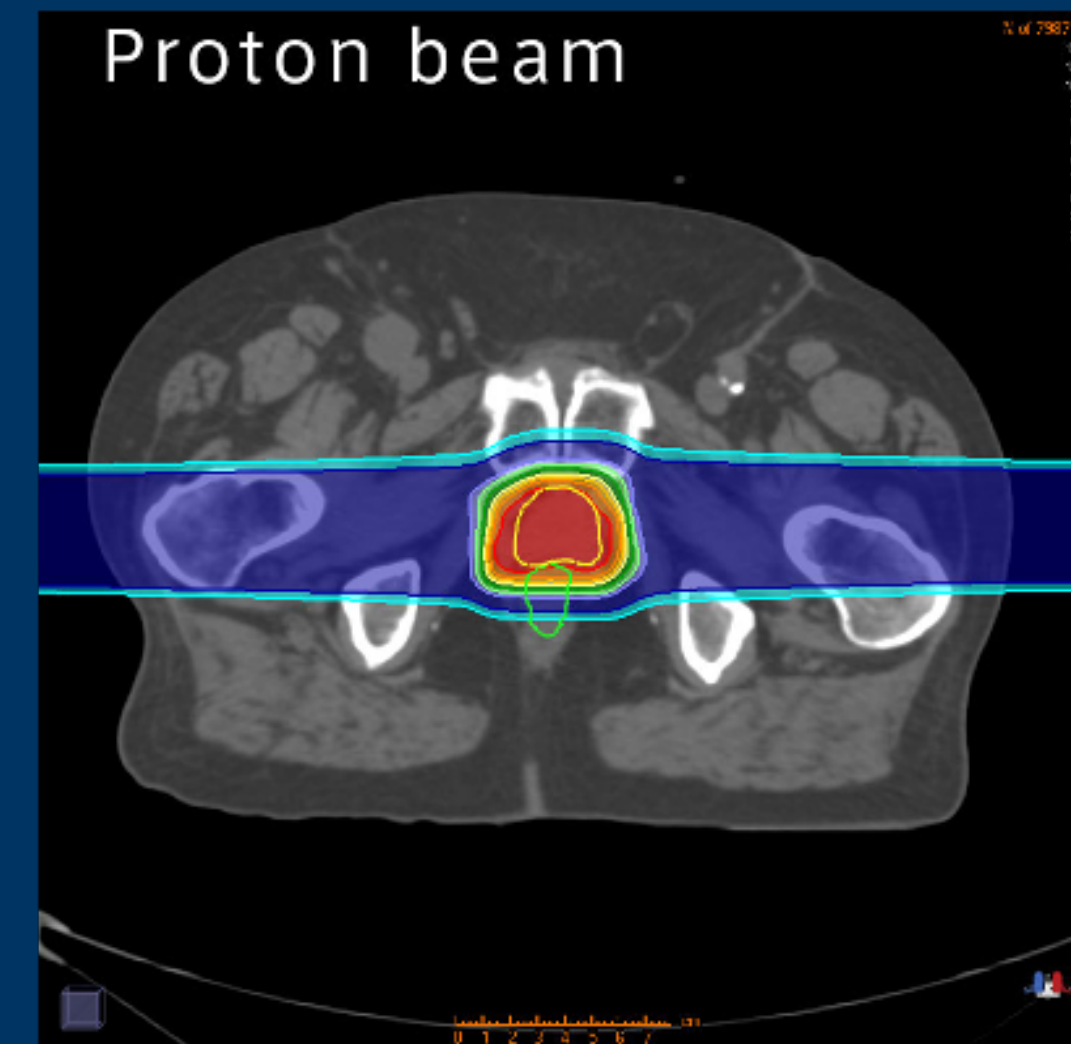
Volumetric Modulated Arc Therapy



Intensity-modulated radiotherapy



## Hadron Therapy



- High tumour dose, normal tissue sparing
- Effective for radio-resistant tumours
- Effective against hypoxic tumour cells

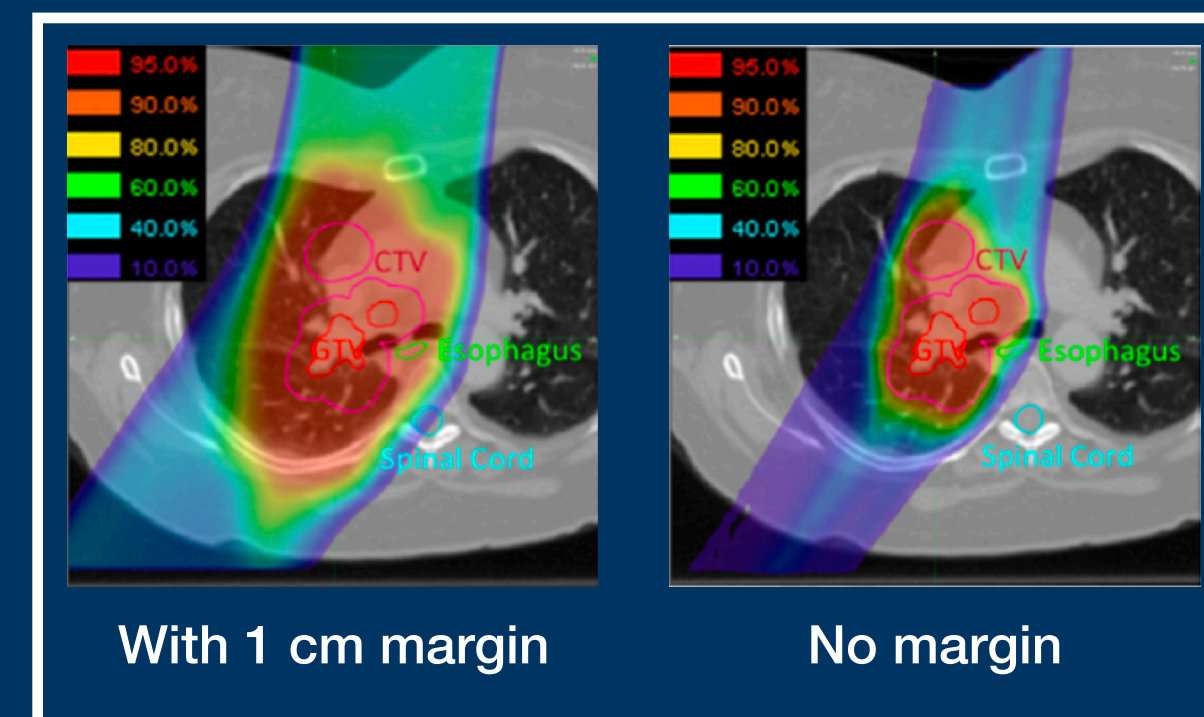
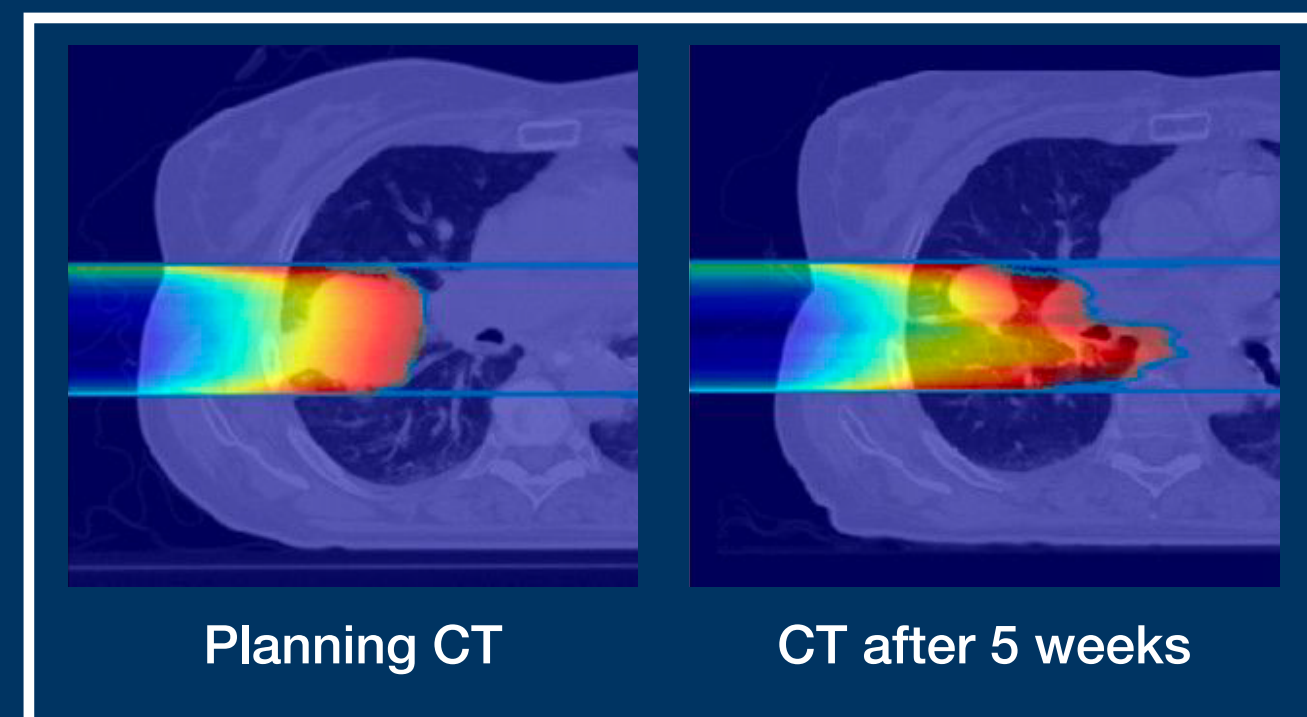


# Ion beam therapy : Challenges

## Range uncertainties

**Highly conformal ► Low tolerance for treatment planning error**

- Inherent uncertainties in the conversion from X-ray CT data to particle range
- Anatomical changes
- Quality of the CT
- Daily errors: patient setup and alignment,...



Typical uncertainties assumed in robust treatment planning for  $^{12}\text{C}$  ion therapy

**Setup uncertainty of  $\pm 3 \text{ mm}$   $\pm 2\%$  of range**



# Range uncertainties: Way forward

## Tumour tracking & Treatment verification

Tumour tracking

4DCT

Beam tracking

...

### Radiotherapy with positron emitters

Range verification with RIB of positron emitters and PET

- Off-line PET dosimetry
- In-beam PET dosimetry
- Prompt radiation measurement

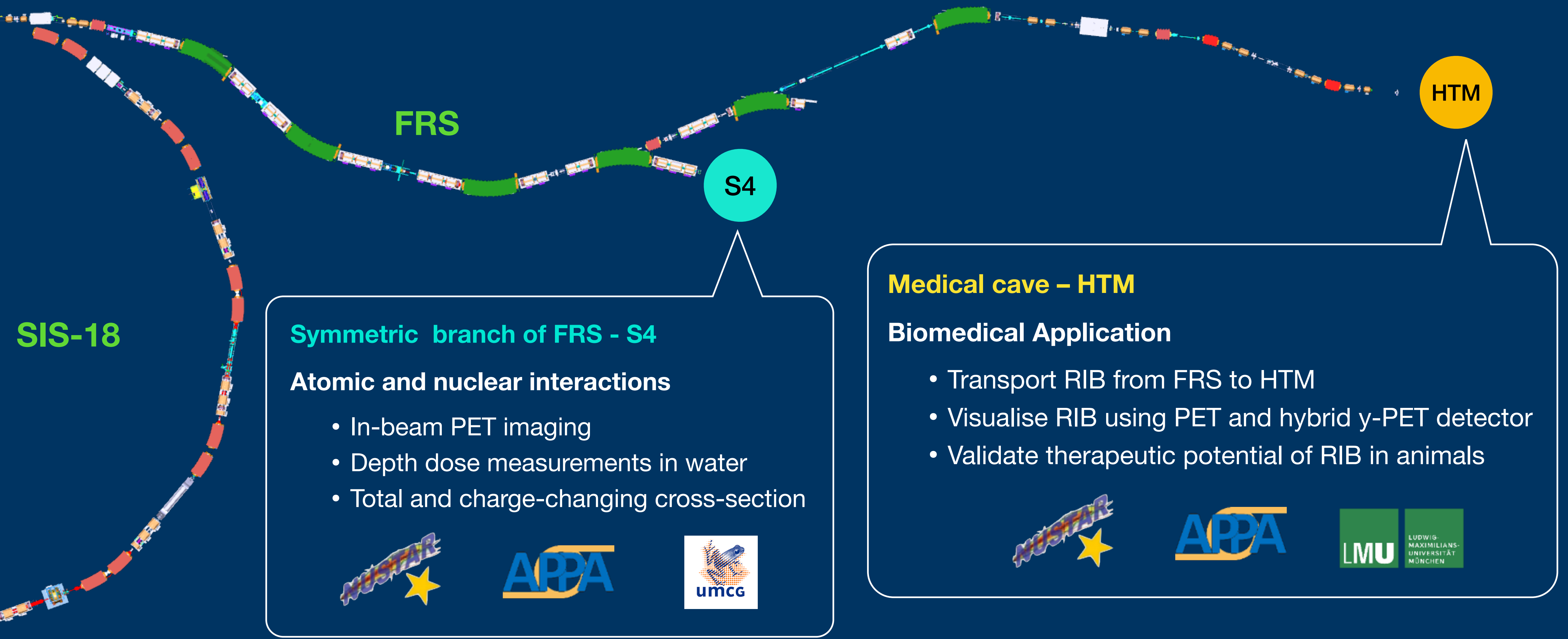


**Biomedical Applications of Radioactive ion Beams**  
**ERC Advanced Grant**

PI: Prof Marco Durante, Co-PI: Prof. Katia Parodi

# BARB experiments with RIB

## Positron emitting beams



# Quasi-real-time range Monitoring

Which is the best positron emitting therapy beam

## Required qualities

### Range verification

- Achieved with the lowest possible dose
- As early as possible

### Availability of therapeutic-quality beam

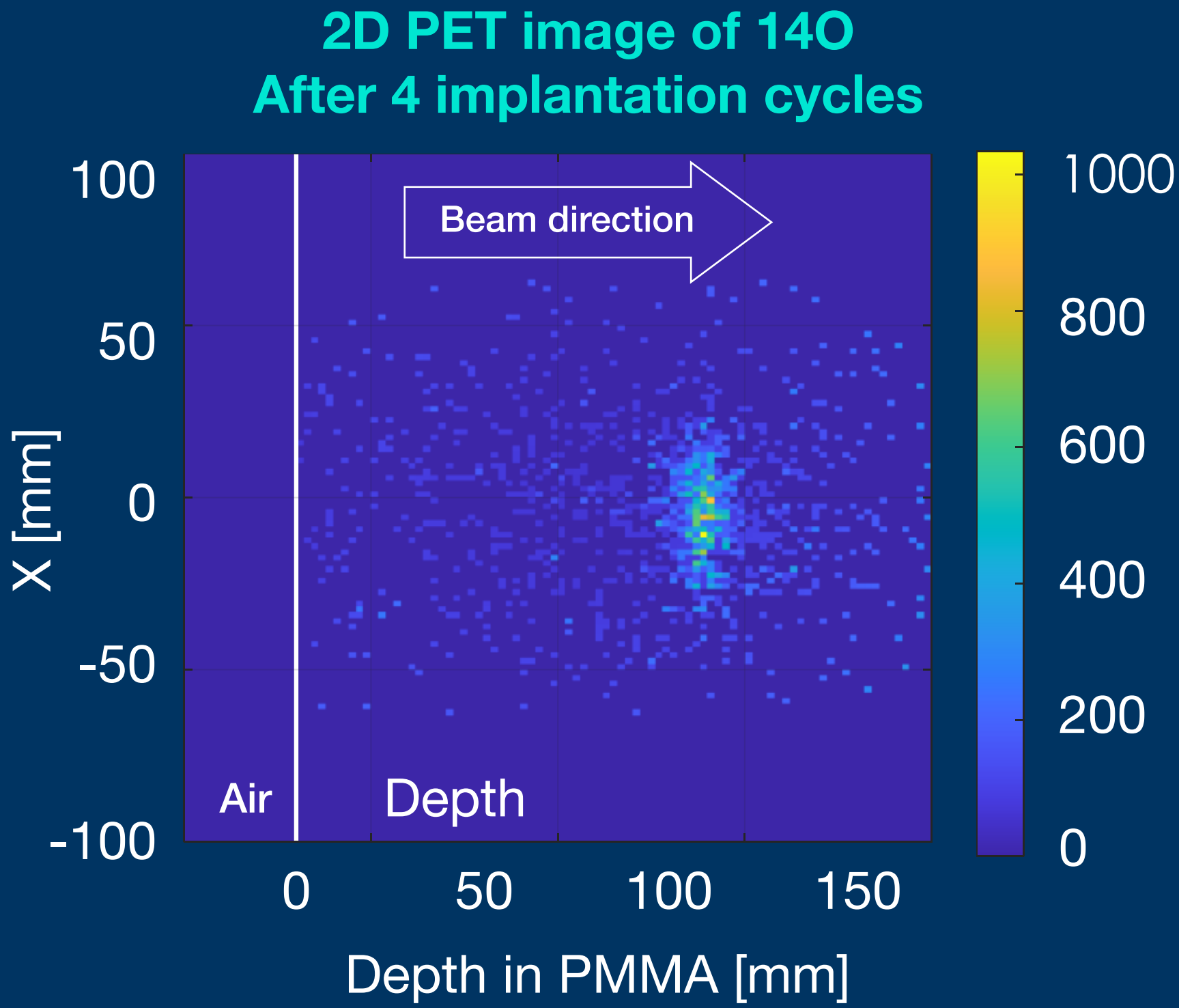
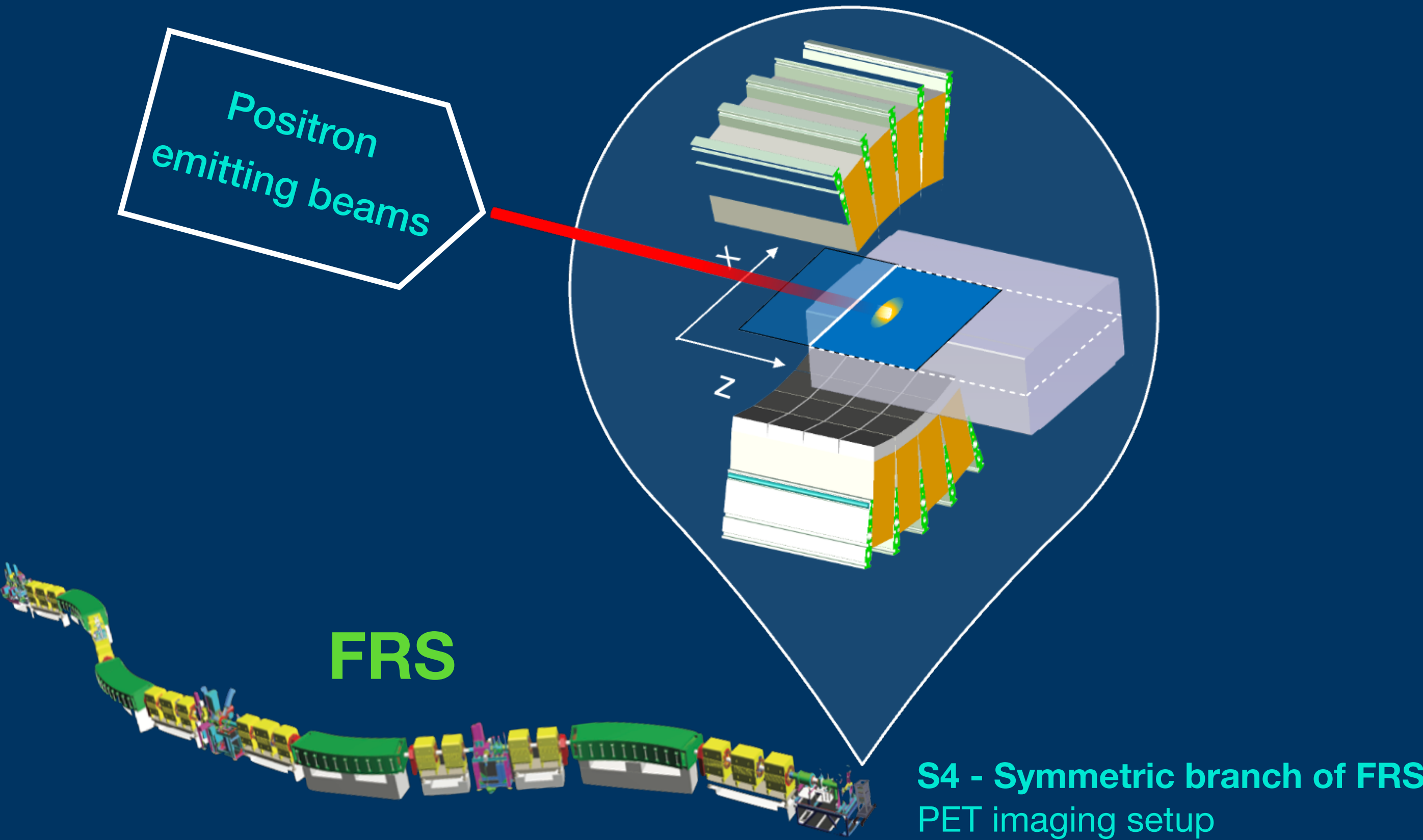
- Intensity
- Purity





# PET imaging at FRS

## Quasi-real-time range Monitoring



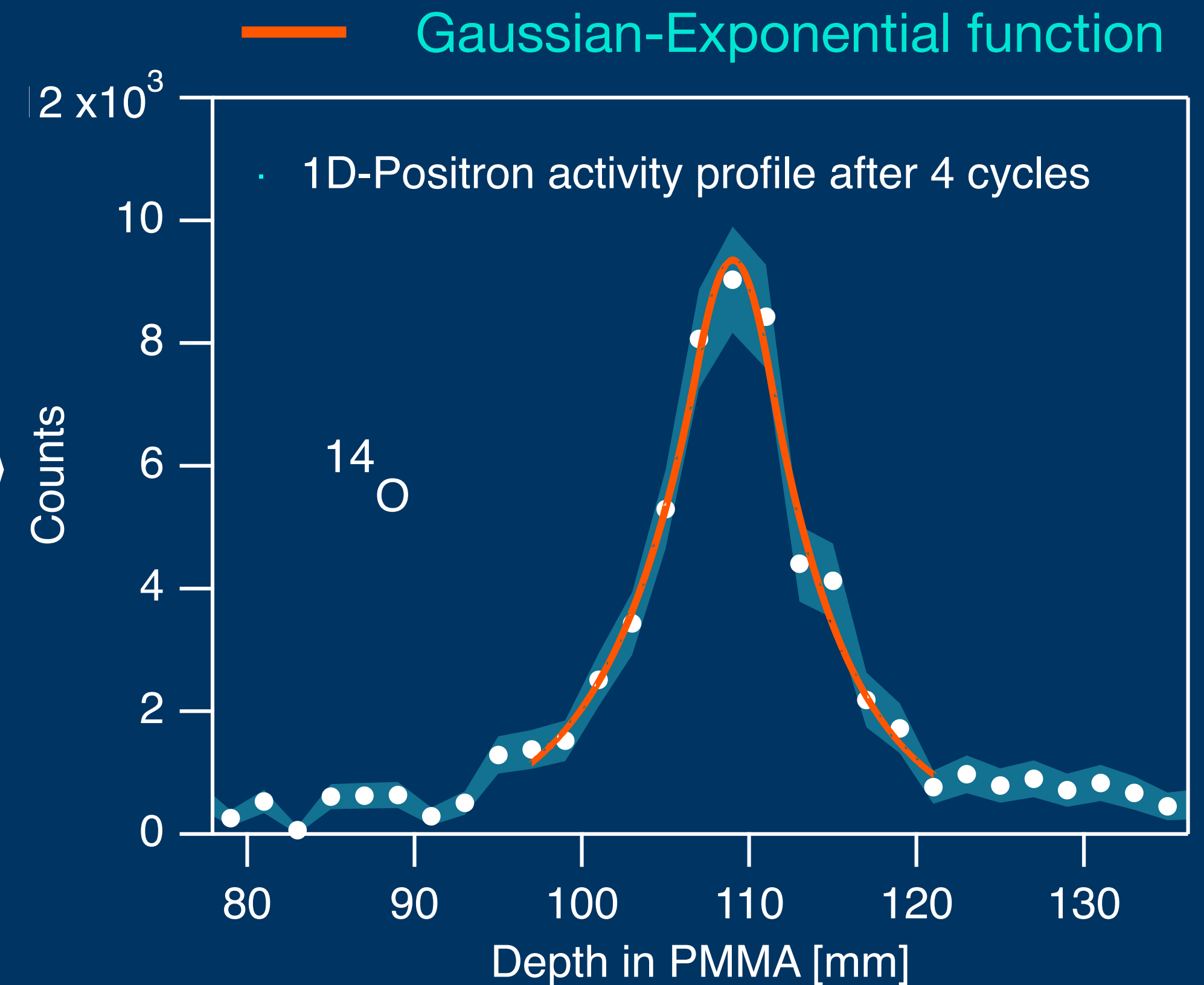
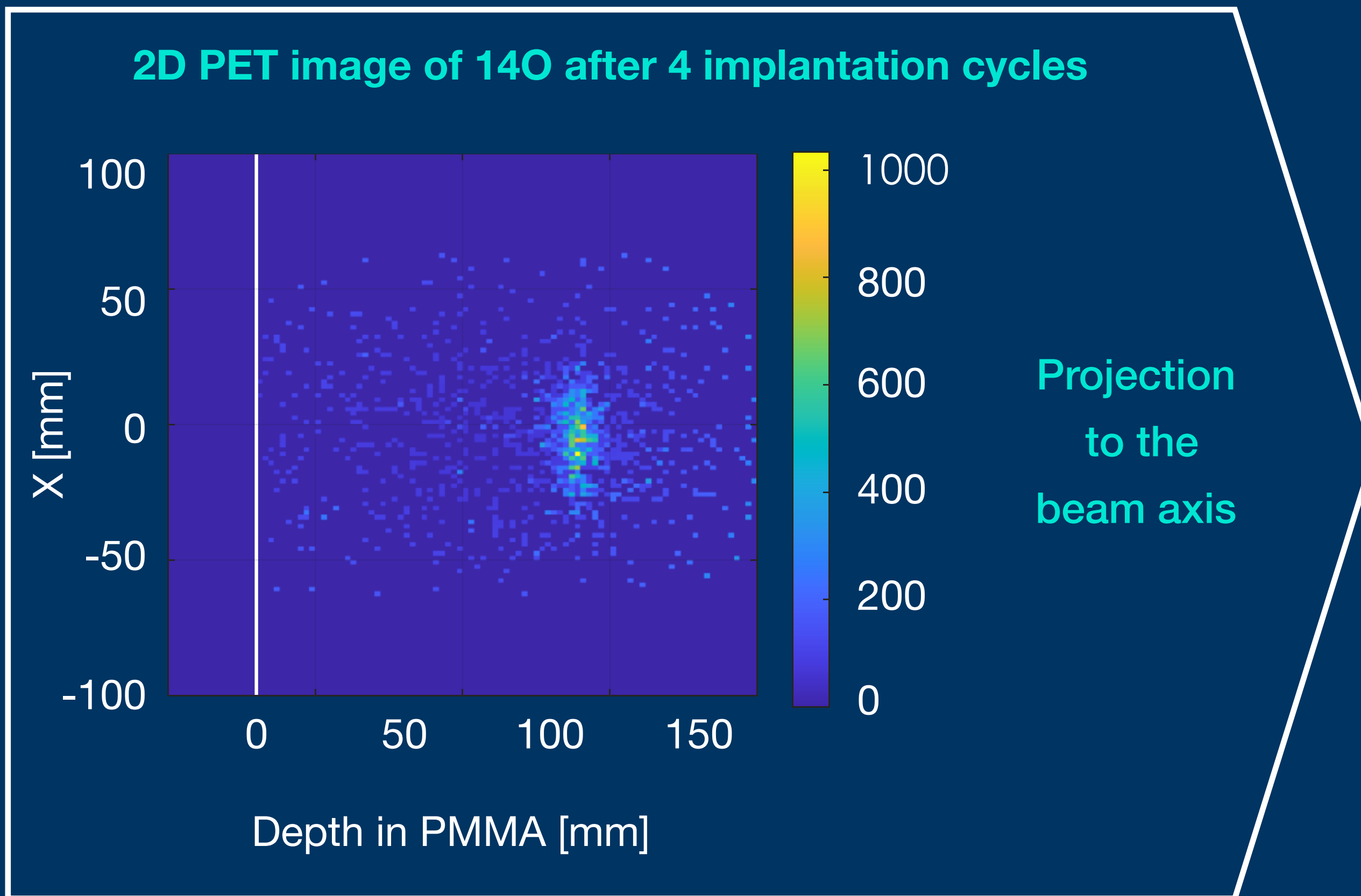
1/6th of a Siemens Biograph  
mCT clinical scanner

Peter Dendooven



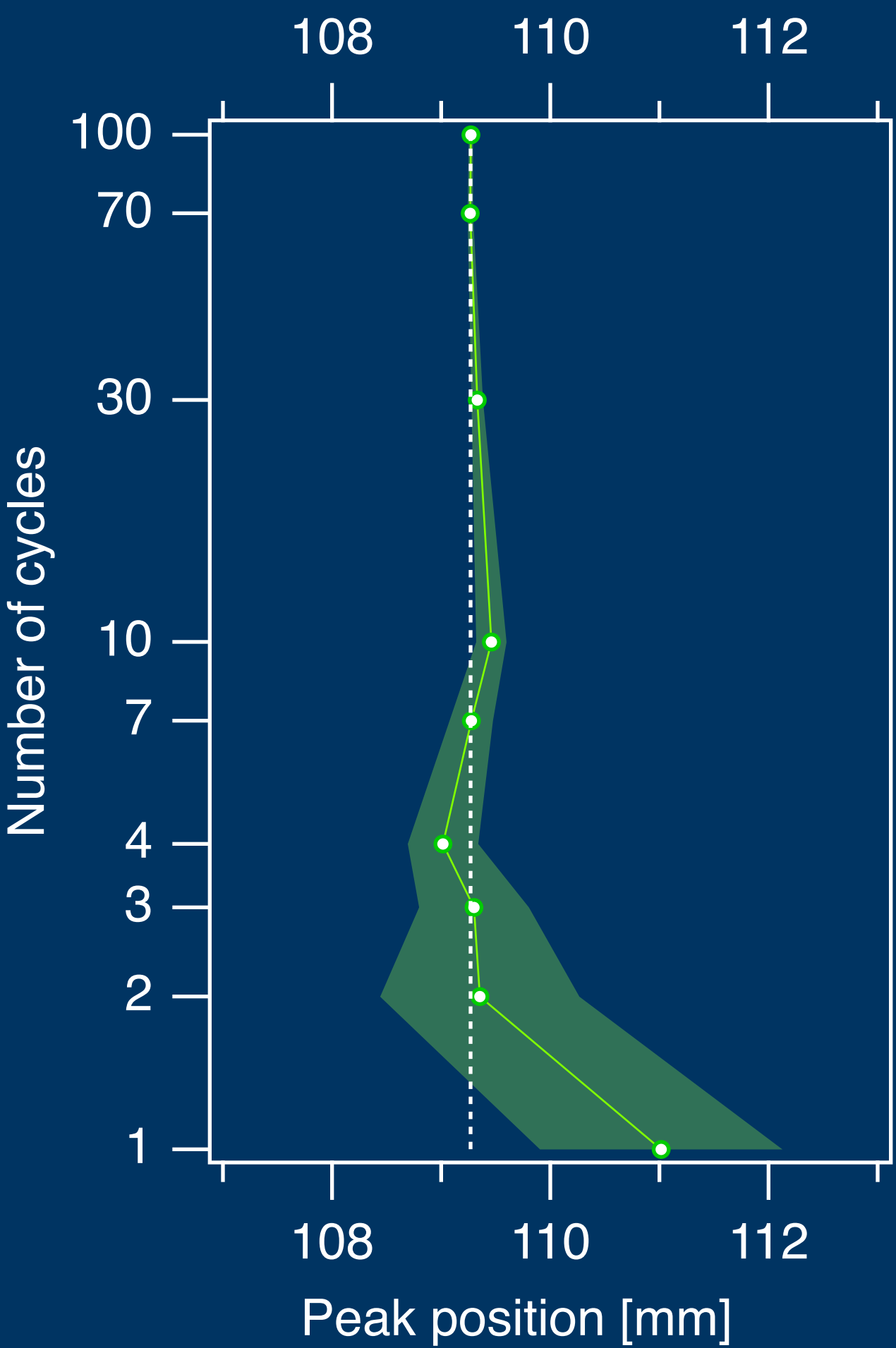
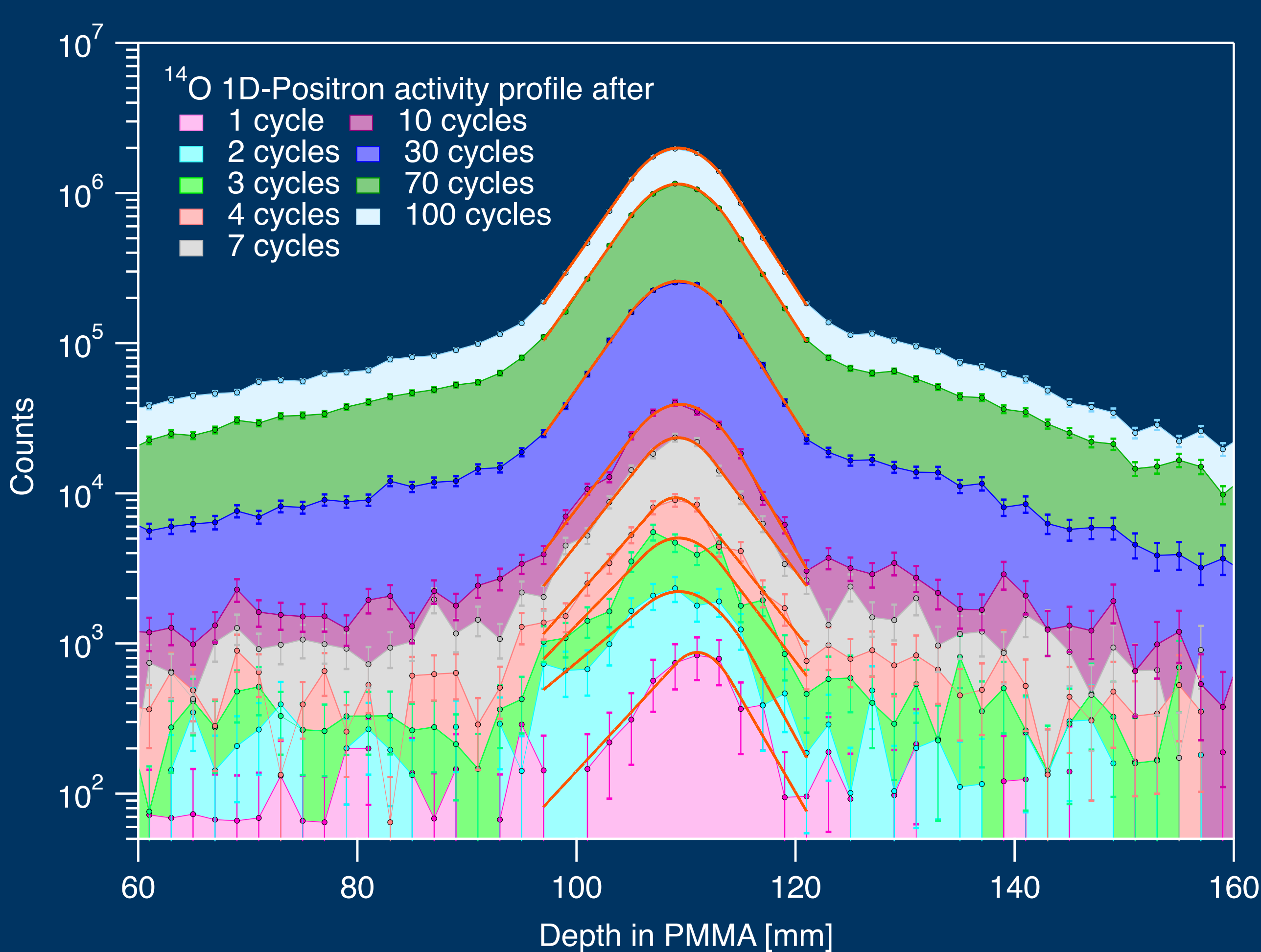
# Evaluation of the positron activity

## Peak position and its uncertainty



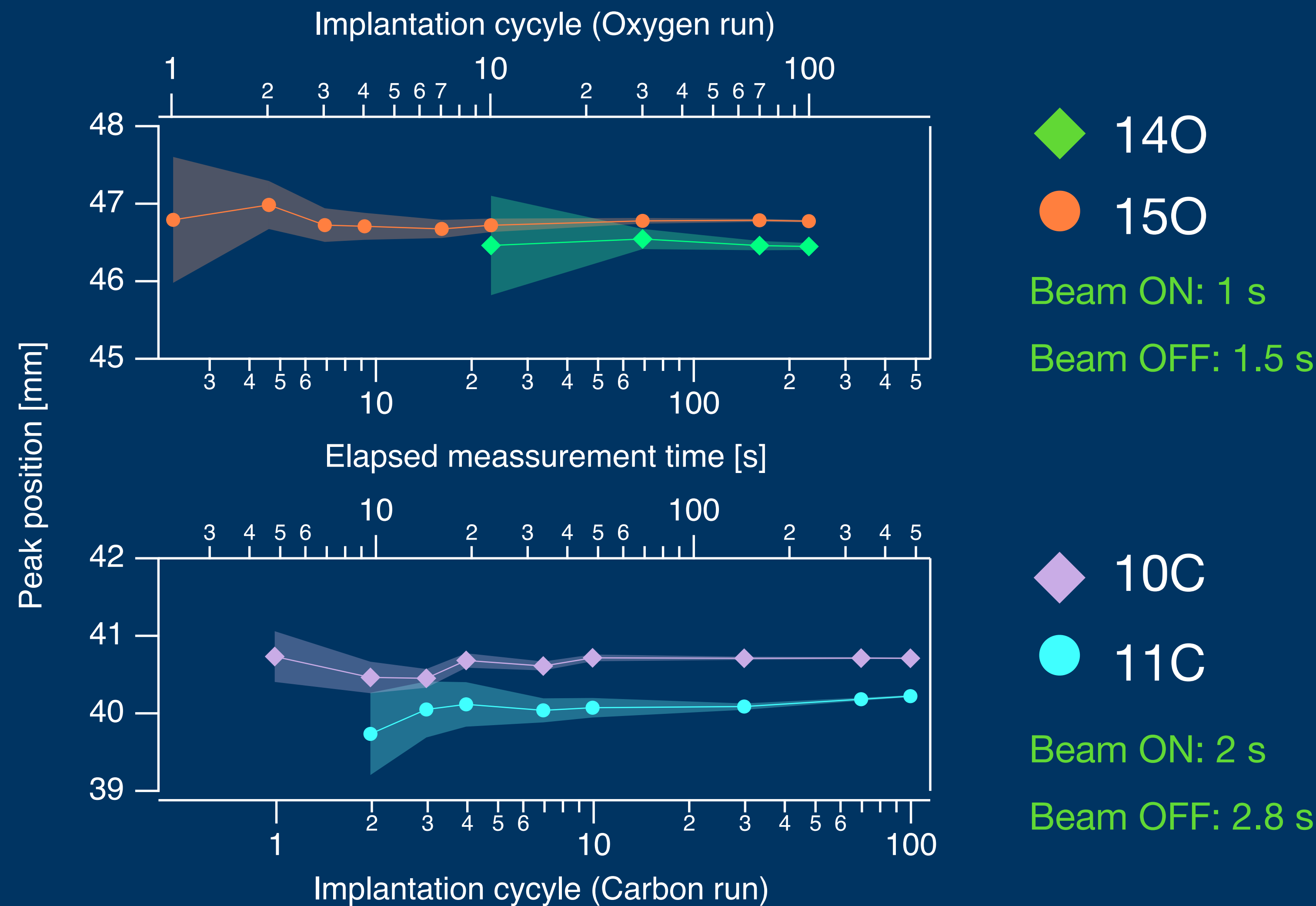
# Evaluation of the positron activity

Cumulative positron activity profiles 1D activity profiles during irradiation





# Evolution of positron activity peak



# Quasi-real-time range monitoring

## Impact of half lives, beam time structure and intensity

### Beam intensity

→ Production cross section

**$^{16}\text{O} \rightarrow \text{Be}$**

- $^{15}\text{O}$  : 43 mb
- $^{14}\text{O}$  : 1.2 mb

**$^{12}\text{C} \rightarrow \text{Be}$**

- $^{11}\text{C}$  : 46.7 mb
- $^{10}\text{C}$  : 4.3 mb



### Half life

$^{11}\text{C}$  : 1220.84 s

$^{15}\text{O}$  : 122.24 s

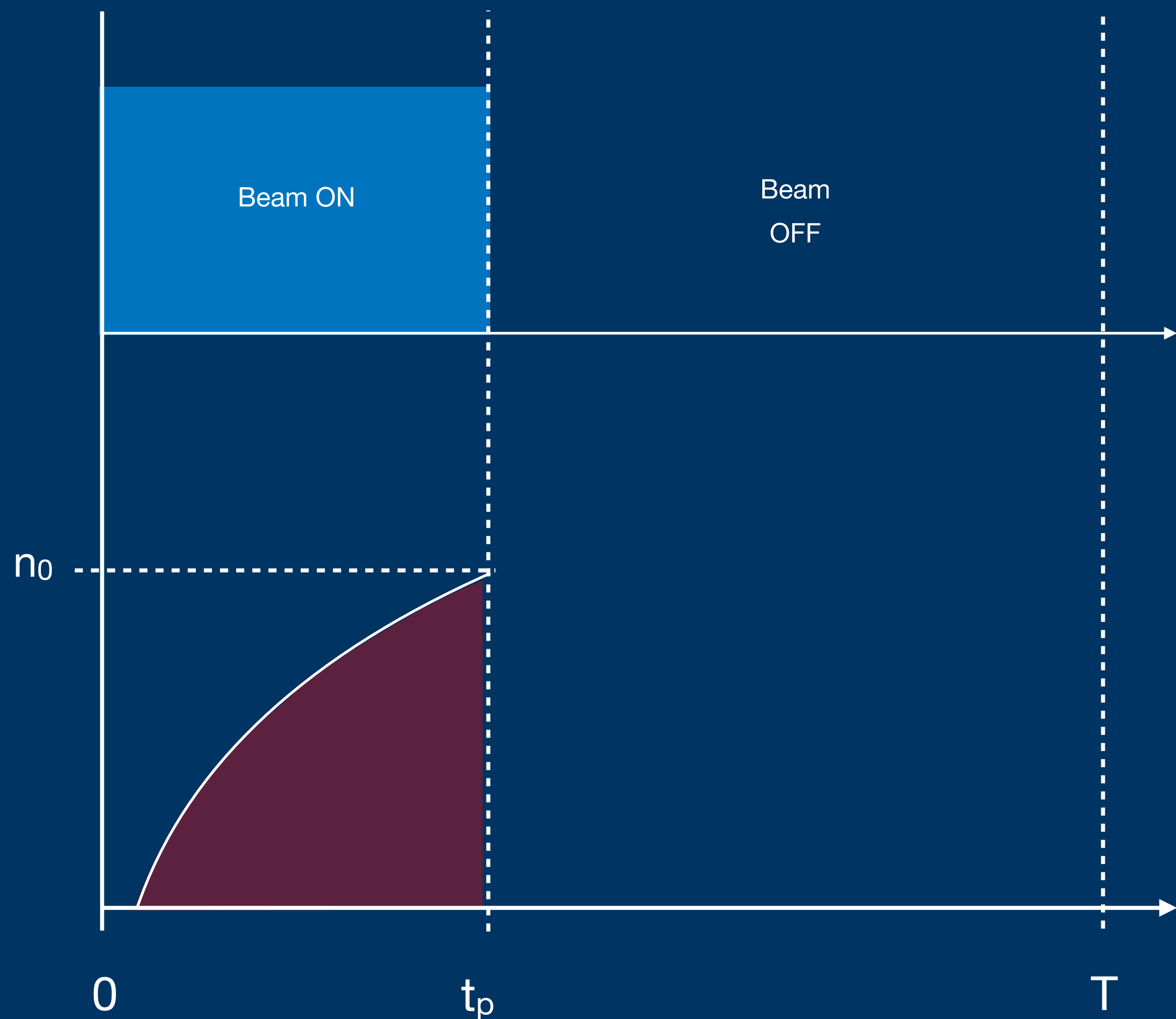
$^{14}\text{O}$  : 70.606 s

$^{10}\text{C}$  : 19.31 s

### Beam pulse time structure

# Quasi-real-time range monitoring

## Impact of half lives, beam time structure and intensity



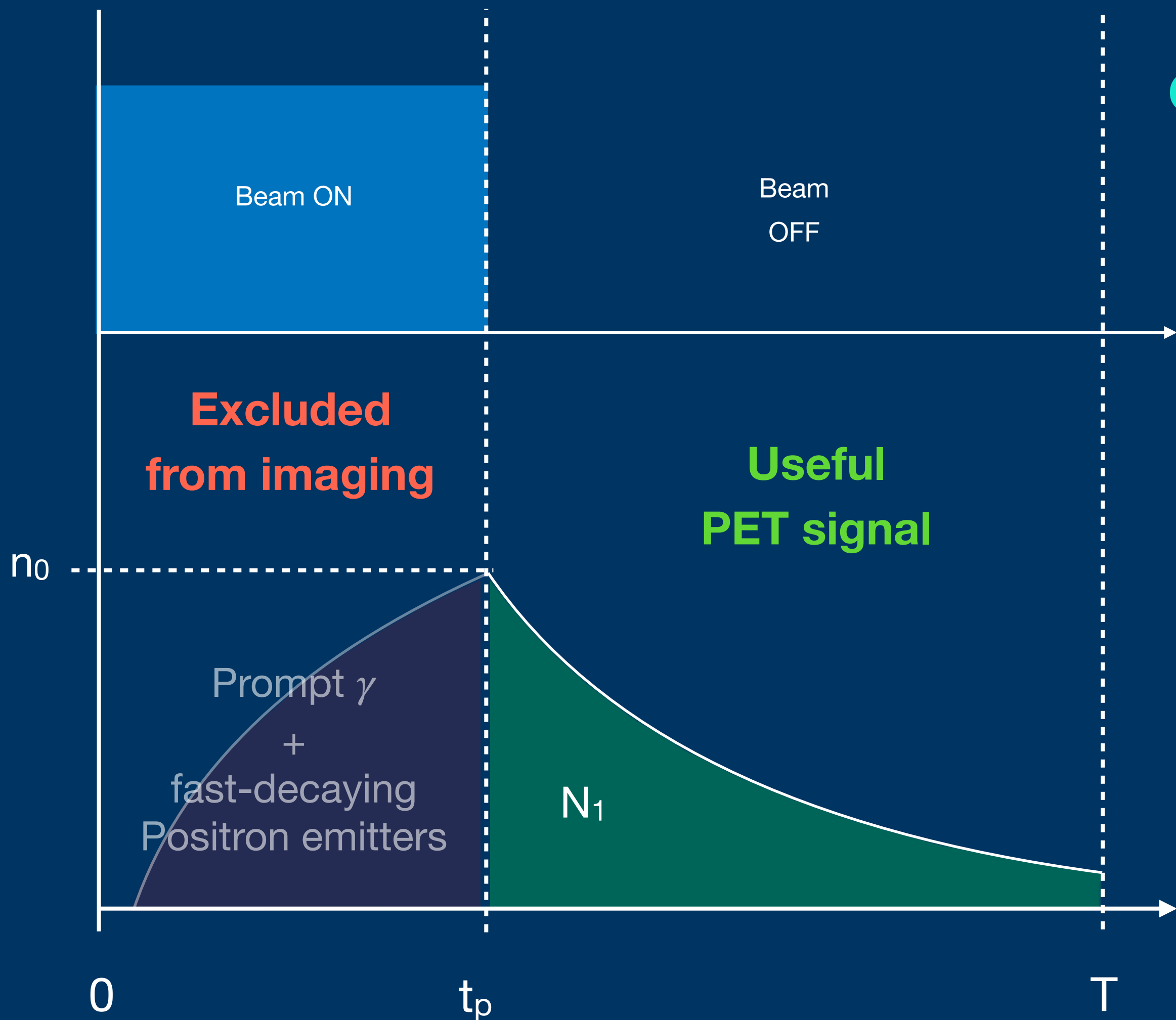
The amount of positron emitters left at the end of the pulse

$$n_0 \propto \frac{\sigma}{\lambda t_p} \left[ 1 - e^{-\lambda t_p} \right]$$



# Quasi-real-time range monitoring

## Impact of half lives, beam time structure and intensity



Coincidence event yield during the beam pause

After 1 implantation cycle

$$N_1 \propto n_0 \left[ 1 - e^{-\lambda(T-t_p)} \right]$$

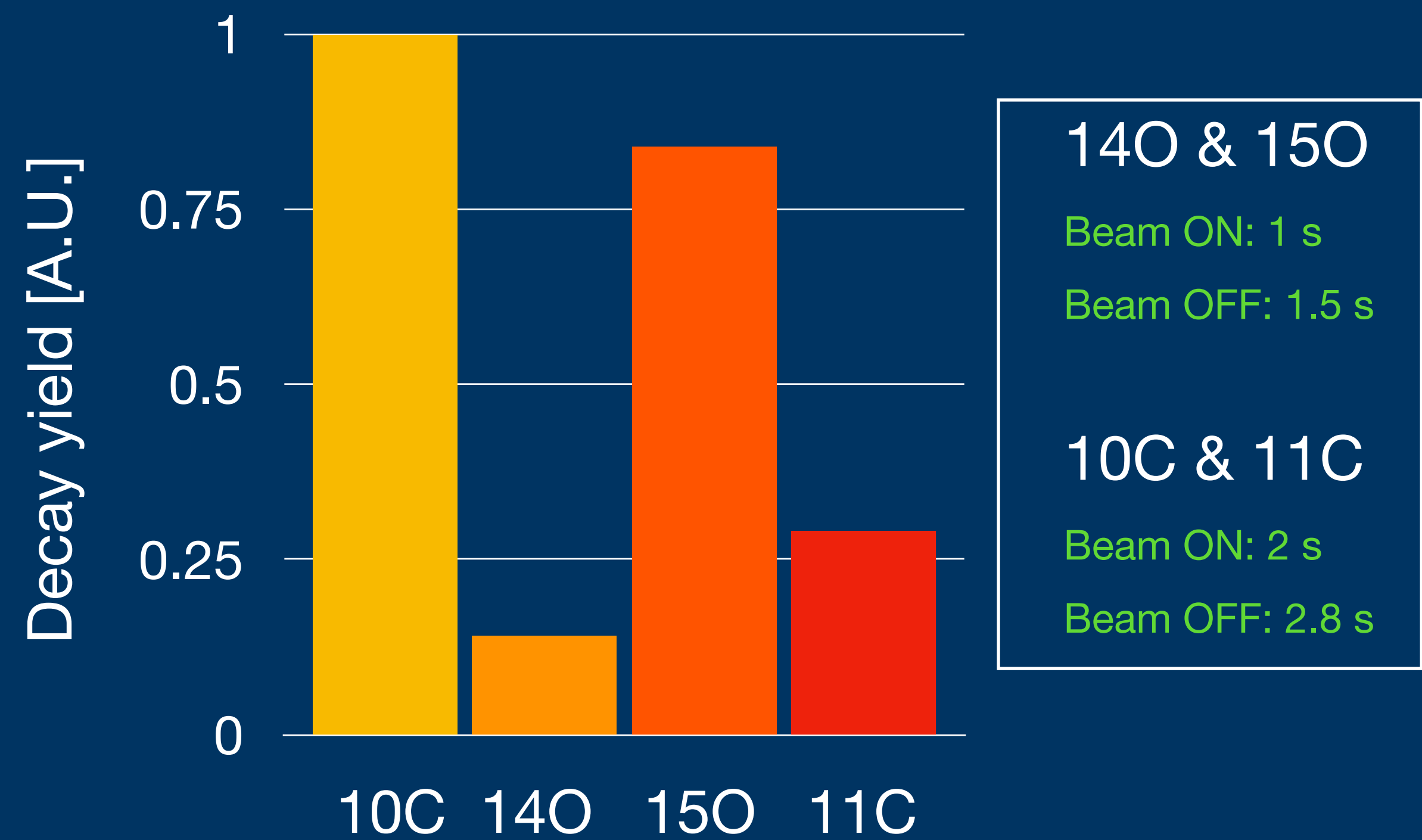
After  $n$  implantation cycles

$$N_n \propto N_1 \sum_{j=0}^{(n-1)} (n-j) e^{-\lambda j T}$$

# Quasi-real-time range monitoring

## Comparison of therapy relevant positron emitters of oxygen and carbon

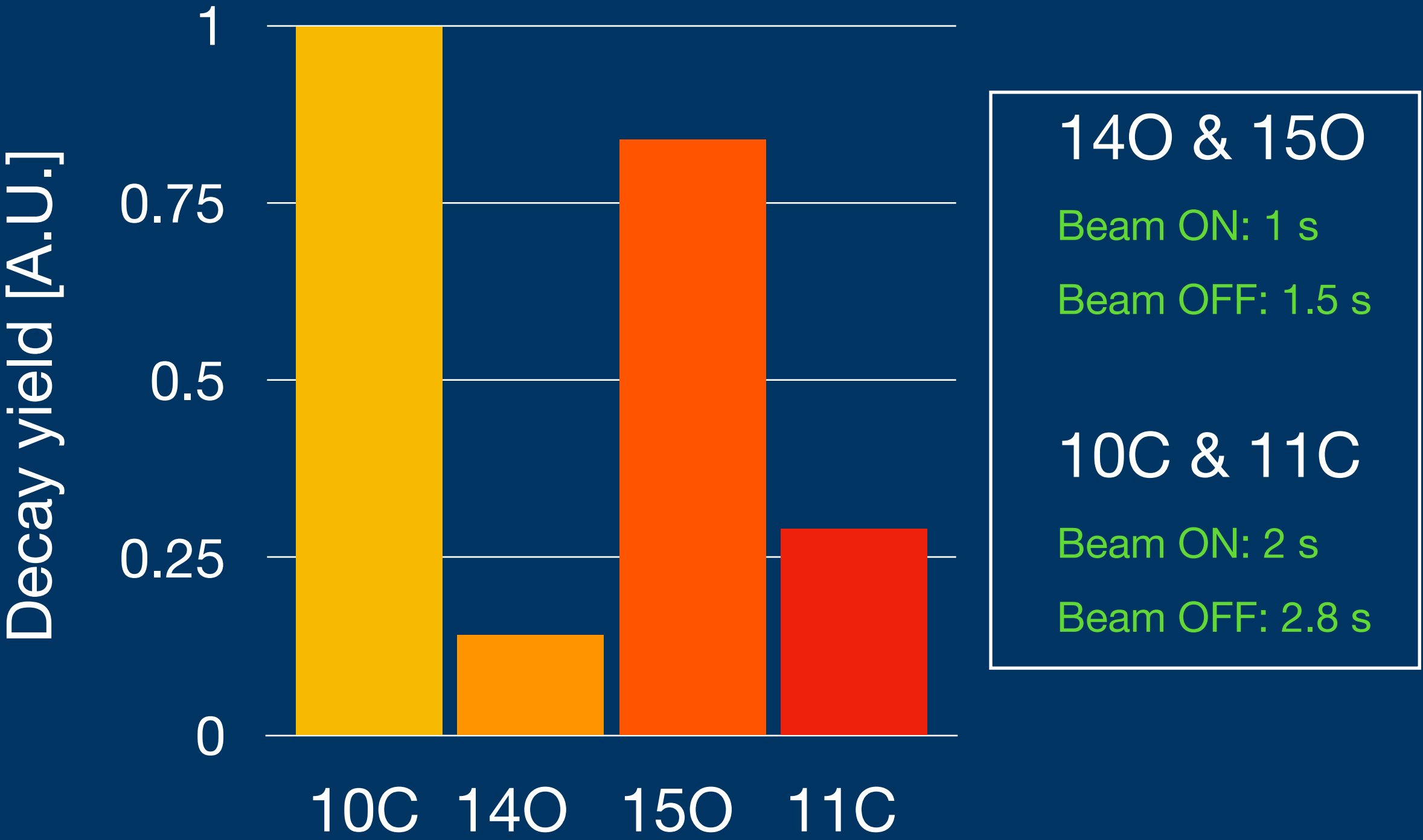
Time structure from experiment (n=1)



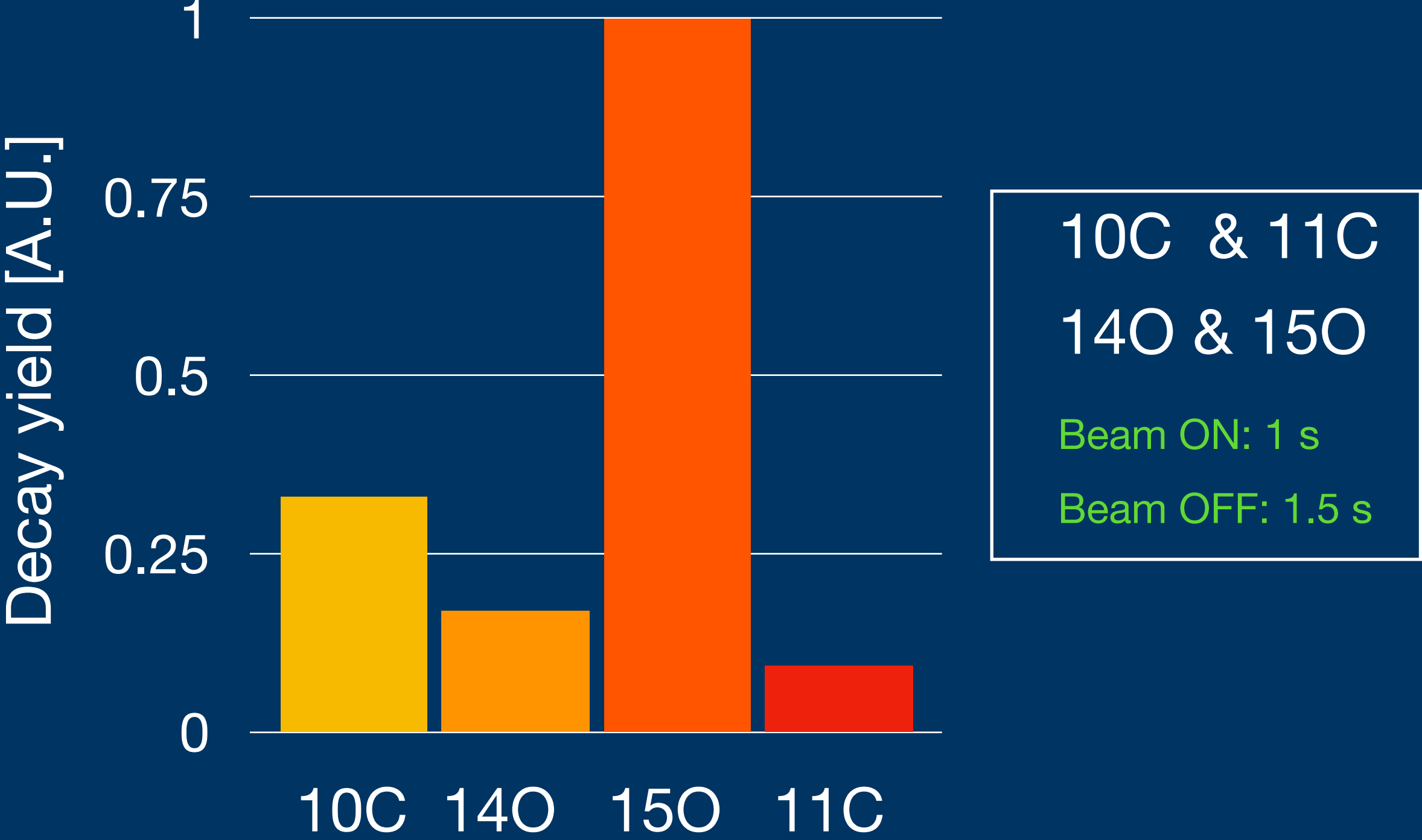
# Quasi-real-time range monitoring

## Comparison of therapy relevant positron emitters of oxygen and carbon

Time structure from experiment (n=1)



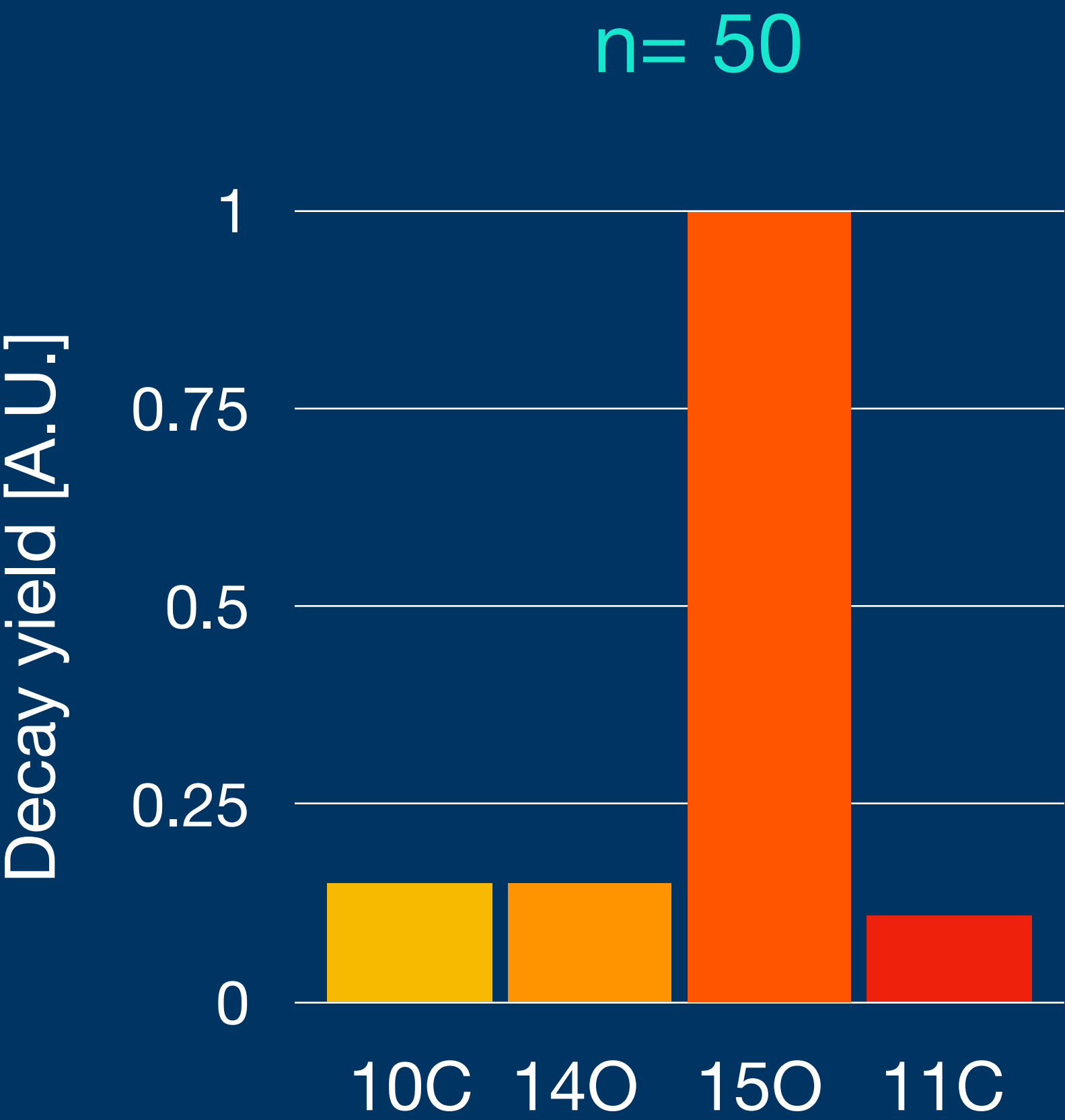
If beam time structure was same (n=1)



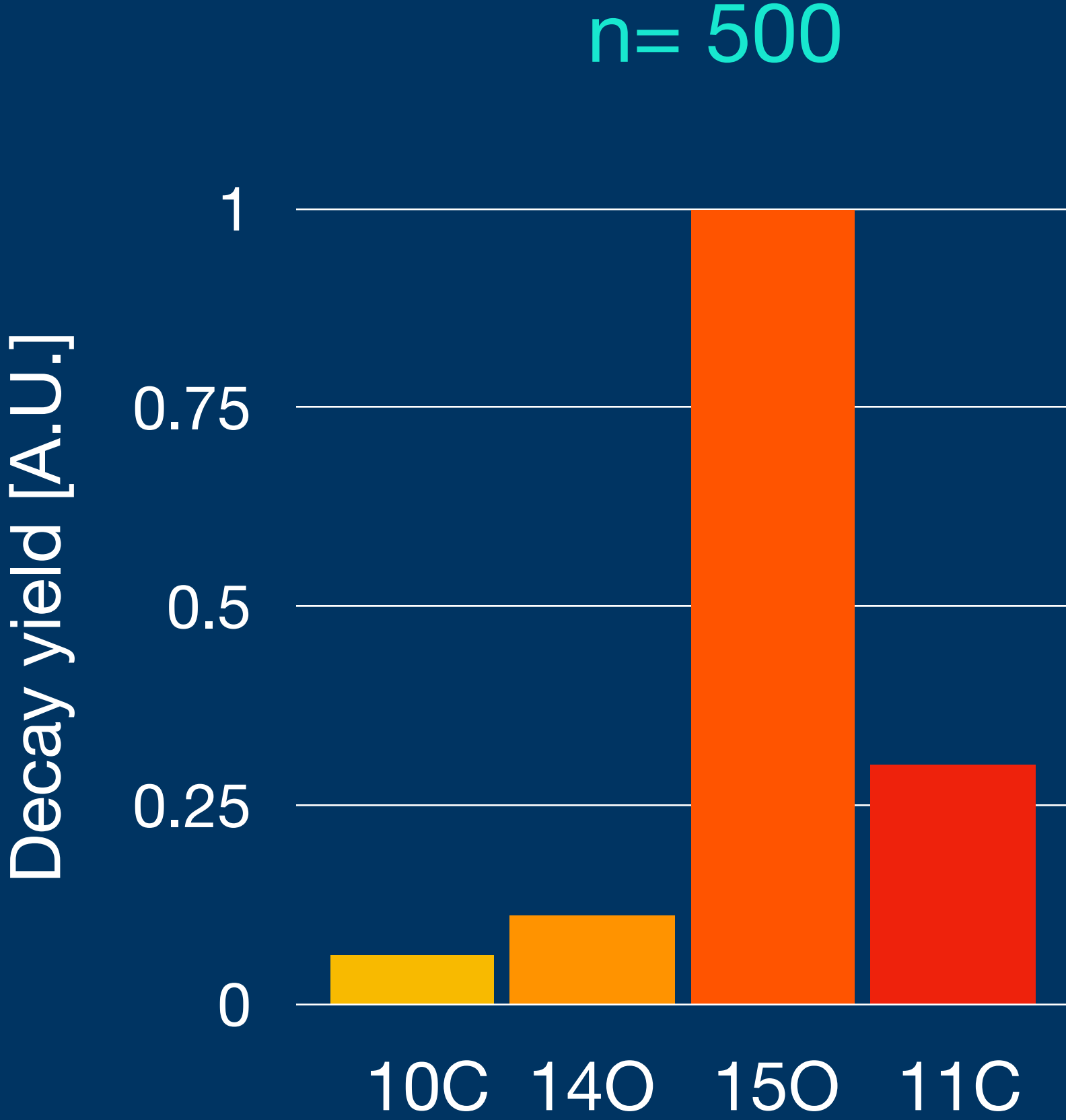


# Quasi-real-time range monitoring

## Comparison of therapy relevant positron emitters of oxygen and carbon

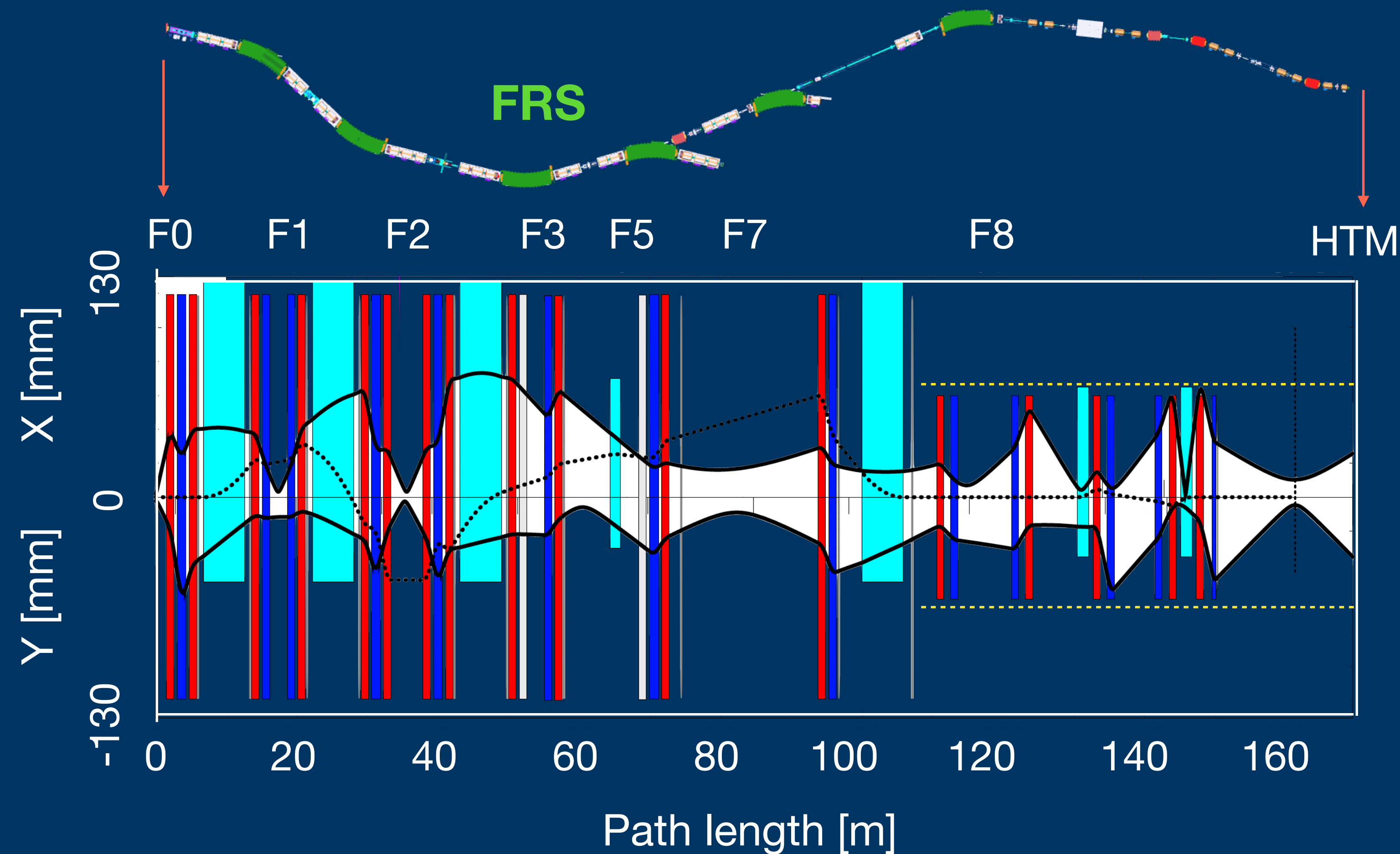


10C & 11C  
14O & 15O  
Beam ON: 1 s  
Beam OFF: 1.5 s



# BARB Biomedical experiments

## RIB transport from FRS to Medical cave (HTM)



**Challenging!**

Reduced aperture from F8  
200 mm → 120 mm

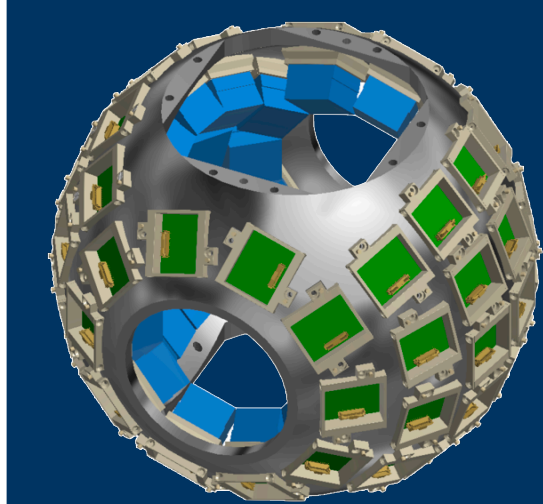
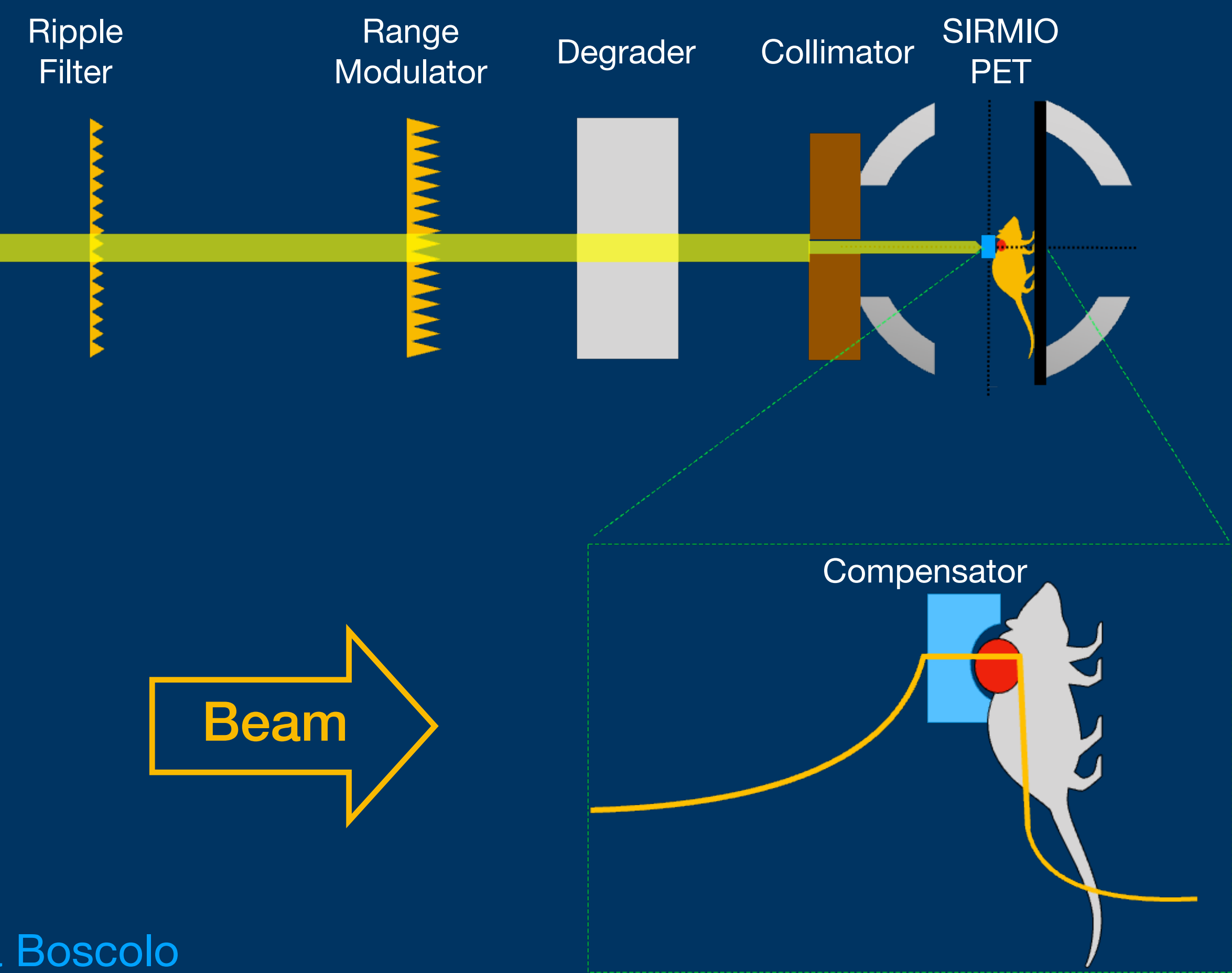
**Successful transport of  
15O and 11C to HTM**

**Measured conversion efficiency**  
 $\sim 3 \times 10^{-4}$  15O ions/16O ion in SIS 18

Hans Geissel  
Bernhard Franczak

# BARB Biomedical experiments

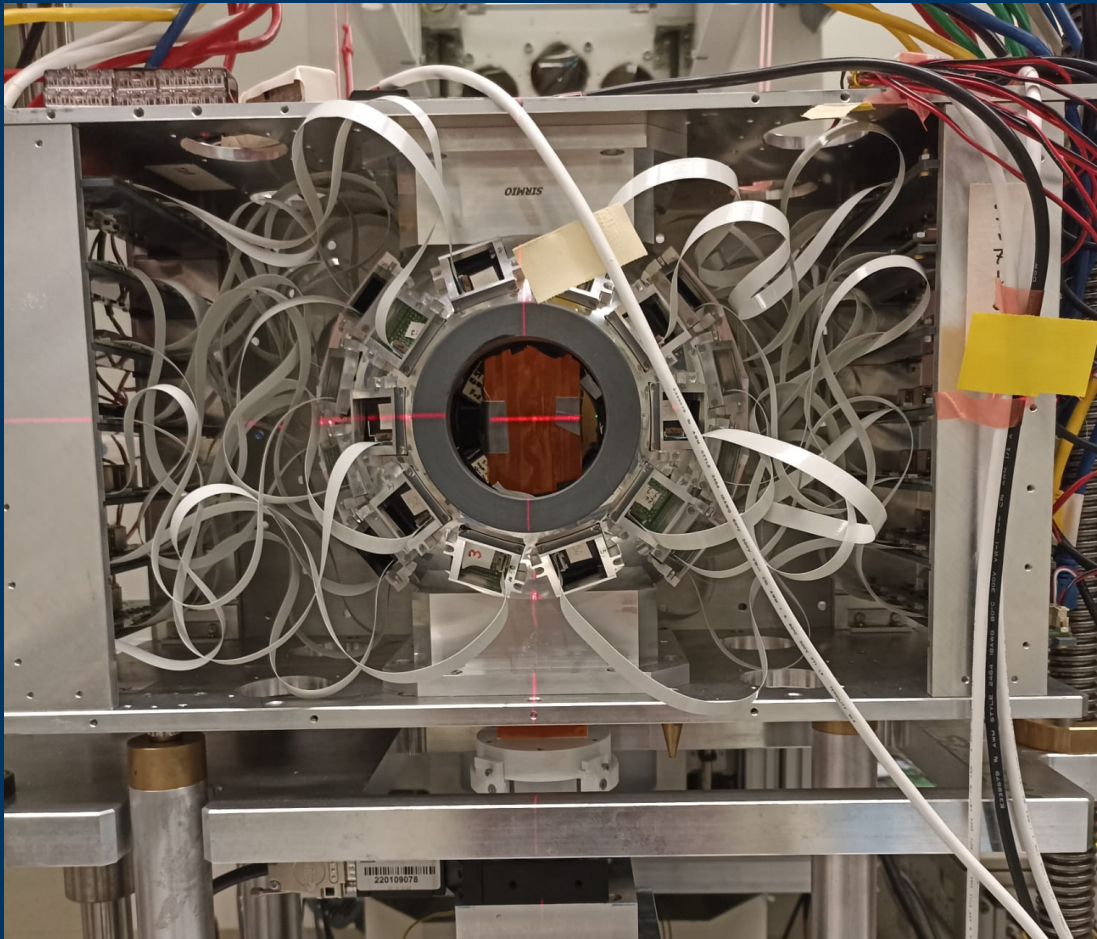
**RIBs for therapy:** Can we shrink the margin with the RIBs?



**SIRMIO PET**  
Inner radius: 72 mm  
Number of detectors: 56  
Number of rings: 6  
coverage: 44%



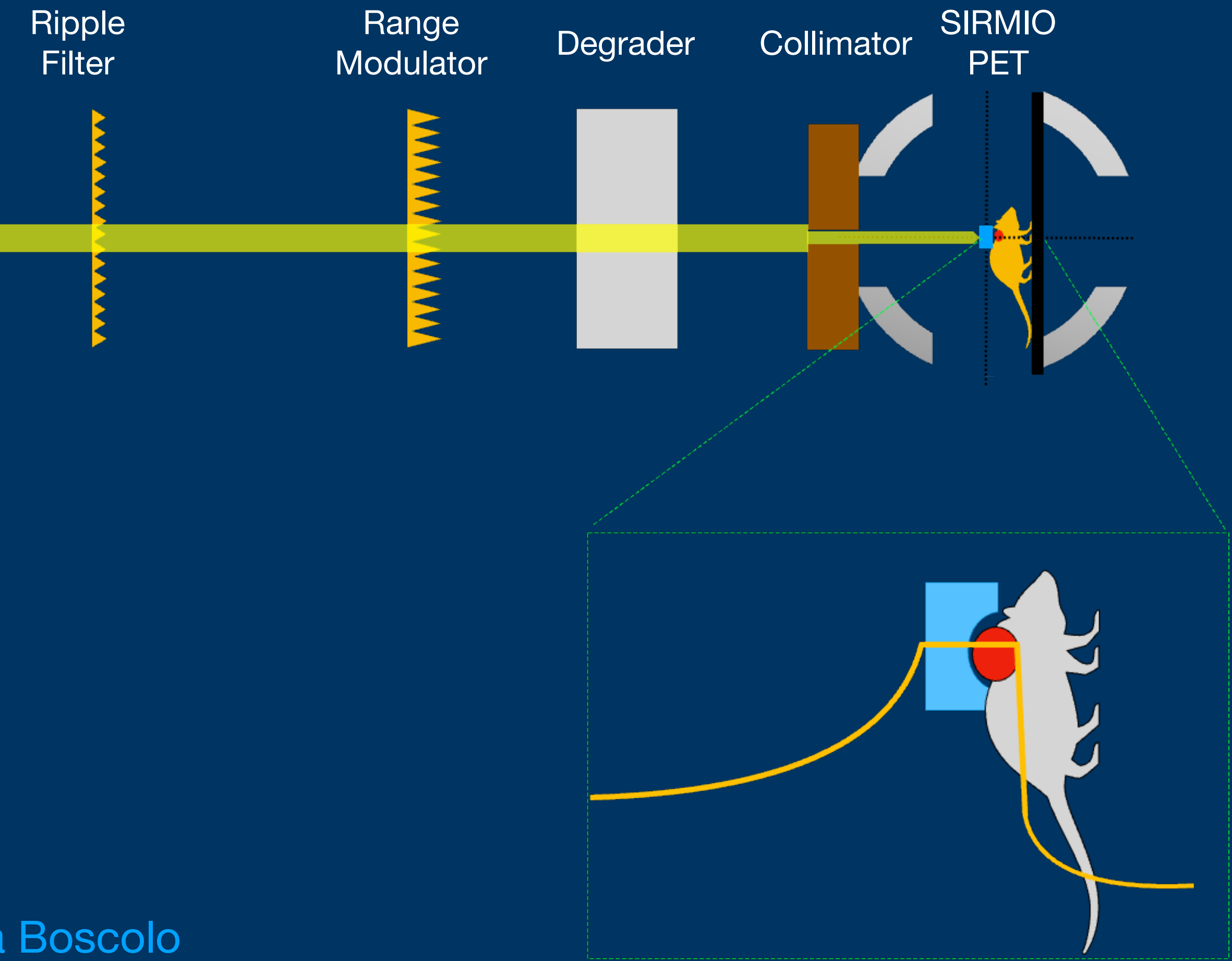
PI: Katia Parodi





# BARB Biomedical experiments

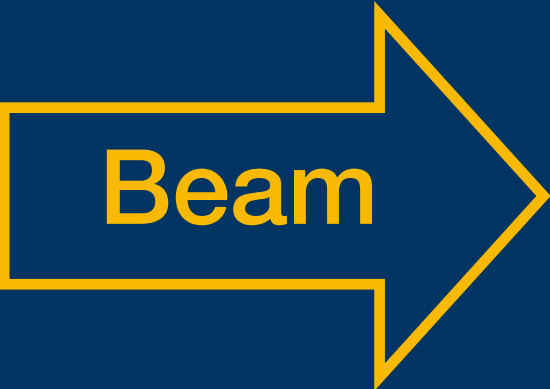
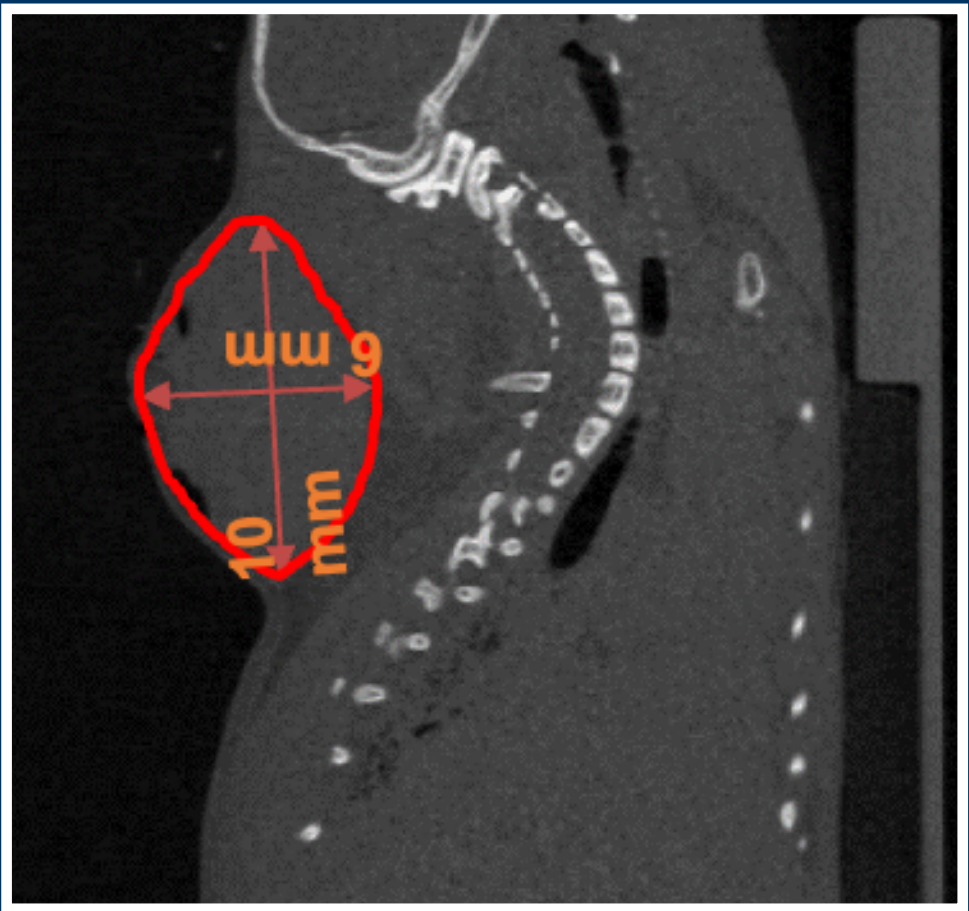
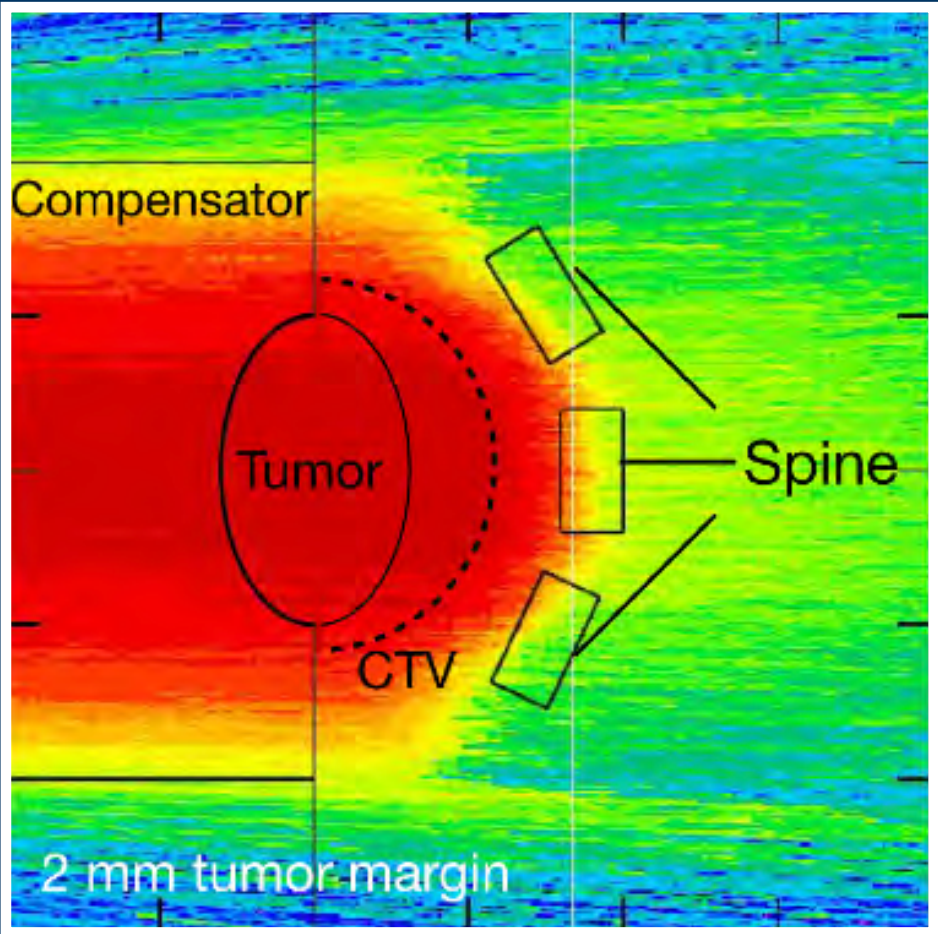
**RIBs for therapy:** Can we shrink the margin with the RIBs?



## Pre-irradiation assessment

Monte Carlo simulation

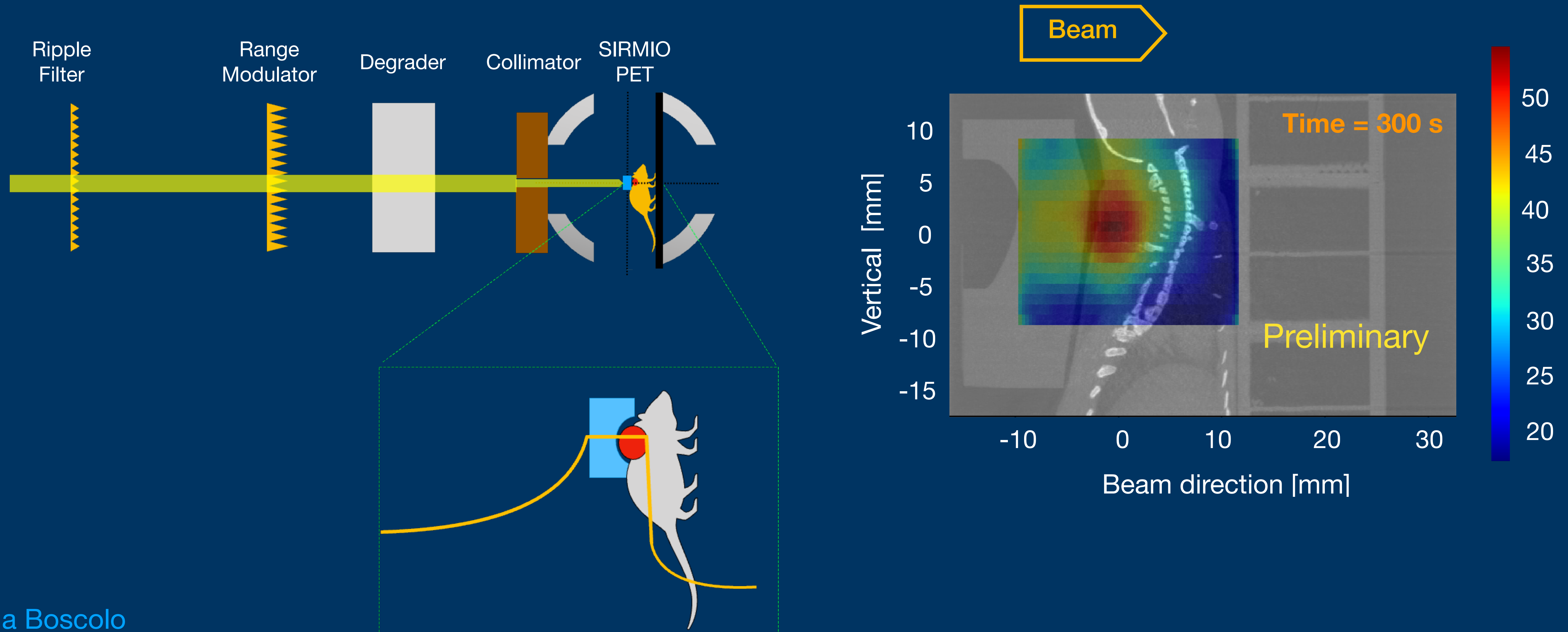
CT





# BARB Biomedical experiments

Online PET imaging of the radioactive  $^{11}\text{C}$  while treating a tumour sparing the spinal cord



# Conclusions and Outlook

- Therapeutic-quality  $^{11}\text{C}$  and  $^{15}\text{O}$  can be efficiently produced via the in-flight method, ensuring high intensities and purities.
- $^{15}\text{O}$  stands out as the prime candidate for quasi-real-time range monitoring, offering significant advantages from an imaging standpoint.
- Successful transportation of Radioactive Ion Beams (RIBs) from the Fragment Separator (FRS) to the GSI medical cave (HTM) has been accomplished.
- Demonstrated success in small animal irradiation and imaging using  $^{11}\text{C}$ , indicating promising applications in preclinical research.
- Implementation of online imaging techniques for radioactive  $^{11}\text{C}$  during tumour treatment, effectively sparing critical structures like the spinal cord, has been achieved.



# Acknowledgements

BARB Collaboration

Super-FRS Experiment Collaboration







THANK YOU